**Mathematical Modeling of the Pain and Progress of the First Stage of Nulliparous Labor**

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**Background:** Patient characteristics may contribute to the progress and pain of labor. Quantitative evaluation of the effects of patient characteristics requires robust mathematical models of labor progress and labor pain.

**Methods:** The authors retrospectively studied 100 sequential deliveries from each of five self-reported ethnic groups (Asian, Black, Hispanic, Other, and White). Demographic variables, cervical dilation, and numerical rating scores for pain before analgesia and cervical dilation were abstracted from the automated medical record. Labor progress was modeled with a biexponential function describing the latent and active phases of labor. Labor pain was modeled as a sigmoid function of cervical dilation by using a previously validated mathematical model. The covariates, including self-described ethnicity, were analyzed with NONMEM.

**Results:** The biexponential function described the time course of labor progress better than several alternative functions, including the sigmoidal function introduced by Friedman. The sigmoidal function of labor pain described its dynamic nature well, with substantial intersubject variability. Asian women had slower active labor than other ethnicities ($P < 0.01$). Asian women also reported less pain during their labor compared to all other patients ($P < 0.001$). Slower labor progress was associated with less rapid progression of pain, but this did not obviate the effect of Asian ethnicity on pain. Neuraxial analgesia is strongly associated with slower labor ($P < 0.0001$). Greater maternal weight was associated with slower active labor ($P < 0.0001$).

**Conclusions:** Mathematical models can be used to detect subtle effects of patient covariates on the progress and pain of the first stage of labor. Asian women and heavier women had slower labor and slower onset of labor pain than others. These effects were modest compared with the substantial remaining unexplained subject-to-subject variability in labor progress and labor pain.

PAIN increases over the course of labor and is highly variable among individuals. Although many physical and physiologic factors have been linked to the amount of labor pain women experience, it is difficult to discern the contribution of individual factors because the pain intensity changes with cervical dilation. As such, a model of labor progress is required to assess the effects of patient demographics and medical interventions on labor pain.

Several genetic polymorphisms that affect pain sensitivity have been described. Recently, studies have shown that ethnic differences exist in the duration of the second stage of labor and in the likelihood of Cesarean delivery. Even though the use of ethnicity as a marker of genetic variation has been debated, we hypothesized that a patient’s self-identified ethnicity might predict labor pain and progress.

In a retrospective cohort trial of 500 nulliparous parturients, we looked for associations among self reported ethnicity (Asian, Black, Hispanic, White, or Other), labor progress, and labor pain. We also investigated the influence of weight, height, maternal age, gestational age, and birth weight, neuraxial analgesia, oxytocin administration, labor induction, or rupture of membranes on labor progress and pain. We used mixed effects models to describe pain and progress of labor, and we tested the effects of these covariates on our models. This required development of a novel model for labor progress, and then we used this model to predict cervical dilation in our model of labor pain.

**Materials and Methods**

This retrospective cohort study was approved by the Institutional Review Board of Columbia University Medical Center (Columbia University Review Board, New York, NY). The requirement for informed consent was waived. Five hundred eligible parturients were identified by screening delivery records at the Columbia University-affiliated Sloane Hospital for Women. Working backward from May 2008, we gathered the data for this study from the first one hundred eligible women from each ethnic group. The inclusion criteria were (1) healthy nulliparous parturients aged 18–45 yr, (2) gestational age of 37–42 weeks, and (3) vaginal delivery of a singleton infant with birth weight 2.5–4.0 kg. Patients with preeclampsia and chronic pain syndromes were excluded.
Labor was managed by residents supervised by an attending obstetrician who was in the hospital. Patients were managed by using a standard clinical protocol with cervical examination every 4 h during latent labor and every 2 h during active labor unless otherwise clinically indicated. We gathered the numerical rating scale for pain, cervical dilation measurements, labor interventions, and time of observations for this study from the electronic medical record. Cervical dilation measurements were reported in 1 cm increments from 0 cm (closed cervix) to 10 cm (fully dilated cervix). Numerical rating scale (NRS) scores with contractions were recorded by obstetrical nurses and physicians by using an 11-point scale (0 for no pain and 10 for the worst pain imaginable). Patients were instructed to rate their pain at the peak of a contraction. Pain scores were requested on admission, with evidence of significant change in status and after treatment. Pain scores reported after patients received any analgesia are not considered in the model. Most labor nurses are bilingual in English and Spanish. When the patient could not converse in either language, a standard translation protocol was initiated as required by law.

We extracted labor characteristics (e.g., when membranes were ruptured) and labor interventions (e.g., when labor was induced, when oxytocin was administered, when analgesia was initiated) from the electronic medical record. We also obtained maternal weight, maternal height, maternal age, gestational age, and birth weight that were recorded from a structured nursing interview from the electronic medical record. Self-reported ethnicity was recorded by labor and delivery administrative personnel according to categories derived from the 2000 census. Although people of Hispanic ethnicity can be of any race, patients are asked to choose only one category.

Statistics and Data Analysis

Demographic and labor characteristics were compared among self-identified ethnic groups. Continuous variables were assessed for normality by using the Kolmogorov-Smirnov test. Normally distributed data are reported as mean ± SD and analyzed by using ANOVA. Nonnormally distributed data are reported as median (range). Differences among nonnormally distributed data are compared with a Mann-Whitney test for two group comparisons or a Kruskal-Wallis test for three or more groups (GraphPad InStat 3.06, San Diego, CA). For categorical data, relative risk was calculated by comparing each ethnic group’s characteristic to the population characteristic using chi-square analysis (GraphPad InStat 3.06). \( P < 0.05 \) was considered significant. The labor progress and labor pain models were analyzed with NONMEM (Nonlinear Mixed-Effects Modeling; Globomax, Ellicott City, MD) using PLT Tools (PLT Soft, San Francisco, CA). One hundred parturients were enrolled in each group; in our previous study with 100 subjects in test and training sets, we were able to identify a covariate effect with the magnitude of 1 NRS point.\(^1\) We consider this difference to be minimally clinically significant.

Labor Progress Model

We used a population approach to model the progress of labor. The labor progress model was then used in the model of labor pain. The development of the labor progress model is described in detail in the appendix. To briefly summarize, the times of each cervical exam were converted to the number of hours before the first measurement of full dilation (10 cm), which was considered time = 0. This was necessary because data collection did not begin at the same time in each patient, and cervical dilation was assessed more frequently as it progressed towards complete dilation. Thus, the first recording of full cervical dilation was chosen as the time-point to align the individual labor progress curves. In our analysis, time is reversed from usual clock time and proceeds along the x-axis from 0 (the time of complete cervical dilation) and is the number of hours before complete cervical dilation. Treating active and latent labor as linear, as originally described by Friedman,\(^8\) produced fits that were extraordinarily dependent on initial parameter estimates and not suitable for hypothesis testing. We tested linear, sigmoidal, and single exponential functions that were significantly inferior to a biexponential model (see appendix).

