Bayesian Population Decoding of Motor Cortical Activity Using a Kalman Filter

Wei Wu
weiwu@dam.brown.edu
Yun Gao
gao@dam.brown.edu
Division of Applied Mathematics, Brown University, Providence, RI 02912, U.S.A.

Elie Bienenstock
elie@dam.brown.edu
Division of Applied Mathematics and Department of Neuroscience, Brown University, Providence, RI 02912, U.S.A.

John P. Donoghue
john_donoghue@brown.edu
Department of Neuroscience, Brown University, Providence, RI 02912, U.S.A.

Michael J. Black
black@cs.brown.edu
Department of Computer Science, Brown University, Providence, RI 02912, U.S.A.

Effective neural motor prostheses require a method for decoding neural activity representing desired movement. In particular, the accurate reconstruction of a continuous motion signal is necessary for the control of devices such as computer cursors, robots, or a patient’s own paralyzed limbs. For such applications, we developed a real-time system that uses Bayesian inference techniques to estimate hand motion from the firing rates of multiple neurons. In this study, we used recordings that were previously made in the arm area of primary motor cortex in awake behaving monkeys using a chronically implanted multielectrode microarray. Bayesian inference involves computing the posterior probability of the hand motion conditioned on a sequence of observed firing rates; this is formulated in terms of the product of a likelihood and a prior. The likelihood term models the probability of firing rates given a particular hand motion. We found that a linear gaussian model could be used to approximate this likelihood and could be readily learned from a small amount of training data. The prior term defines a probabilistic model of hand kinematics and was also taken to be a linear gaussian model. Decoding was performed using a Kalman filter, which gives an efficient recursive method for Bayesian inference when the likelihood and prior are linear.
and gaussian. In off-line experiments, the Kalman filter reconstructions of hand trajectory were more accurate than previously reported results. The resulting decoding algorithm provides a principled probabilistic model of motor-cortical coding, decodes hand motion in real time, provides an estimate of uncertainty, and is straightforward to implement. Additionally the formulation unifies and extends previous models of neural coding while providing insights into the motor-cortical code.

1 Introduction

Recent research on developing neural motor prostheses has demonstrated the feasibility of direct neural control of computer cursor motion and other devices using implanted electrodes in nonhuman primates (Wessberg et al., 2000; Serruya, Hatsopoulos, Paninski, Fellows, & Donoghue, 2002; Taylor, Helms Tillery, & Schwartz, 2002; Carmena et al., 2003). These results are enabled by a variety of mathematical decoding methods that produce an estimate of the subject’s state (e.g., hand position) from a sequence of measurements (e.g., the firing rates of a population of cells). A number of algorithms have been proposed for decoding extracellularly recorded neural firing activity in the arm area of primary motor cortex (MI) to perform off-line reconstruction of hand motion or online control of cursors or robotic devices (see Schwartz, Taylor, & Helms Tillery, 2001; Serruya, Hatsopoulos, Fellows, Paninski, & Donoghue, 2003, for a brief overview). Here we pose this problem as one of Bayesian inference in which the goal is to estimate the a posteriori probability of hand kinematics conditioned on an observed sequence of firing rates. The Bayesian approach formulates this posterior probability as the product of a likelihood term and an a priori probability. The likelihood term models the probability of the firing rates given the current hand motion and can be learned from training data. The prior combines a model of how the hand moves over time with an estimate of the kinematics at the previous time instant. The Kalman filter (Gelb, 1974; Kalman, 1960) provides an efficient recursive algorithm to optimally estimate the posterior probability when the likelihood and prior models are linear and gaussian.

Previous methods for decoding MI activity include the population-vector algorithm (Georgopoulos, Schwartz, & Kettner, 1986; Moran & Schwartz, 1999a, 1999b; Schwartz & Moran, 1999; Taylor et al., 2002), linear filtering (Paninski, Fellows, Hatsopoulos, & Donoghue, 2004; Sanchez et al., 2003; Serruya et al., 2002; Wessberg et al., 2000), and artificial neural networks (Wessberg et al., 2000). Each of these methods can be viewed as a direct method that attempts to estimate the hand kinematics \( x \) as a function of the neural firing \( z \), that is,

\[
x = f_1(z).
\]
In contrast, most models of neural coding can be viewed as generative models where the neural activity is a function of a behavior or stimulus $x$, that is,

$$z = f_2(x) + \text{noise},$$

where the noise might be assumed to be Poisson. The Bayesian approach presented here provides a clear and rigorous way of taking generative models of neural encoding and exploiting them to perform decoding.

Previous authors have explored the relationship between firing rates in MI and various aspects of hand motion (position, direction, speed, velocity, or acceleration) (Kettner, Schwartz, & Georgopoulos, 1988; Georgopoulos et al., 1986; Moran & Schwartz, 1999b; Flamet & Hore, 1988). While previous studies have typically viewed these behavioral variables in isolation, we found that decoding performance is improved when the encoding model simultaneously takes into account all these variables. This suggests the need for a richer model of neural coding than is typically considered. Additionally, our results demonstrate the importance of modeling correlated noise in the firing rates of multiple cells. Decoding performance drops significantly when cells are assumed to be conditionally independent.

Much of the prior work on motor cortical decoding has focused on relatively constrained “center-out” motions rather than the continuous motions considered here (Paninski et al., 2004). To cope with continuous motion, we adopt a simple prior model of hand motion that, in contrast to previous decoding methods, explicitly models the temporal evolution of the hand kinematics. Bayesian methods have been exploited previously to infer the 2D location of a rat from hippocampal place-cell activity (Brown, Frank, Tang, Quirk, & Wilson, 1998; Twum-Danso & Brockett, 2001; Zhang, Ginzburg, McNaughton, & Sejnowski, 1998). The application of Bayesian decoding to motor cortical data was proposed in Gao, Black, Bienenstock, Shoham, & Donoghue, (2002) with various Kalman filter formulations being recently studied (Sanchez, Erdogmus, Principe, Wessberg, & Nicolelis, 2002; Wu, et al., 2002, 2003). Some of the results in this letter were previously reported in Wu et al. (2003).

The Kalman filter has a number of desirable properties for motor cortical decoding. The inclusion of prior information about the system state enables an efficient recursive formulation of the decoding algorithm and effectively smooths noisy estimates in a mathematically principled way; this is particularly important for decoding complex, natural hand motions required for neural motor prostheses. We reconstructed hand trajectories from pre-recorded neural firing rates and found that the Kalman filter method was more accurate than previous approaches while also being computationally efficient. The detailed application of the method provides insight into neural coding in MI and is useful for examining optimal time lags between
spiking activity and hand movement, the accuracy of different models of hand kinematics, the contributions of different neural population sizes, and the effect of temporal bin sizes for estimating neuronal firing rate. We describe the implementation and structure of a Kalman filter method that is computationally efficient to learn, requires little training data, provides real-time decoding, is applicable to the complex natural motions, and thus seems well suited to prosthetic applications.

The structure of this letter is as follows. Section 2 summarizes the experimental paradigm used previously to obtain the neural recordings. This section also introduces the linear gaussian model of motor cortical activity, our Bayesian framework, the underlying statistical assumptions, the Kalman filter decoding algorithm, and an approach for estimate optimal time lags. Section 3 describes the decoding results as well as experimental results related to various modeling choices that are important for accurate decoding. It also compares the Kalman filter with previous decoding methods (the linear filter and population vector methods). Section 4 discusses related work and section 5 offers conclusions. The appendix provides the mathematical details of the Kalman filter algorithm, a comparison with the Wiener filter, and a few additional algorithmic and modeling details with associated experimental results.

2 Materials and Methods

2.1 Experimental Methods. The neural data used here were prerecorded and have been described elsewhere (Paninski et al., 2004; Serruya et al., 2002). Briefly, after initial task training, two macaque monkeys were implanted with silicon microelectrode arrays containing 100 platinized-tip probes (Cyberkinetics Inc., Foxboro, MA). Details of the array and recording protocols are described elsewhere (Maynard, Nordhausen, & Normann, 1997; Maynard et al., 1999). The devices were implanted in the arm area of primary motor cortex (MI) (see Donoghue, Sanes, Hatsopoulos, & Gaal, 1998, for details). All procedures were in accordance with protocols approved by Brown University Institutional Animal Care and Use Committee. Signals were amplified and digitized using commercial hardware (Plexon Inc., Dallas TX). As is common practice in the literature, waveforms crossing experimenter-determined thresholds were further processed to detect action potentials; the details differed for each of the two behavioral tasks described below. Action potentials were then counted within fixed time windows (bins), and the firing rate (number of spikes per unit time) within each bin was computed for each neuron. All encoding and decoding analysis was performed using these discrete approximations to the firing rate.

The behavioral paradigms for the two tasks below are described in Paninski et al. (2004) and Serruya et al. (2002). In each task, the monkey viewed a computer monitor while continuously moving a manipulandum on a 30 cm × 30 cm tablet (with approximately a 25 cm × 25 cm workspace).
that was parallel to the floor. The position of the manipulandum (hand position) controlled the 2D motion of a feedback cursor on the monitor. The hand position and neural activity were recorded simultaneously. In addition to hand position, we computed derivatives of the position using finite differences; these approximated velocity, acceleration, and higher-order hand kinematics. For example, given a time series of positions \((x_k, y_k)\) at time \(t_k\), we approximated the velocity, \((v_{x,k}, v_{y,k})\) as \((\frac{x_k - x_{k-1}}{\Delta t}, \frac{y_k - y_{k-1}}{\Delta t})\) (where \(\Delta t\) is the time step length). It is well known that this approach results in noisy estimates of the derivatives with the effects of noise being more pronounced in the higher derivatives. Consequently, we also experimented with using splines to smoothly interpolate the position data. Differentiating these splines produced less noisy derivatives but did not significantly improve decoding performance. It also increased the complexity of the method and complicated real-time decoding. Consequently, in all further analysis we used the simple, discrete, derivative approximations to represent the hand kinematics.

**Pursuit Tracking Task.** The pursuit tracking task was clearly described in Paninski et al. (2004). Briefly, a target dot moved slowly on the monitor, and the behavioral task required moving the feedback cursor with the manipulandum so that it tracked the target within a given distance range. On each trial, the target motion followed a unique random walk from a different random starting location. Each trial ended when the dot was out of the tracking range and lasted at most 10 seconds, with the majority of trials lasting approximately 8 or 9 seconds. Short trials, in which the monkey was unable to track the target for more than 5 seconds, were judged unsuccessful and were not considered. Our subsequent analysis was based on the remaining 182 trials. The 2D histograms of the hand position, velocity, and acceleration over all trials are shown in Figure 1 (first row). Note that these distributions are significantly different from those obtained during simple, stylized, movements found in center-out reaching tasks (Taylor et al., 2002). While the hand motions were more “general” than those in stereotyped reaching tasks, the motion was still constrained to follow a particular path.