We therefore chose a biexponential model,

\[
\text{Dilation} = C e^{-\lambda_1 t} + (10-C) e^{-\lambda_2 t},
\]

where \(\lambda_1\) and \(\lambda_2\) are rate constants of active and latent labor, respectively, and where \(C\) is the number of centimeters of dilation associated with the active phase of labor. \(\tau\) is time. This model produces similar predictions to the bilinear model, but it is suitable for hypothesis testing with NONMEM. We used an exponential model for interindividual variability and an additive model for intrindividual variability. The full data set is provided as an Excel file (see Supplemental Digital Content 1, http://links.lww.com/ALN/A556), and the NONMEM control files (see Supplemental Digital Content 2, http://links.lww.com/ALN/A557, which is the NONMEM control file for the final labor progress model, and Supplemental Digital Content 3, http://links.lww.com/ALN/A558, which is the NONMEM control file for the final labor pain model) are available as text files.

We modeled the effect of time invariant continuous covariates, including age, weight, height, gestational age, and birth weight, as a proportional change in the values of \(\lambda_1\), \(\lambda_2\), or \(C\). For example, \(\lambda_1 = \theta_1 + \theta_2 \times (\text{patient age} - \text{median age})\), where \(\theta_1\) is the nominal value of the parameter and \(\theta_2\) is effect of age on the parameter. We modeled the effect of ethnicity by introducing new parameters into the model for each ethnic group. We modeled the effect of abrupt changes in patient state during labor

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(initiation of neuraxial analgesia, rupture of membranes, initiation of an oxytocin infusion) by using a time scale factor, as described in the appendix.

In each case, models were assessed for statistical significance by using the improvement in the objective function (−2 Log Likelihood – equivalent to the sum of squares in linear regression) with the likelihood ratio test. An improvement in −2 Log Likelihood greater than 6.63 with the introduction of a new parameter was considered statistically significant (chi-square distribution for P < 0.01 with 1 degree of freedom). The model parameters were estimated by NONMEM using the “first order conditional estimation” approach. We chose P < 0.01 rather than P < 0.05 in building the models to compensate (in part) for the large number of models examined in the process of model development.

We first explored whether treatment factors (initiation of neuraxial analgesia, oxytocin administration, induction of labor, or rupture of membranes) influenced the nominal progress of labor. Once these factors were incorporated into a model of labor progress, we explored the influence of the time invariant patient covariates weight, height, maternal age, gestational age, and birth weight. The completed model was then used to see if self-identified ethnicity further informed the progress of labor model. This order of analysis was chosen so that only an influence (if any) of self-identified ethnicity other than differences in weight, height, maternal age, gestational age, or birth weight would be captured.

Confidence in each parameter was assessed by using log likelihood profiling and bootstrap analysis. The log-likelihood profile calculated the −2 log likelihood by fixing the value of the parameter at different estimates and reestimating the other model parameters. Parameters that are known with certainty are expected to have a narrow range before the −2 log likelihood increases by more than 3.84 (chi-square distribution for P < 0.05, 1 degree of freedom). The bootstrap was calculated by randomly sampling a new data set from the patient data, with replacement, and then repeating the NONMEM analysis. This procedure was repeated 1,000 times. A 95% confidence interval was calculated from the bootstrap analysis as the interval from the parameter value at the 2.5% rank to the parameter value at the 97.5% rank. The log likelihood profile addresses the confidence in the parameter relative to the overall model. The bootstrap analysis addresses the confidence in the parameter relative to the data.

The improvement introduced from analysis of covariates was assessed by using a jackknife crossvalidation procedure in which the data were randomly grouped into 10 subsets. In 10 separate analyses, 9 of the 10 subsets were grouped, and the model was estimated from those data. The model was then applied to the excluded subset, and the median weighted residual error were calculated for the excluded subset. The median weighted residual was calculated as median \[ \frac{\text{measured dilation} - \text{predicted dilation}}{\text{predicted dilation}} \]. The median absolute weighted residual was calculated as median \[ \frac{\text{measured dilation} - \text{predicted dilation}}{\text{predicted dilation}} \]. This was repeated 10 times, each time excluding one-tenth of the data.

**Labor Pain Model**

We used the labor pain model that we have previously reported. The NRS pain response to cervical dilation was fit to a sigmoid equation:

\[
NRS = \frac{\text{NRSMIN} + (\text{NRSMAX} - \text{NRSMIN}) \cdot \frac{\text{CD}^2}{\gamma + \text{CD}^2}}
\]

with four parameters by using NONMEM. CD is the cervical dilation predicted by the labor progress model, NRSMIN is the minimum reported pain score, NRSMAX is the maximal reported pain score, CD50 is the cervical dilation associated with 50% of maximal pain, and \( \gamma \) is the steepness of the sigmoidal relationship. This model assumes that for a population of laboring women, reported pain with contractions is modest when the cervix is closed and increases in intensity as the cervix dilates, reaching maximum intensity when the cervix is fully dilated. The assumption of monotonicity was verified by tallying the number of women who reported a decrease in pain during labor and by qualitatively assessing the distribution of bias and the fit of the model to the raw data.

For two reasons, we modeled pain as a function of the post boc individual Bayesian predicted cervical dilation from the labor progress model, rather than the actual measured dilation. First, some pain measurements did not have associated cervical dilations. Using the individual post boc Bayesian predicted dilations provided a predicted cervical dilation at every point in time. Second, the post boc Bayesian predicted dilation is arguably a more accurate measurement than an actual measurement, both because the actual measurement is always reported as an integer and because the prediction represents, in part, an average of many predictions. Consider progressive cervical examinations of 4, 4.5, 5.0, and 5.5 cm, which is what the post boc Bayesian prediction would reflect.

We tested whether the sigmoidal model was better than a simple linear model. We then fit the sigmoidal model of NRS as a function of predicted cervical dilation, and we systemically evaluated the effects of weight, height, maternal age, gestational age, and birth weight on each parameter of the model. We then tested whether the presence or absence of an oxytocin infusion, labor...
induction, and rupture of membranes affected the parameters of the model. We did not test neuraxial analgesia; by definition, all data following the initiation of neuraxial analgesia initiation were censored from the analysis. Lastly, we tested the effect of the instantaneous rate of dilation on each of the model parameters.

Once the model incorporated the effects (if any), of weight, height, maternal age, gestational age, birth weight, oxytocin administration, labor induction, rupture of membranes, and the instantaneous rate of dilation we tested whether self-identified ethnicity affected any of the parameters. As described for the labor progress model, we took this approach to identify only an effect of ethnicity (if any) not already explained by other patient covariates. In addition, we tested each possible combination of ethnicities to identify the most parsimonious model that properly accounted the effect (if any) of self-reported ethnicity on time course of labor pain. The calculation of instantaneous rate is shown in the appendix.