After thresholding, detected waveforms were analyzed off-line using commercial software (Plexon Inc., Dallas TX). Twenty-five well-isolated individual units (neurons) were detected (Serruya et al., 2003), and the firing rate for each unit was computed in nonoverlapping 50 ms time bins. The hand kinematics were subsampled to match the 50 ms time intervals.

**Pinball Task.** The pinball task (Serruya et al., 2002) was designed to test a direct neural control task and differed from the pursuit tracking task in that the target did not move continuously but rather appeared in random locations on the monitor. The monkey was required to move the feedback dot with the manipulandum to “hit” the target (within a
Figure 1: Normalized, log 2D histograms of kinematics for both the pursuit tracking task (first row) and the pinball task (second row). These plots show the log prior probability of the position, velocity, and acceleration of the hand.

prespecified distance). When the target was acquired, it disappeared and then reappeared in a new random location. Each time the target appeared, the monkey moved to hit the new location. The motions made by the monkey on the 2D plane were less constrained than in the pursuit tracking task since the exact motion used to reach the targets was under the control of the subject.

From this experiment, we obtained two sets of trials: one was approximately 3.5 minutes in length and was used as training data to learn our encoding model; the other was approximately 1 minute in length and was used as test data for decoding. The 2D histograms of position, velocity, and acceleration of all data are shown in Figure 1 (second row). Note that the distribution over position is more uniform than in the pursuit tracking task. Also note that the magnitude of the velocity and acceleration of the hand was significantly higher in this task.

The recording of hand motion and the approximation of the temporal derivatives (velocity, acceleration, and so forth) were exactly the same as in the pursuit tracking task. The waveforms, however, were sorted online into units using manually set thresholds without a separate off-line sorting process. All the waveforms crossing the thresholds were treated as action
potentials from a single unit, potentially resulting in multiunit data. The firing rate was computed for each such unit in 70 ms time bins, and there were 42 such units for this task.

The firing rates of the cells were significantly higher than in the pursuit tracking task (likely due to the faster hand motion). Quantitatively, the average hand speeds were approximately 14.67 cm/s (pinball) and 2.88 cm/s (pursuit tracking), while the average firing rates over all cells were approximately 30 spikes/s (pinball) and 10 spikes/s (pursuit tracking).

2.2 Statistical Methods. Our focus here is on a probabilistic, Bayesian approach for inferring hand movement from the firing rate of neurons in MI. We want our approach to (1) have a sound probabilistic foundation, (2) explicitly model noise in the data, (3) indicate the uncertainty in estimates of hand position, (4) make the statistical assumptions about the data explicit, (5) require a minimal amount of “training” data, (6) provide online estimates of hand position with short delay (less than 200 ms); and (7) provide insight into the neural coding of movement. To that end, we developed a Kalman filtering method (Gelb, 1974; Welch & Bishop, 2001) that provides a rigorous and well-understood framework that addresses these issues. This approach provides a control-theoretic model for the encoding of hand movement in motor cortex and for inferring, or decoding, this movement from the firing rates of a population of neurons. The approach generalizes and extends previous coding models.

2.2.1 Modeling Neural Coding of Hand Kinematics. Georgopoulos, Kalaska, Caminiti, and Massey (1982) observed that the firing rate of cells in MI were approximated by a cosine “tuning function.” In particular, the firing rate, $z_k$, of a cell at some time $t_k$ is related to movement direction, $\theta_k$, by

$$z_k = h_0 + h_p \cos(\theta_k - \theta_p),$$

(2.1)

where $\theta_p$ is the cell’s “preferred” direction (i.e., the direction of maximal response) and $h_0$ and $h_p$ are scalar constants. Equivalently, this can be expressed as

$$z_k = h_0 + h_1 \sin(\theta_k) + h_2 \cos(\theta_k),$$

(2.2)

where $h_1, h_2$ are scalar parameters that can be fit to training data.

The above model has formed the foundation for much of the analysis of motor cortical encoding of motion. For general prosthetic applications, however, this model is insufficient as it relates neural activity only to movement direction. Since it does not capture the full kinematics of hand motion, decoding using this approach has focused on center-out tasks, where movement direction is the key component of the motion.
Moran and Schwartz (1999b) extended the above model to include the speed, $||v||$, of the hand,

$$z_k = h_0 + ||v||(h_x \sin(\theta_k) + h_y \cos(\theta_k)).$$  \hspace{1cm} (2.3)

This is equivalent to modeling the firing rate as a linear function of velocity in the $x$ and $y$ coordinates,

$$z_k = h_0 + h_x v_{x,k} + h_y v_{y,k},$$  \hspace{1cm} (2.4)

where $v_{x,k}$ and $v_{y,k}$ represent the hand velocity in the $x$ and $y$ directions, respectively, at time $t_k$.

A similar linear model was proposed to relate firing rate and hand position (Kettner et al., 1988),

$$z_k = f_0 + f_x x_k + f_y y_k,$$  \hspace{1cm} (2.5)

where $x_k$ and $y_k$ represent hand position and $f_0$, $f_x$, $f_y$ are the linear coefficients that are fit to training data.

We found that linear models of position and velocity (see equations 2.5 and 2.4, respectively) provided reasonable approximations to our data. In the pursuit tracking data, 23 of the total 25 cells are appropriately characterized by equations 2.5 and 25 are by equations 2.4 (multiple regression, $F$ test, $p < 0.05$). In the pinball data, these numbers are 39 and 41 of the total 42 cells (multiple regression, $F$ test, $p < 0.05$). Some examples of linear fits are shown in Figure 2 for illustration. In addition to position and velocity, the firing rate has been shown to be related to hand acceleration (Flament & Hore, 1988).

Based on this previous work, we assume (for now) that the population activity is related to the position, velocity, and acceleration of the hand (this will be verified and extended later). We then define the system state to be a six-dimensional vector $x_k = [x, y, v_x, v_y, a_x, a_y]^T$ representing the $x$-position, $y$-position, $x$-velocity, $y$-velocity, $x$-acceleration, and $y$-acceleration of the hand at time $t_k = k \Delta t$ where $\Delta t = 70$ ms (pinball task) or 50 ms (pursuit tracking task) in our experiments. Other models of the hand kinematics are possible and are explored in the experimental results.

Below, we show how to estimate this system’s state in a principled way that extends previous work, incorporates an explicit noise model, and models correlations between the activity of different cells.

### 2.2.2 Bayesian Formulation

The above models all linearly relate components of the system state to the firing rates of individual neurons. Generalizing this idea, let observations $z_k \in \mathbb{R}^C$ represent a $C \times 1$ vector containing the firing rates at time $t_k$ for $C$ observed neurons within a $\Delta t$ time interval.
Figure 2: Empirical tuning functions and their linear approximation. The top two rows show data and models from the pursuit tracking task, while the bottom two rows illustrate the pinball data. For each task, the first row shows empirical firing rates, and the second row shows the linear fit to these data. The empirical plots show the mean firing rate as a function of position (left two columns) or velocity (right two columns). The darkest blue areas correspond to kinematics that were never observed. The color coding (blue through red) represents the mean firing rate observed for a discrete region in the parameter space. The linear fit to these data is computed during the training of the Kalman filter model. The linear fit is seen to provide a crude but reasonable approximation to the raw data.

Let $\mathbf{z}_k = [\mathbf{z}_1, \mathbf{z}_2, \ldots, \mathbf{z}_k]^T$ represent the history of measurements up to time bin $k$.

We pose the problem of estimating the system state as one of Bayesian inference. Let $p(\mathbf{x}_k | \mathbf{z}_k)$ be the a posteriori probability of the system state conditioned on the measurements. We make two Markov assumptions:

$$p(\mathbf{x}_k | \mathbf{x}_{k-1}, \mathbf{x}_{k-2}, \ldots, \mathbf{x}_1) = p(\mathbf{x}_k | \mathbf{x}_{k-1}) \quad (2.6)$$
These state that, given the hand kinematics at time $k - 1$, the hand kinematics at time $k$ is conditionally independent of the previous hand motions and that, conditioned on the current state, the firing rates are independent of the firing rates at previous time instants. Then, using Bayes’ theorem and simple algebra, we can write the posterior probability as

$$p(x_k | z_k) = \kappa \int p(z_k | x_k) p(x_k | x_{k-1}) p(x_{k-1} | z_{k-1}) \, dx_{k-1},$$

(2.8)

where $p(z_k | x_k)$ is called the likelihood of the state, $p(x_k | x_{k-1})$ is a temporal prior that models how the state evolves from one time instant to the next, and $p(x_{k-1} | z_{k-1})$ is simply the posterior probability at the previous time instant. The term $\kappa$ is a normalizing term, independent of $x_k$, which ensures that posterior integrates to 1.

Decoding then involves estimating the posterior probability, $p(x_k | Z_k)$, at each time instant, which we can do recursively using equation 2.8. Having a representation of the full posterior has advantages over methods that estimate $x_k$ with no representation of uncertainty. Given the posterior, one can compute an estimate of $x_k$ in a variety of standard ways. For example, one can compute the expected value of $x_k$, $E[x_k | Z_k]$, or the value that maximizes $p(x_k | Z_k)$ resulting in a maximum a posteriori (MAP) estimate. In the general case, the posterior probability, $p(x_k | Z_k)$, can be an arbitrary, non-gaussian, multimodal distribution (Gao et al., 2002; Cisek & Kalaska, 2002), and the integral in equation 2.8 can be numerically approximated using Monte Carlo integration techniques (Brockwell, Rojas, & Kass, 2004; Gao et al., 2002; Shoham, 2001). To achieve a real-time decoding algorithm, we assume that the likelihood and the prior are both gaussian, and this leads to a closed-form recursive solution for estimating the posterior (which is also gaussian); this is known as the Kalman filter (Kalman, 1960; Gelb, 1974; Welch & Bishop, 2001).

To fully specify the decoding model, we must define the likelihood, the temporal prior, and the algorithm for estimating the posterior. These are described below.

**Likelihood Model.** The likelihood relates the hand kinematics to the neural firing rates. We begin by defining a generative model for the activity of the population as

$$z_k = H_k x_k + q_k,$$  

(2.9)
where $k = 1, 2, \ldots, M$, $M$ is the number of time steps in the trial, and $H_k \in \mathbb{R}^{C \times 6}$ is a matrix that linearly relates the six-dimensional hand state to the firing rates. We assume that the noise in the observations is zero mean and normally distributed with covariance $Q_k$, that is, $q_k \sim N(0, Q_k)$, $Q_k \in \mathbb{R}^{C \times C}$.

Note that the assumption of zero-mean gaussian noise in equation 2.9 is applicable only to centralized (zero-mean) firing rates. The raw data are neither zero mean nor truly gaussian. Consequently, before processing the firing-rate data, they were square-root transformed (Maynard et al., 1999; Moran & Schwartz, 1999b) to make them better modeled by a gaussian. This preprocessing step is not absolutely necessary and improves decoding performance only slightly; nevertheless, we will assume square-root-transformed firing rates in the remainder of the article. We then centralized the firing data as well as the hand kinematics so that both had zero mean; this was done by computing the mean firing and mean kinematics in the training set and subtracting this from the data in both the training and test sets.