We used additive models for interindividual variability in NRS\textsubscript{MIN} and NRS\textsubscript{MAX}, and we used an exponential model for the interindividual variability in CD\textsubscript{50}. Because interindividual variability was miniscule on NRS\textsubscript{MAX}, it was fixed in our final model. No interindividual variability was modeled for $\gamma$. We used an additive model of intraindividual residual error. Control files for the final model is provided as Supplemental Digital Content 3, http://links.lww.com/ALN/A558.

Confidence in each parameter in the labor pain model was assessed as described for the labor progress model. However, the log likelihood profiles produced curves with fluctuations as a result of the very steep value of $\gamma$ in the model, causing a near step-function around CD\textsubscript{50}. This hindered NONMEM from accurately searching the parameter space. After verifying that the steepness of the relationship around CD\textsubscript{50} had not precluded NONMEM from converging on the optimal model, log likelihood profiles were run approximately 100 times with different starting parameters and occasionally with some parameters of the model fixed to verify that the curves were unimodal and to force NONMEM to further explore the parameter space. Lastly, for several log likelihood profiles, some residual jaggedness was removed by manually selecting local minimum values.

### Results

Delivery records from October 2006 to May 2008 were screened (6,524 women). Enrollment and exclusion criteria are shown in figure 1. The five self-reported groups that have major representation in our population are Asian (12%), Black (12%), Hispanic (30%), White (29%), and Other (18%). All Hispanic and White women were delivered between May 2007 and May 2008. Because of their decreased frequency, Black, Asian, and Other women were delivered between October 2006 and May 2008. The demographic characteristics of these five groups are shown in table 1. Gestational age, maternal age, height, weight, birth weight, and emotional status did not differ among the five groups. Employment, marital status, and primary language varied among groups. On the basis of an analysis of primary and secondary languages, the Other group consists of a large number of subjects with mixed ethnicity, and the Asian group is composed of patients from many countries in Asia including China, Japan, Korea, India, and the Philippines.

The characteristics of labor and its management are described in table 2. Overall, 27% of patients were admitted for induction of labor, 60% of patients received oxytocin during the first stage of labor, and 94% of patients received labor analgesia. The majority of patients were treated with combined spinal epidural analgesia or epidural analgesia, treatments which are referred to collectively as neuraxial anesthesia. Three percent of patients were treated with opioids for labor analgesia. Induction, oxytocin, and analgesia rates were similar among groups. The cervical exams at arrival to the hospital are also similar among the groups. The length of the second stage of labor was significantly shorter for Black women (median 1.1 h) and longer for the Other group (median 1.7 h) compared with the overall population, who had a median second stage of labor of 1.4 h. Hispanic women were more likely then others to have their membranes artificially ruptured than other women (relative risk = 1.4).

### Labor Progress Model

As explained in the appendix, the biexponential model accurately captured the shape of the progress of labor. Maternal age, height, gestational age, birth weight, oxytocin infusion, labor induction, and rupture of mem-
branes did not significantly affect the progress of labor. As shown in table 3, self-identified Asian ethnicity, increasing maternal weight, and presence of neuraxial analgesia were associated with significantly slower labor. The model was built by first incorporating the strongest effect (presence of neuraxial analgesia) and then incorporating the next strongest effect (weight) and finally adding the effect of self-identified ethnicity. Thus, the P values shown in table 3 represent the P values for the incremental improvement, and they are thus conservative relative to the improvement that might be observed from assessment of the covariate effect in the absence of other explanatory covariates.

Figure 2 shows all of the labor progress data for (A) an initial model without covariates and (B) the final model with the covariate effects. The top figures show the observations as vertical lines and the individual post hoc predictions (gray lines). Figures 2C and 2D show the error in the fits, based on the population values of the parameters (e.g., with interindividual variability set to 0). The fit for the initial and final models are almost visually indistinguishable. Indeed, the median absolute prediction error for the initial model is 0.98 cm, which the model incorporating covariates has only improved to 0.94 cm. Figure 3 shows the predicted (X axis) versus measured (Y axis) cervical dilation for (A) the initial model and (B) final covariate adjusted model. As noted for figure 2, the improvement in fit with the inclusion of covariates is almost invisible in the figure. Thus, even though the covariate effects shown in table 3 are highly statistically significant, they represent very small improvements in the model.

Figure 4 shows the log-likelihood profiles and 95% confidence intervals for active labor rate constant ($\lambda_1$), latent labor rate constant ($\lambda_2$), and the coefficient (C) on the model parameters in the Non-Asian and Asian patients. Figure 5 shows log-likelihood profiles and 95% confidence intervals for the neuraxial analgesia scale factor and the effect of weight on the active and latent rate constants. In every case, the parameter estimates are well constrained within the boundaries of the model and do not cross 0, showing that they are statistically different from 0. The likelihood profiles similarly reach the edges of the 95% confidence interval derived from the

### Table 1. Demographic Characteristics of 500 Nulliparous Women

<table>
<thead>
<tr>
<th></th>
<th>Overall (n = 500)</th>
<th>Asian (n = 100)</th>
<th>Black (n = 100)</th>
<th>Hispanic (n = 100)</th>
<th>Other (n = 100)</th>
<th>White (n = 100)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Gestational age, weeks</td>
<td>39 ± 1</td>
<td>39 ± 1</td>
<td>39 ± 1</td>
<td>39 ± 1</td>
<td>39 ± 1</td>
<td>39 ± 1</td>
</tr>
<tr>
<td>Median age, yr</td>
<td>29 (18–44)</td>
<td>30 (19–41)</td>
<td>27 (18–39)</td>
<td>26 (18–42)</td>
<td>30 (18–44)</td>
<td>31 (19–41)</td>
</tr>
<tr>
<td>Weight, kg</td>
<td>78 ± 15</td>
<td>74 ± 13</td>
<td>84 ± 20</td>
<td>76 ± 12</td>
<td>74 ± 11</td>
<td>81 ± 16</td>
</tr>
<tr>
<td>Height, cm</td>
<td>163 ± 9</td>
<td>162 ± 7</td>
<td>164 ± 6</td>
<td>164 ± 6</td>
<td>163 ± 6</td>
<td>161 ± 9</td>
</tr>
<tr>
<td>Baby weight, kg</td>
<td>3.23 ± 0.37</td>
<td>3.17 ± 0.36</td>
<td>3.15 ± 0.35</td>
<td>3.24 ± 0.36</td>
<td>3.31 ± 0.40</td>
<td>3.28 ± 0.38</td>
</tr>
<tr>
<td>Employment, % employed*</td>
<td>52 65</td>
<td>46 31</td>
<td>54 65</td>
<td>65</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Marital status, % married*</td>
<td>66 93</td>
<td>40 39</td>
<td>67 93</td>
<td>93</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Emotional status, % happy</td>
<td>82 81</td>
<td>82 80</td>
<td>80 85</td>
<td>84</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Primary language, % English*</td>
<td>71 70</td>
<td>76 40</td>
<td>75 91</td>
<td></td>
<td></td>
<td></td>
</tr>
</tbody>
</table>

The number of cervical exams per patient varied significantly by race ($P < 0.001$, Kruskal-Wallis test). Values are medians (range). Relative risk (RR) compares the value for the specific group to the population characteristic. Blacks and Hispanics had more exams than Others ($P < 0.01$, 0.05). There was no difference in the incidence of labor induction. Hispanics had higher RR of AROM 1.4 (artificial rupture of membranes, 1.0–2.0; Fisher Exact test). The number of numerical rating scale (NRS) per patient varied significantly by ethnicity ($P < 0.001$, Kruskal-Wallis test). Asians had lower scores than Hispanics and Whites ($P < 0.001$).