Previous work showed that the correlation in MI neurons is important for the encoding of movement parameters (Fetz, Toyama, & Smith, 1991; Hatsopoulos, Ojakangas, Paninski, & Donoghue, 1998). Consequently, we take $Q_k$ to be a full covariance matrix to model correlated noise in the firing rates. Specifically, noise here results from errors in the predictions from the generative model. This formulation of an explicit generative model with an explicit noise term generalizes previous work. In our experiments, we found that the full system state and full covariance matrix produced the most accurate decoding results. The previous models above can be viewed as using a reduced system state and a diagonal covariance matrix. These simplified models resulted in degraded performance. This will be quantitatively verified later for both tasks.

**Temporal Prior.** By modeling how the system state is expected to evolve over time, the temporal prior can reduce the effects of noise and smooth the estimates in a mathematically principled way. We take the simple approach of assuming that the state propagates in time according to a linear gaussian model,

$$x_{k+1} = A_k x_k + w_k,$$

(2.10)

where $A_k \in \mathbb{R}^{6 \times 6}$ is the coefficient matrix, and the noise term $W_k \sim N(0, W_k)$, $W_k \in \mathbb{R}^{6 \times 6}$. As in the case of the measurement model, $W_k$ is taken to be a full covariance matrix. Equation 2.10 states that the hand kinematics (position, velocity, and acceleration) at time $k + 1$ is linearly related to the state at time $k$.

This is similar to the system model used in Brown et al. (1998) for estimating a rat’s position from the firing rates of hippocampal place cells. In contrast, here we also model higher-order hand kinematics (velocity and
acceleration). While more complex, nonlinear, dynamical models could also be exploited, our focus here is on the likelihood term, which represents our model of the neural code.

2.2.3 Learning and Decoding with the Kalman Filter. In practice, $A_k$, $H_k$, $W_k$, $Q_k$ may vary with time $t_k$; however, we make the common simplifying assumption that they are constant (independent of $k$). Thus, we can estimate all the constant parameters $A$, $H$, $W$, $Q$ from training data by maximizing the joint probability $p(X_M, Z_M)$, where both the hand kinematics $X_M = [x_1, x_2, \ldots, x_M]^T$ and the firing rates $Z_M$ are known for the $M$ time instants in the training set. Given our first-order Markov assumptions, the joint probability distribution over states $X_M$ and firing rates $Z_M$ is

$$p(X_M, Z_M) = \left[ p(x_1) \prod_{k=2}^{M} p(x_k | x_{k-1}) \right] \left[ \prod_{k=1}^{M} p(z_k | x_k) \right].$$

This is simply the product of the prior hand state $p(X_1)$ at the first time instant, the probability of each new state conditioned on the previous one, and the likelihood at each time instant. Given training data, we maximize this probability with respect to $A$, $H$, $W$, $Q$, as described in the appendix.

Decoding then involves reconstructing (or inferring) the system state at each time instant given the prior estimate of the state and the new measurements of neural firing. Since the measurement and system equations, 2.9 and 2.10, are both linear and gaussian, decoding can be performed using the Kalman filter (Kalman, 1960). The details of the algorithm for recursive Bayesian inference are provided in the appendix. The appendix also outlines the relationships between the Kalman filter, traditional linear filtering methods, and the Wiener filter.

2.3 Estimating the Optimal Lag. The physical relationship between neural firing and arm movement implies the existence of a time lag between them (Moran & Schwartz, 1999b; Paninski et al., 2004). If an “optimal lag” can be found, it should improve the model’s encoding ability and the accuracy of the decoding. Introducing a time lag in the model means that to estimate the state $x_k$ at time $t_k$, we should consider measurements, $z_{k-i}$, at some previous (or future) instant in time $t_{k-i}$ for some integer $i$.

2.3.1 Uniform Lag. The simplest assumption is that all cells exhibit the same lag. Finding the optimal lag then involves fitting the Kalman model for a variety of integer values $i$ and choosing the one that gives the best encoding or decoding performance. Since we can easily bound the range of possible lags, this search is straightforward to perform.
In our experiments, the data were binned into 70 or 50 ms time bins. We found that a uniform lag of two or three time bins, corresponding to 140 or 150 ms, produced the most accurate decoding results. This result is similar to Moran and Schwartz (1999b) where 145 ms was chosen as the average time lag between firing activity and hand velocity.

2.3.2 Nonuniform Lag. We found, however, that the best decoding results were obtained by allowing each cell to have its own lag (within a predefined range of possible lags consistent with known lags for cells in MI). To deal with different lags for each cell, we extend our notation: let \( l_i \in \{0, 1, \ldots, L\} \) be the lag of the \( i \)th cell, \( i = 1, 2, \ldots, C \) (\( C \) is the total number of cells). Let \( \{l_j\} = \{l_1, \ldots, l_C\} \) be some set of lag times for the \( C \) units. As suggested by the optimal 140 or 150 ms uniform time lag for both tasks, we took the maximum lag to be \( L = 4 \) in the pinball task (corresponding to 0 ms \( \leq \) lag \( \leq 280 \) ms) and \( L = 5 \) in the pursuit tracking task (corresponding to 0 ms \( \leq \) lag \( \leq 250 \) ms). The \( k \)th firing-rate vector is \( z_{i,k} = (z_{1,k}, z_{2,k}, \ldots, z_{C,k}) \), in which each \( z_{i,k} \) is the firing rate of cell \( i \) at time step \( k - l_i \). For each possible assignment, \( \{l_j\} \), of lags to cells, one could train the Kalman filter model. The Kalman filtering algorithm generates the error covariance matrix \( P_k \) (for \( k \) large enough, it is approximately constant). Letting \( mse(\{l_j\}) \) be the sum of the first two components on the main diagonal of \( P_k \) (equivalent to the mean-squared error of position), our goal is to find the optimal assignment of lags to cells \( \{l_j\} \), that is,

\[
\arg\min_{\{l_j\}=\{l_i\in\{0,\ldots,L\};i=1,2,\ldots,C\}} mse(\{l_j\}).
\]

A brute force search of all possible combinations of lags would require estimating the Kalman model for \( L^C \) possibilities. This is impractical, so we instead devise a fast, randomized, greedy searching approach, which is able to obtain very stable approximations to the desired time lags. The algorithm is sketched in Table 1.

The algorithm works by optimizing the lag time for cells individually; that is, it solves for the lag of one cell while holding the lags of all the other cells fixed. The algorithm then cycles through all the cells in a random order, updating their lag in this way. This process is repeated multiple times, and we found that it converges quickly in practice (after three or four passes through the cells).

This algorithm requires that the Kalman filtering algorithm be applied to the training data only \( LRC \) times. In our experiments, we took the number of iterations, \( R \), to be five. In the pinball experiment, for example, the number of cells, \( C \), was 42, resulting in a computational cost that was much lower than the \( L^C \) operations required for exhaustive search.
Table 1: Greedy Algorithm for Estimating Individual Lag Times for Each Cell.

1. Randomly choose initial lag $l_i \in \{0, 1, \ldots, L\}$ for each cell $i = 1, 2, \ldots, C$.
2. For iteration $t = 1$ to $R$
   \begin{itemize}
   \item Randomize the order in which cells are considered
   \item to minimize effects of dependencies between cells
   \end{itemize}
   For $C$ iterations
   select a cell index $c$ at random from $\{1, \ldots, C\}$ without replacement
   hold all other lags constant (i.e. $l_m, m \neq c$).
   Update $l_c$ by minimizing:
   $$l_c = \arg\min_{l_c \in \{0, 1, \ldots, L\}} \text{mse}(\{l_1, \ldots, l_c, \ldots, l_C\}).$$
3. Return the final set of values $\{l_k\}$.

3 Results

The Kalman filter is well known, and its implementation is quite standard. Our focus here is on the development of this method for neural prosthetic applications. This application to neural decoding requires a number of modeling choices, which are explored below in detail. Optimizing these modeling choices may provide insight into neural coding in MI. Below, we report results for the two different continuous hand-motion tasks described in section 2 on two different animals.

The accuracy of the reconstructions is reported using two different criteria: the correlation coefficient ($CC$, describing the similarity) and the mean squared error ($MSE$, describing the Euclidean distance) between the reconstructed and true hand trajectories. Assume $\left(\hat{x}_t, \hat{y}_t\right)$ is the estimate for the true position $\left(x_t, y_t\right)$, $t = 1, \ldots, T$. Then $MSE$ and $CC$ are defined as follows:

$$MSE = \frac{1}{T} \sum_{t=1}^{T} \left((x_t - \hat{x}_t)^2 + (y_t - \hat{y}_t)^2\right),$$

and

$$CC = \left(\frac{\sum_t (x_t - \bar{x})(\hat{x}_t - \bar{\hat{x}})}{\sqrt{\sum_t (x_t - \bar{x})^2 \sum_t (\hat{x}_t - \bar{\hat{x}})^2}}, \frac{\sum_t (y_t - \bar{y})(\hat{y}_t - \bar{\hat{y}})}{\sqrt{\sum_t (y_t - \bar{y})^2 \sum_t (\hat{y}_t - \bar{\hat{y}})^2}}\right),$$

where $\bar{x}$ and $\bar{y}$ represent the means of the $x$ and $y$ positions, respectively. Note that while we computed the full kinematic state vector, we characterized the error solely in terms of position, since position accuracy is the key criterion for many neural control tasks. We note also that the $MSE$ is more meaningful for prosthetic applications, where the subject needs precise control of cursor position; we observed decoding results with relatively...
high correlation coefficients that were sometimes far from the true 2D hand trajectory.

We first explore the basic Kalman model and its decoding performance for the two different movement tasks. We then analyze its behavior with respect to a number of modeling choices. Finally, we compare it with other techniques (the population vector and linear filter).

3.1 Decoding

*Pinball Task.* To be practical, we must be able to train the model (i.e., estimate $A$, $H$, $W$, $Q$) using a small amount of data. Experimentally we found that approximately 2.5 minutes of training data sufficed for accurate reconstruction (this is similar to the result for fixed linear filters reported in Serruya et al., 2002). The exact amount needed will increase as the number of parameters in the model (neurons and kinematic variables) increases. We explore the effect of varying the amount of training data below.

After learning the Kalman model as described in section 2 and the appendix, we evaluate it by reconstructing test trajectories off-line using approximately 1 minute of recorded neural data not present in the training set. At the beginning of a test trial, we made the assumption that hand kinematics were unknown, and we let the predicted initial condition be equal to the average of the kinematics in the training data. The Kalman filter was then applied to reconstruct the hand kinematics. Some examples of the reconstructed hand trajectory are shown in Figure 3A; Figure 4 shows the reconstruction of each component of the state variable (position, velocity and acceleration in $x$ and $y$) for 1/3 of the test data. Note that since the ground-truth velocity and acceleration curves were computed from the position data with simple finite differences, the ground truth for these variables is quite noisy.