* $P < 0.001$; † $P < 0.05$.

SROM = spontaneous rupture of membranes.

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bootstrap analysis at roughly the \( P < 0.01 \) range. This shows that the likelihood profiles are not dependent on particular patients or observations.

Figure 6A shows predictions of the labor progression model moving forward in time from 1 cm of cervical dilation. The “nominal” patient is a non-Asian patient of median weight without neuraxial analgesia. The prediction for that patient appears as a black line. Representative predictions are shown for an Asian patient (red line) also of median weight without neuraxial analgesia, a non-Asian patient of the lightest weight in the population (48 kg, blue line), a non-Asian patient of the heaviest weight in the population (171 kg, green line), a nominal patient with neuraxial analgesia placed at 1 cm of cervical dilation (dashed line) and 4 cm of cervical dilation (dotted line). The effect of neuraxial analgesia is visible as a very slight slowing in rate. Figure 6B is the prediction as determined by the model.

Figure 7A shows the individual post hoc Bayesian fits for the model used to interpolate cervical dilations. The only covariate incorporated in this model is the presence of neuraxial analgesia. As explained in the methods, labor pain was modeled as a function of the cervical dilation predicted by the labor progress model. This provided a predicted cervical dilation at every timepoint. The model was based on incorporation of the neuraxial analgesia effect, which is associated with a different progress of labor. The median error was 0.01 cm and the median absolute error was 0.42 cm. Figure 7B shows the final post hoc Bayesian fits.

### Table 3. Labor Progress Model

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Parameter Approximate CV*</th>
<th>( P ) Value 95% Confidence Interval</th>
</tr>
</thead>
<tbody>
<tr>
<td><strong>Non-Asians</strong></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Active labor rate constant, ( \text{hr}^{-1} )</td>
<td>0.65</td>
<td>0.51 to 0.85</td>
</tr>
<tr>
<td>Latent labor rate constant, ( \text{hr}^{-1} )</td>
<td>0.11</td>
<td>0.10 to 0.13</td>
</tr>
<tr>
<td>Coefficient, cm</td>
<td>4.6</td>
<td>4.0 to 5.2</td>
</tr>
<tr>
<td><strong>Asians</strong></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Active labor rate constant, ( \text{hr}^{-1} )</td>
<td>0.48</td>
<td>0.34 to 0.73</td>
</tr>
<tr>
<td>Latent labor rate constant, ( \text{hr}^{-1} )</td>
<td>0.07</td>
<td>0.05 to 0.09</td>
</tr>
<tr>
<td>Coefficient, cm</td>
<td>5.8</td>
<td>4.8 to 6.6</td>
</tr>
<tr>
<td>Epidural scale factor</td>
<td>0.63</td>
<td>0.48 to 0.78</td>
</tr>
<tr>
<td>Weight factors</td>
<td></td>
<td></td>
</tr>
<tr>
<td>On active labor rate constant, ( \text{kg}^{-1} )</td>
<td>0.0084</td>
<td>&lt; 0.0001</td>
</tr>
<tr>
<td>On latent labor rate constant, ( \text{kg}^{-1} )</td>
<td>-0.011</td>
<td>&lt; 0.0001</td>
</tr>
<tr>
<td><strong>Errors</strong></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Median error, cm</td>
<td>0.19</td>
<td>0.0012 to 0.0167</td>
</tr>
<tr>
<td>Median absolute error, cm</td>
<td>0.94</td>
<td>-0.016 to -0.006</td>
</tr>
</tbody>
</table>

* The approximate coefficient of variance (CV) is actually the standard deviation of the interindividual variability in the log domain.

Fig. 2. Labor progress data. Small vertical lines are data points, and gray lines are individual fits. (A) Initial model without covariates, solid black line represents the typical individual, thick gray line represents a supersmoother through the data, and the dashed line is a supersmoother through the post hoc estimates. (B) Final model incorporating covariate effects, thick gray line represents a supersmoother through the data, and the dashed line is a supersmoother through the post hoc estimates. (C and D) Individual measured-predicted observations over time for the initial and final modals are thin gray lines. The dashed line is a supersmoother through the data. Asian ethnicity, presence of neuraxial analgesia, and maternal weight were included as covariates in the final model. All data points are represented in the initial model. The final model excludes patients in whom weight was not recorded (n = 98 excluded).
estimate for the final covariate model. It is almost indistinguishable visually from the top graph. This model was not used for the labor pain analysis because it excludes those patients whose weights were not recorded. The bias and accuracy is similar to the upper figure, with a median error of $+0.005$ cm and a median absolute error of $0.43$ cm.

The magnitude of unaccounted for intersubject variability can be estimated by comparing the residual error for the population model (fig. 2D, median error $= 0.94$ cm) with the residual error in the individual post hoc Bayesian model (fig. 7B, median error $= 0.43$ cm). There is considerable intersubject variability that is not accounted for by the covariates assessed in this study.

### Labor Pain Model

Maternal weight, height, maternal age, gestational age, birth weight, oxytocin infusion, labor induction, and rupture of membranes did not significantly affect the relationship between cervical dilation and NRS score. As shown in table 4, self-identified Asian ethnicity and the instantaneous rate of labor affected the relationship of cervical dilation to NRS score. Thus, $P$ values shown in...
Table 4 represent the incremental improvement, first of incorporating self-identified ethnicity, and then from incorporating dilation rate.

Figure 8 shows the data fits to (A) the initial model without covariates and (B) the final model incorporating self-identified Asian ethnicity and the rate of cervical dilation. In the initial model, there is only one fit; in the final model, the prediction incorporates instantaneous dilation rate and thus is not a simple line. Rather, individual predictions are shown as black. The shallower line represents the Asian predictions.

A single observation is circled in figure 8. This point represents an Asian patient whose NRS pain score was 3 at a predicted cervical dilation of 9 cm and in whom labor had slowed considerably. Removing this observation did not affect the parameters or the statistical significance of the effect of self-identified ethnicity. How-

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**Fig. 5.** Log Log-likelihood profiles: epidural and weight factors. Significance estimates calculated on a chi-square distribution (dashed lines) and 95% confidence intervals derived from bootstrap analysis (vertical lines) for (A) epidural scale factor, and the effect of weight on the (B) active and (C) latent rate constants.