*Pursuit Tracking Task.* The data from the pursuit tracking task consisted of 182 short trials from which we randomly selected 130 trials (approximately 17 minutes) as training data and took the remaining 52 trials (approximately 6.5 minutes) as test data.

In contrast to the pinball task, each test trial here was of short duration, and consequently the choice of initial starting state for the hand kinematics had a large impact on the accuracy of the results. Whereas in the pinball task, we let the starting kinematics be equal to the mean state in the training data, here we took it to be the true initial condition. Starting from this state, the Kalman filter algorithm was applied to reconstruct the system state as before. Figure 3B shows some examples of reconstructed hand trajectories. Numerical results are presented below for various lags.

3.2 Real-Time Performance. The encoding and decoding software was written in Matlab (Mathworks Inc., Natick, MA), and the experiments were
run on a computer with a Pentium III 866MHz processor. For the pursuit tracking task, with 17 min of training data, the Kalman model took 1.70 s to learn, while the pinball task, with approximately 3.5 min of training data, took 0.14 s to train.

Decoding was performed at a rate of 0.15 ms per 50 ms time bin for the pursuit tracking task and 1.54 ms per 70 ms time bin for the pinball task. This decoding cost is insignificant relative to these bin sizes. Note that decoding for the pinball data took longer due to the fact that the kinematic
model had more parameters (six rather than four as discussed below) and there were more neurons recorded for this task (42 versus 25).

### 3.3 Optimal Lag

**Pinball Task.** It is convenient to choose time lags corresponding to multiples of the bin size, although one could always re-bin the data and compute a finer discretization of the time lag. We used uniform time lags of 0, 70, 140, 210, 280 ms for the training and testing of the Kalman filter (see Table 2). From Table 2 (similar to Table 1 in Wu et al., 2003), we see that the optimal uniform lag was approximately two time bins (or 140 ms). Note that at each time step, the firing rate was the number of spikes over the previous 70 ms bin; therefore, binning the spikes introduces a lag even at what we are calling 0 lag in the binned data. The same lag property also exists in the pursuit tracking task (with bin size 50 ms).

In general, we observed that individual neurons do not all have the same optimal lag, though, in practice, the range of possible lags is bounded \(0 \leq i \leq 4 \text{ or } 0 \text{ ms} \leq \text{lag} \leq 280 \text{ ms}\). To simplify our data analysis, we assume that the optimal lag for all cells is less than four time bins (280 ms) and
Table 2: Pinball Task: Reconstruction Results for the Recursive Kalman Filter with Varied Time Lags.

<table>
<thead>
<tr>
<th>Method</th>
<th>$CC (x, y)$</th>
<th>$MSE \text{ (cm}^2\text{)}$</th>
</tr>
</thead>
<tbody>
<tr>
<td>Kalman (0 ms lag)</td>
<td>(0.78, 0.91)</td>
<td>7.01</td>
</tr>
<tr>
<td>Kalman (70 ms lag)</td>
<td>(0.80, 0.93)</td>
<td>6.25</td>
</tr>
<tr>
<td>Kalman (140 ms lag)</td>
<td>(0.82, 0.93)</td>
<td>5.87</td>
</tr>
<tr>
<td>Kalman (210 ms lag)</td>
<td>(0.81, 0.89)</td>
<td>6.80</td>
</tr>
<tr>
<td>Kalman (280 ms lag)</td>
<td>(0.76, 0.82)</td>
<td>8.81</td>
</tr>
<tr>
<td>Kalman (nonuniform, init 1)</td>
<td>(0.84, 0.93)</td>
<td>4.75</td>
</tr>
<tr>
<td>Kalman (nonuniform, init 2)</td>
<td>(0.84, 0.93)</td>
<td>4.77</td>
</tr>
</tbody>
</table>

Notes: The upper portion shows uniform lags for all cells, and the bottom portion shows nonuniform lags. In the case of uniform time lags, we found that 140 ms provided the best description of the relationship between firing pattern and hand movement. Optimizing the individual lag for each cell, however, produced relatively more accurate decoding in terms of mean-squared error. The nonuniform time lag is obtained by a greedy search process with a randomized initial starting point. The results for two differentiations (init 1 and init 2 are shown.)

exploit the greedy algorithm described in Table 1 to approximate the optimal lag for each neuron.

The algorithm requires an initial guess of the lag for each cell. We experimented with multiple random initial conditions and found that the greedy search algorithm produced lags that were almost the same in all cases. The results for two experiments are shown in Figure 5A. These two suboptimal time lag solutions gave similar decoding results (see Table 2).

These results suggest that a nonuniform time lag is superior to a uniform one for modeling the relationships between firing patterns and hand movement. In the interest of simplicity, however, and for the remainder of the letter, except where noted, we choose a fixed uniform time lag of 140 ms with which we evaluate all other aspects of the Kalman model.

**Pursuit Tracking Task.** For the pursuit tracking task, the decoding accuracy for different uniform lag times is shown in Table 4 (column labeled “Pos, Vel, Accel”); the accuracy is reported in terms of the average $MSE$ and $CC$ over 52 test trials. We observed that 150 ms was approximately the optimal lag, which is consistent with the 140 ms lag found for the pinball task. (Recall that data for the pursuit tracking task were binned into 50 ms time bins in contrast to the 70 ms bins in the pinball task.)