**Fig. 6.** Effect of individual factors on labor progress. (A) Forward simulations from the labor progression model of the time course required for cervical dilation from 1–10 cm for a “nominal” patient (non-Asian patient of median weight without epidural analgesia), Asian patient (median weight without epidural analgesia), lightest patient (a 48-kg non-Asian patient), heaviest patient (a 171-kg non-Asian patient), and a patient (non-Asian, median weight) with epidural analgesia initiated at 1 cm of cervical dilation or at 4 cm of cervical dilation. The X-axis is hours of labor beginning at 1 cm of cervical dilation. (B) Predictions from the labor progression model from full cervical dilation (10 cm) backward through time as actually fit by the model. The X-axis is time before full cervical dilation.

**Fig. 7.** Model of labor progress. (A) Individual post hoc Bayesian fits for the model used to interpolate cervical dilations including epidural effect, and (B) the final post hoc Bayesian estimate for the final model incorporating the effect of Asian ethnicity, neuraxial analgesia, and maternal weight.
PAIN AND PROGRESS OF NULLIPAROUS LABOR

Table 4. Pain Model

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Intersubject Variability</th>
<th>95% Confidence Interval</th>
</tr>
</thead>
<tbody>
<tr>
<td>NRS_{min}, NRS units</td>
<td>±495</td>
<td>0.5–1.6</td>
</tr>
<tr>
<td>NRS_{MAX}, NRS units</td>
<td>8.7</td>
<td>8.5–9.2</td>
</tr>
<tr>
<td>CD_{50}, cm</td>
<td>2.3</td>
<td>2.1–2.6</td>
</tr>
<tr>
<td>(\gamma), non-Asian</td>
<td>4.8</td>
<td>3.3–5.0</td>
</tr>
<tr>
<td>(\gamma), Asian</td>
<td>2.2</td>
<td>1.5–3.1</td>
</tr>
<tr>
<td>Rate scale on (\gamma)</td>
<td>2.3</td>
<td>0.0–3.3</td>
</tr>
</tbody>
</table>

Errors

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Value</th>
<th>95% Confidence Interval</th>
</tr>
</thead>
<tbody>
<tr>
<td>Median error, NRS units</td>
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<td></td>
</tr>
<tr>
<td>Median absolute error, NRS units</td>
<td>1.7</td>
<td></td>
</tr>
</tbody>
</table>

The approximate CV (coefficient of variation), more precisely the standard deviation of the interindividual variability in the log domain.

\(\text{CD}_{50}\) = the cervical dilation associated with 50% of maximal pain; NRS = numerical rating scale; NRS_{MAX} = the maximal reported pain score; NRS_{MIN} = the minimum reported pain score.


however, with this point removed, the effect of cervical dilation rate on the model was no longer statistically significant. The point was left in, and the effect of dilation rate was included in the final model because there was no reason to exclude the observation other than identifying it post hoc as an outlier.

Figure 9 shows the predicted and measured NRS scores from (A) the initial and (B) final model. The improvement with inclusion of the covariates is nearly invisible. The median absolute prediction error was 1.77 with the initial model, and 1.70 with the final model. As described for the labor progress model, even though the covariate effects shown in table 4 are highly statistically significant, they represent trivial improvements in the model.

Figure 10 shows the log likelihood profiles and bootstrap analysis for the parameters of the labor pain model. They notably do not have the smooth parabolic shape of the log likelihood profiles in the labor progress model, reflecting the influence of the steep slope that is sensitive to starting estimates. The curves initially had considerable jaggedness, which is still shown by a representative notch in the NRS_{MAX} profile. These proved to be an artifact of NONMEM’s inability to fully explore the parameter space, were addressed by calculating log likelihood profiles dozens of times, and selecting minimum values that represented the true minimum (or, at least, as close to the true minimum as NONMEM could identify). The 95% confidence intervals from the bootstrap analysis agree well with the log likelihood profiles, with the exception of the rate scalar on \(\gamma\). The lower bound of the bootstrap analysis was very close to 0, which reflects the dependence on that parameter on a single point, circled in figure 8. Indeed, this is a demonstration of how the bootstrap shows robustness of a parameter estimate relative to the data, whereas the log likelihood profile shows the robustness of the parameter estimate relative to the model.

Figure 11 shows the error in (a) the final population pain model and (b) the final post hoc Bayesian individual pain model. The dashed line snaking through the center of the figure is a supersmoother (a moving average, implemented in the R programming language). A bias is evident in the population fit (upper graph) at cervical dilations less than 3 cm. This is related to the prediction of the “typical” baseline NRS pain score of approximately 1, which results in an asymmetric distribution of the prediction error; patients can have pain that is 9 points higher than the prediction for a typical individual, but only one point lower than the prediction for a typical individual. Once the cervix has dilated to 3 cm, the model predicts a pain score of 5 in the typical individual, and error in the prediction becomes symmetrical. The bias is not seen in the predicted pain scores for individual patients (b) because the model for each individual adjusts the predicted pain score when the cervix is not dilated to the actual level of pain when the patient entered the study. The median absolute residual error was 1.7 NRS points for the population model, and 0.95 NRS points for the individual post hoc Bayesian model. The difference between the models shows the magnitude of the still unexplained intersubject variability.

Discussion

Labor is a dynamic process. The biexponential model of labor progress introduced in this paper is a continu-

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ous model suitable for hypothesis testing. The combination of the biexponential labor progress model with our previously described sigmoidal model of labor pain permitted testing the influence of the patient covariates self-identified ethnicity, maternal age, maternal weight, maternal height, birth weight, and gestational age on labor progress and pain. Examining the labors of 500 consecutive nulliparous parturients from 5 self-identified ethnicities, we found that ethnicity and other demographic variables impart highly significant differences in labor progress and labor pain. However, the magnitude of the effects of patient covariates is quite small and is unlikely to have great clinical significance. Our findings do not suggest that targeting a specific self-identified ethnicity is important to reduce variability in future prospective trials of labor pain.

The racial and ethnic identities recorded by our hospital were recommended for use in the 2000 census, where participants were asked to chose one or more of the following categories: American Indian or Alaska Na-

![Fig. 9. Predicted and measured NRS scores.](image)

**A** Initial Model

**B** Final Model

![Log-likelihood profiles: Pain Model](image)

**A** NRSMIN for all subjects, **B** Non-Asian γ-slope function, **C** NRSMAX for all subjects, **D** Asian γ-slope function, **E** CDso for all subjects, and **F** the rate scalar on γ. NONMEM had considerable difficulty calculating the log-likelihood profiles, requiring a local minimum function to remove some of the jaggedness from several curves. The retained jaggedness in the curve for CDso is representative of the unsmoothed curve. CDso = the cervical dilation associated with 50% of maximal pain; NRS = numerical rating scale; NRSMAX = the maximal reported pain score; NRSMIN = the minimum reported pain score.
time before delivery. Potentially consistent with our findings, Greenberg et al. found that both nulliparous and multiparous Black women had a shorter second stage of labor when compared with White women, whereas Asian women experience a longer second stage of labor and higher Cesarean section rates.\textsuperscript{5,11} It is possible that the slower rate of labor in Asians in the active phase may contribute to Cesarean sections for failure to progress. All subjects screened for this study had a vaginal delivery; as such, we do not know whether our Asian and White patients had a higher Cesarean section rate. It is likely that our results are biased to some extent by limiting our population to women who delivered their children vaginally.

We did not study other patient covariates related to ethnicity, such as the country in which a woman was raised, the ethnicity of the partner, the patient’s language, educational status, or attendance at labor educational programs. We do not consider it likely that these covariates would explain the large unexplained intersubject variability in labor progress and labor pain, given the very modest effects of self-identified ethnicity. The more productive line of investigation, in our view, will be to look for genetic polymorphisms that correlate with labor pain and progress.

The rates of both active and latent labor in our cohort are slower than those described by Friedman for nulliparous patients.\textsuperscript{12} Several authors have documented this historical change.\textsuperscript{13,14} Population demographics and the medical management of labor have changed markedly in the years since Friedman reported his results. Particularly, the induction of labor is common, and use of oxytocin has increased and represented 27% and 60% of our sample respectively. While labor induction and oxytocin use did not vary according to ethnicity, it might account for the overall slower progress of labor compared to historical data. The mothers in our study are older and heavier than previously.\textsuperscript{15,16} In our sample, high maternal weight was predictive of slower labor (fig. 6). This association has been noted previously and may contribute to a higher risk of Cesarean delivery in obese women.\textsuperscript{15,16} There may be a direct effect of obesity on the myometrium. Myometrium from obese women taken at Cesarean section contracted with less force and had reduced calcium transients when compared with uterine tissue from lean women.\textsuperscript{17}

We found that the placement of neuraxial analgesia was associated with a decreased rate of labor progress (fig. 6). In retrospective studies, neuraxial analgesia has often been associated with slower labor and a higher rate of Cesarean delivery.\textsuperscript{18} This has typically not been validated in prospective, randomized controlled studies, which suggests that the relationship between neuraxial analgesia and labor slowing is not causal.\textsuperscript{19–23} In addition, studies have correlated early severe labor pain with dystocia\textsuperscript{24–26}, as a result,
a temporal association of neuraxial anesthesia with slowed labor is an expected finding.

The retrospective design of our cohort study imposes significant limitations on consideration of causality. However, our model of the neuraxial analgesia effect permits a modest exploration of causality. In each patient, we estimated the parameters of labor: the active rate constant, the latent rate constant, and the coefficient. As described in the appendix, the model incorporated the effect of neuraxial analgesia as a scalar on time (X axis). If the model accurately captures the biologic effect of epidural anesthesia, then the active rate constant, the latent rate constant, and the coefficient estimated by NONMEM are the values as though neuraxial analgesia had never been placed.

As shown in figure 12, earlier initiation of neuraxial analgesia (greater time) is associated with lower values of the active and latent rate constants, at $P = 0.011$ and $P = 0.024$, respectively. Thus, patients with slower labor (smaller rate constants) received earlier neuraxial analgesia. These data are consistent with, but do not prove, the association of neuraxial analgesia placement with slower labor progress is not causal.

Demographic variables were comparable among groups, except for employment, marital status, and primary language. These variables showed no correlation with labor pain or progress. The interventions used in labor management, including analgesia and oxytocin were also similar among groups, suggesting that there were no systematic differences in treatment based on ethnicity in our population. Previous studies have suggested that differences in Cesarean section rates between Black and White women is related to variability in birth weight. However, we did not observe an association between birth weight and the rate of labor progress.

Asians report less labor pain and have a slower active phase of labor; it is possible that both outcomes may relate to having weaker contractions. In some cases, factors that increase contractility such as oxytocin and placental abruption are also associated with more reported pain.\(^1,6\) Instantaneous labor rate was a significant covariate for labor pain in our study. Although logical and apparently valid, the statistical significance of this finding was dependent on the data from a single Asian patient who had a slow labor and little pain and as such should be taken with caution.

The relationship between ethnicity and other types of pain has been studied in the past.\(^27,28\) Previous studies have shown differences among ethnic groups with respect to stoicism, healthcare quality, and pain coping strategies. Prepared childbirth and breathing techniques have been shown to reduced pain scores in early labor.\(^2,29\) We do not know which patients had professional childbirth preparation; as such, we cannot determine whether this variable contributed to the difference that we have identified.

Our study found that the Asian group reported slightly less painful labor, whereas the Black, Hispanic, and Other groups reported more pain when compared to all patients in other groups. The White patients could be grouped with the Asians if rate were not taken into account. However, even when the Asian group’s slower rate of labor is accounted for, the Asian group still reported less pain then all other patients. Between 3 to 5 cm cervical dilation, there is at least 1.5 NRS difference between the Hispanic-Black-Other groups compared with the Whites-Asian groups. Most epidural anesthetics were administered when the patient had 3–5 cm of cervical dilation. The anesthesiologist might encounter positioning and patient cooperation issues when initiating epidural anesthetics in patients with more pain. Average cervical dilations at epidural analgesia request for the five ethnic groups were not different but the NRS scores varied, suggesting that a more active ap-
proach to pain management might be considered in selected groups.

Interpretation of our results is limited by the fact that the subjects included in the study were from incompletely overlapping time periods. We do not believe that there were any major alterations in obstetrical or nursing protocols during this time period; as such, we do not believe significant bias is introduced. Ninety-four percent of women in our population received analgesia during their labor. As such, there are fewer NRS scores in late labor because we did not consider pain scores after analgesia initiation. As no parturient reported a decrease in pain during labor in the absence of analgesia, women who reported high pain scores in early labor and then requested analgesia would likely have continued to have high pain scores throughout labor. As such, we have likely underestimated NRS_MAX. There was little variability in NRS_MAX. All subjects without analgesia reported significant pain close to full dilation. Similarly, it is possible that women having a very rapid painful labor would be more likely to be rushed to a labor room and have an epidural placed before the nurse could take a pain score with their admission exam. As such, pain might be underrepresented. The impact of the frequent use of epidural analgesia in our population can be evaluated with a similar study in a population with lower use of epidural analgesia. Similarly, the interpretation of our data are affected by informed censoring, in that patients with higher levels of pain are more likely to receive epidural analgesia and have censored observations. Fortunately, a mixed effects approach is fairly robust, even in the presence of informed censoring.

We only have access to pain reports after arrival to the hospital. One reason for coming to the hospital is pain. Women with more pain likely arrive earlier. We might have a greater representation of higher pain scores in early labor. However, this should not confound our analysis of ethnicity as the cervical exam on hospital arrival did not vary among ethnic groups. A prospective study of labor pain with NRS scores starting in earlier labor would help to clarify this issue.

Evidence-based medicine applies the best current evidence in making decisions to guide the care of the individual patient. The practice of pain management in obstetrical anesthesia should be individualized to the needs of each patient. We identified significant variability in both the rates of labor progress and the pattern of labor pain report. However, only a small portion of this variability is explainable by consideration of demographic variables including ethnicity. The rest of the variability may yet be explained by genetic or environmental factors that we have not considered.

No model can be a “final model.” Our models of labor progress and pain are the best that we could achieve with the currently available data. We have used our model to carefully examine the effect of several demographic and labor management-related variables on the progress and pain of labor. Several covariates had highly statistically significant effects, but the effects explained a very small part of intersubject variability in labor progress and pain. Future studies might find that genetic polymorphisms were more important covariates of labor progress and labor pain than the covariates we explored. We have provided our data and the details of our models as Supplemental Digital Content in the hope that other investigators will find it useful for testing hypotheses that may go further to explain the extensive biologic variability.

Appendix: Population Model of Labor Progress

Friedman originally modeled labor progress as a sigmoidal relationship, which was later simplified to a model of two straight lines. The first line is used to describe latent labor, were the cervix dilates at approximately 0.2–0.5 cm/h. The second line describes active labor, where the cervix dilates at 1–2 cm/h. Traditionally, women have been considered to transition from latent to active labor when the cervix is dilated to approximately 4–5 cm.

Figure 13 shows a bilinear model that captures this structure, consisting of two intersecting straight lines. As is usually the case with labor progress models, time runs backwards along the X axis, with 0 being the time of full dilation. The bilinear model has three parameters, M_Latent, the rate (slope) of latent labor, M_Active, the rate (slope) of active labor, and Inflection, the cervical dilation where women transition from latent labor to active labor. The time of the transition from latent to active labor (i.e., the time when the curves intersect) can be readily calculated as (10 – Inflection)/M_Active. The bilinear model is necessarily bounded at 0 and 10, as cervical dilation cannot be negative, and full dilation is defined as 10 cm.
Using NONMEM, we estimated the parameters of the bilinear model from the cervical dilation data in all patients. We estimated both intersubject and intrasubject variability with additive error models. We also used the “first order” method because the “first order conditional estimation” method failed to run. The parameters for each individual patient were estimated using the post hoc step. The population fit of the bilinear model to all of the data are shown in figure 14. There is a considerable amount of variability about the typical prediction, with a median absolute error, \(|\text{measured dilation} - \text{predicted dilation}|\), of 1.0 cm. The goodness of fit is shown in figure 15 for the population estimate (A) and the individual post hoc Bayesian estimates (B). The \(-2\) log likelihood function for the bilinear model is 2741.

Figure 16 shows log likelihood profiles for the three parameters of the bilinear model, the latent slope (A), active slope (B), and inflection point (C). The log likelihood profiles reveal a profound sensitivity of the model to initial parameter estimates, with small changes in the initial estimates resulting in fluctuations in \(-2\) log likelihood of nearly 200 points. This instability is caused by the bilinear model itself, which has an abrupt change at the intersection of the two lines (i.e., at the transition from latent to active labor). Consider an observation immediately to the left of the transition point. A change in either slope, or in Inflection, might move the transition point so that the observation is now to the right of the transition. Suddenly, this data point is being fit to an entirely different line, with unpredictable results. The lack of a smooth transition (or, more precisely, the lack
of a derivative at the transition point) makes the model profoundly sensitive to starting estimates. This profound sensitivity to starting estimates preclude use of the model for hypothesis testing. The bounding of the model at 0 may also contribute to the instability of the model, as the derivative is undefined for all points to the right of the intersection of the line for latent labor with the X axis.

Figure 17 compares the linear model to a sigmoidal model, similar to Friedman’s original model, estimated with NONMEM by using the function

$$\text{Dilation} = CD_0 + (CD_{\min} - CD_0) \frac{\text{Time}^\gamma}{\text{Time}_{50}^\gamma + \text{Time}^\gamma},$$

where $CD_0$ is the cervical dilation at time 0 (typically 10 by definition), $CD_{\min}$ is the minimal cervical dilation (which should be 0, but because women arrive at the hospital somewhat dilated was 0.43 cm in the final model), $\text{Time}$ is the number of hours before full dilation, $\text{Time}_{50}$ is the time of half dilation, and $\gamma$ is the steepness of the transition. The model follows the data better than the simple bilinear model, as suggested by the $-2 \log$ likelihood of 2,499, a decrease of 242 points from the log likelihood for the bilinear model. The sigmoidal model provides for a terminal deceleration in labor progress, which is not evident in the raw data, is virtually invisible in the function, and has been disputed by several investigators.

The data suggest another model. The solid line in figure 18 is a supersmoother function (a moving average, implemented in the R programming language) applied to the data. The best bilinear fit appears as the dashed line. The supersmoother curve suggests a biexponential model, which we implemented with the function $\text{Dilation} = Ce^{-\lambda_2 t} + (10-C)e^{-\lambda_1 t}$. This function has the same number of parameters as the model with two intersecting lines. $\lambda_1$ and $\lambda_2$ are rate constants, with units of inverse time. During latent labor, cervical dilation will double every $0.693/\lambda_2$ hours. During active labor, cervical dilation will double approximately $0.693/\lambda_1$ hours. $C$ can be thought of as approximately the number of centimeters of dilation associated with the active phase of labor. Therefore, 10-C is approximately the number of centimeters of dilation associated with the latent phase of labor, and represents the transition point between latent and active labor. The transition from latent to active labor occurs gradually; therefore, it is probably best to not focus on the value of C or the specific exponents, but rather to consider the function in its entirety. The rate of cervical dilation is the derivative of $\text{Dilation} = Ce^{-\lambda_2 t} + (10-C)e^{-\lambda_1 t}$, with respect to time, which can be calculated as $\text{Rate} = \frac{\partial\text{Dilation}}{\partial t} = -\lambda_1 Ce^{-\lambda_1 t} - \lambda_2 Ce^{-\lambda_2 t}$.

Figure 18 shows the fit of the biexponential model to the data (dotted line). Although the visual improvement is not dramatic, the improvement over the bilinear model is considerable from the perspective of NONMEM: a decrease in the $-2 \log$ likelihood from 2,741 to 2,416, an improvement of 325 points. The $-2 \log$ likelihood of the three-parameter biexponential model is 83 points less than the four-parameter sigmoidal model. Although the models are not nested, and thus cannot be directly compared with the likelihood ratio test, the improvements in $-2 \log$ likelihood strongly support the use of the biexponential model to describe the data, as does the visual congruence of the bilinear model with the nonparametric supersmoother curve. For completeness, we also considered a monocexponential curve, $\text{Dilation} = Ce^{-\lambda t}$. This curve produced a $-2 \log$ likelihood that was 178 points worse than the biexponential model, and was not further considered.
Figure 19 shows the goodness of fit for the population biexponential model (A) and the individual biexponential model (B). The median absolute residual error for the population model is 0.98 cm, indistinguishable from the median absolute residual error of 1.0 cm with the bilinear model.

Figure 20 shows the likelihood profiles for the latent rate constant (A), active rate constant (B), and the coefficient (C). The smooth shape demonstrates the correct behavior for a model useful for hypothesis testing. The dashed lines show the change in the $-2 \log$ likelihood that would justify inclusion of an additional parameter at $P = 0.05$ and $P = 0.01$.

We estimated the 95% confidence for each parameter in the biexponential model by performing 1,000 bootstrap replicates with replacement using PLT Tools. The 95% confidence interval was calculated by using an Excel spreadsheet as the 2.5% and 97.5% values for each parameter from the 1,000 replicates. The 95% confidence intervals for each parameter are included in figure 20. Because of the different methodologies (i.e., each bootstrap analysis considers a resampled population, not the same data set as used in calculating the $-2 \log$ likelihood profile), it is an expected result that the 95% confidence intervals from the bootstrap analysis do not exactly match the intervals suggested by the $-2 \log$ likelihood profiles.

The slope of the biexponential function $\text{Dilation} = C e^{-\lambda_1 t} + (10-C)e^{-\lambda_2 t}$ can be calculated as the derivative with respect to time: $\text{Rate(cm/h)} = \lambda_1 C e^{-\lambda_1 t} + \lambda_2 (10-C) e^{-\lambda_2 t}$. Figure 21 shows the rate of cervical dilation per hour (A) and the rate of dilation as a function of cervical dilation (B).

Given the visual similarity of the biexponential model to the supersmooth curve, the improved quality of the fit of the biexponential model compared to the bilinear model (325 points) and sigmoidal model (83 points), the stability demonstrated in the likelihood profiles, and the confirmation of the approximate confidence intervals using bootstrap analysis (fig. 20), we used the biexponential model for testing the relationship among self-identified ethnicity, labor progress, and labor pain.

We considered two types of covariates in the analysis: time invariant covariates (covariates that did not change over the course of labor) and time variant covariates (covariates that occurred during the labor). The time invariant covariates were patient age, weight, height, gestational age, birth weight, and self-reported ethnicity. We modeled the time invariant covariates as simple linear adjustments to $\lambda_1$, $\lambda_2$, and $C$.

The time variant covariates were institution of epidural anesthesia, an oxytocin infusion, labor induction, and rupture of membranes. We could not model these as simple linear adjustments to $\lambda_1$, $\lambda_2$, and $C$; that approach would produce two distinct curves, with an abrupt discontinuity in predicted cervical dilation at the moment of transition. We could have used a mathematical function to constrain the model to a smooth function at the moment of a time-varying covariate, but we could find no precedent for that approach nor an intuitively tractable mathematical model. Instead, we adopted a very simple approach that ensured a smooth transition. We introduced a "time adjustment" factor that accelerated (or decelerated) the time axis at the transition moment. This required introducing only a single term, which represented how the time-varying covariate accelerated (factor $> 1$) or decelerated (factor $< 1$) the progress of labor. The factor, $\theta$, was defined as the time interval from the moment of the intervention until 10 cm of dilation in the absence of the intervention divided by the time interval from the moment of the intervention until 10 cm of dilation in the presence of the intervention. To express it more formally, let $T_{\text{Observed}}$ be the actual time between the intervention and full dilation (which is the same as the time of the intervention) and $T_{\text{NoIntervention}}$ be expected time if the person had not had the intervention. We define the
time scale factor, \( \theta \), as:

\[
\theta = \frac{T_{\text{NoIntervention}}}{T_{\text{Observed}}}.
\]

If \( \theta < 1 \), then \( T_{\text{Observed}} \) is greater than \( T_{\text{NoIntervention}} \) and labor is slowed. For example, \( \theta = 0.6 \), then labor runs at only 60\% of the expected pace after an intervention. If \( \theta > 1 \), then \( T_{\text{Observed}} \) is less than \( T_{\text{NoIntervention}} \) meaning that labor is accelerated by the intervention. For example, if \( \theta = 2 \), then the pace of labor is doubled following the intervention.

The labor model is represented as a biexponential function of time, \( t \). The model runs backwards in time, with \( t = 0 \) representing the time of full dilation. Any intervention scales the time axis from the moment of the intervention until full dilation, which is when \( t = 0 \). Thus, the presence of an intervention such as epidural placement requires recalculation of all values of \( t \) to reflect the acceleration or deceleration of labor. This requires the introduction of two terms, \( t_{\text{unscaled}} \), which is the time recorded in the study, and \( t_{\text{scaled}} \), which is a scaled time that has expanded or contracted from the intervention, and is the value of time used in the labor progress model. The calculation of \( t_{\text{scaled}} \) can be derived from the definition of \( \theta \).

Before the intervention, \( t_{\text{scaled}} \) must include the full impact of the intervention on the time course. Based on the definition of \( \theta \), \( T_{\text{NoIntervention}} = \theta \times T_{\text{Observed}} \). The full impact is the difference between the observed time, \( T_{\text{Observed}} \), and the expected time in the absence of the intervention, \( \theta \times T_{\text{Observed}} \). Thus, \( t_{\text{scaled}} = t_{\text{unscaled}} + \theta \times T_{\text{Observed}} - T_{\text{Observed}} = t_{\text{unscaled}} + T_{\text{Observed}}(\theta - 1) \).

At the moment of the intervention, \( t_{\text{scaled}} = T_{\text{NoIntervention}} \) and \( t_{\text{unscaled}} = T_{\text{Observed}} \). By the definition of \( \theta \), \( T_{\text{NoIntervention}} = \theta \times T_{\text{Observed}} \); therefore, at the moment of the intervention \( t_{\text{scaled}} = t_{\text{unscaled}} \times \theta \). This relationship holds after the intervention as well: \( t_{\text{scaled}} = t_{\text{unscaled}} \times \theta \).

Figure 22 shows the effect of the model. The top figure 22A, in which time goes forward, shows the effect of an epidural placed at 16 h and \( \theta = 0.66 \). The course of labor is abruptly slowed from that time of epidural placement, so that the woman reaches full dilation approximately 4 h later than had the epidural not been placed. The lower figure 22B represents the data as seen from the model, in which time runs backwards from the point of full dilation. Only 24 h of labor is shown. The woman with the
The parameters of the models explored in this appendix were estimated by NONMEM by using the “first order” method. This was necessary because the extreme sensitivity of the bilinear model to initial estimates precluded using the “first order conditional estimates” approach. In this way, the appendix compares models estimated with exactly the same methodology. This differs from the model development in the article text, where only “first order conditional estimates” were used.

References


24. Panni MK, Segal S. Local anesthetic requirements are greater in dystocia than in normal labor. Anesthesiology 2003; 98:957–63