Here we found less variation in decoding results with respect to time lag. Consequently the optimal nonuniform lag (see Figure 5B) showed no improvement over the best uniform lag. We hypothesize that this is due to the much slower hand motions present in this task; the hand is moving slowly enough that the difference in kinematic state between various lags...
Figure 5: (A) Pinball experiment. Optimization of individual lag times within a bound of $0 \text{ ms} \leq \text{lag} \leq 280 \text{ ms}$. The vertical axis shows the lag in terms of the number of time bins. Each unit on the horizontal axis corresponds to one of the 42 cells. The left plot shows two random initial lags: (1) dashed line with circles; (2) solid line with stars. The right plot shows final estimated lags from the two initial conditions. Note that for most cells, these two solutions are the same. This suggests that the greedy search approach, with random initial starting lags, provides reasonably stable results. (B) Pursuit tracking experiment. Optimization of individual lag times using the greedy algorithm. The range of possible lag steps is bounded $0 \leq i \leq 5$, or $0 \text{ ms} \leq \text{lag} \leq 250 \text{ ms}$.

is less important. For the remainder of the letter, except where noted, we choose a fixed uniform time lag of 150 ms for the pursuit tracking task.

3.4 Kinematic Model. We assumed above (by default) that position, velocity, and acceleration of the hand were related to neural firing rates. Other kinematic models with more or fewer terms could be employed. To understand the relationship between the order of the kinematic model and neural activity, we tested a variety of models, including position alone (zeroth order); position and velocity (first order); position, velocity, and acceleration (second order); and so on up to fifth order. Note that velocity and acceleration correspond to first and second derivatives of position, respectively. The next three higher-order derivatives are referred to as jerk, snap, and crackle.

Pinball Task. We trained and evaluated each of these models. To avoid overfitting, we learned each Kalman model using the training data set and then evaluated the decoding accuracy in test data set. The decoding results in Table 3 show that adding higher-order terms increases the decoding accuracy, but with diminishing returns. As the number of terms in the model increases, so does the need for training data and the risk of overfitting.

The optimal choice of kinematic model is an example of a model selection problem. The Bayesian information criterion (BIC) (Rissanen, 1989)
Table 3: Pinball Task: Decoding and BIC Results with Respect to the Order of the Kinematic Model.

<table>
<thead>
<tr>
<th>Number of Orders</th>
<th>CC ((x, y))</th>
<th>(\text{MSE (cm}^2)</th>
<th>(\alpha + \beta)</th>
</tr>
</thead>
<tbody>
<tr>
<td>0</td>
<td>((0.72, 0.87))</td>
<td>7.72</td>
<td>−80834</td>
</tr>
<tr>
<td>1</td>
<td>((0.82, 0.91))</td>
<td>6.31</td>
<td>−84049</td>
</tr>
<tr>
<td>2</td>
<td>((0.82, 0.93))</td>
<td>5.87</td>
<td>−84411</td>
</tr>
<tr>
<td>3</td>
<td>((0.82, 0.93))</td>
<td>5.72</td>
<td>−84458</td>
</tr>
<tr>
<td>4</td>
<td>((0.82, 0.93))</td>
<td>5.61</td>
<td>−84307</td>
</tr>
<tr>
<td>5</td>
<td>((0.82, 0.93))</td>
<td>5.60</td>
<td>−84081</td>
</tr>
</tbody>
</table>

Notes: Order 0 corresponds to a system state containing just hand position. Order 1 combines position with the first derivative of position (i.e., velocity). Order 2 uses position, velocity, and acceleration. Order 3 adds the third derivative (jerk), while orders 4 and 5 add the additional derivatives (snap and crackle, respectively). Experiments showed that the higher-order system models result in more accurate decoding but with diminishing returns. The boldface entries are optimal in terms of a BIC as well as for practical purposes.

provides one approach to deal with the general case. Assume the hand kinematics \(X_M = [x_1, x_2, \ldots, x_M]^T\) and the firing rates \(Z_M = [z_1, z_2, \ldots, z_M]^T\) are known for the \(M\) time instants in the training set. Let

\[
\alpha = -\log_{A,W,H,Q} p(X_M, Z_M), \quad \text{and} \quad \beta = \frac{\# \text{ of parameters} \log M} {2}
\]

Then from information theory, \(\alpha\) is the number of bits to describe the data, and \(\beta\) is the number of bits to describe the model. BIC searches for the minimal number of bits to describe the model and the data: the kinematic model that has the smallest \(\alpha + \beta\). Table 3 shows that (position, velocity, acceleration, jerk) was the optimal kinematic model. In practice, we have found a second-order model to be sufficient and to provide a good trade-off between accuracy and model complexity. This model is used in the experiments below (except where noted).

**Pursuit Tracking Task.** Table 4 shows the decoding accuracy for different kinematic models as well as different lags. For this data set, we found that velocity is crucial, while the acceleration and higher-order terms result in overfitting of the model and a reduction of accuracy. One hypothesis for the difference between the pursuit tracking and pinball tasks with respect to the optimal kinematic model has to do with the particular type of motion present. In the pursuit tracking task, the range of accelerations was much smaller than in the pinball task. In particular, the magnitude of the acceleration was much smaller relative to the magnitude of the velocities (see Figure 1). We observed increased firing rates as velocity and acceleration increased. The slow motions in the pursuit tracking task and the resulting low firing rates suggest that the effects of acceleration cannot be distinguished
Table 4: Pursuit Tracking Task: Reconstruction Results for the Recursive Kalman Filter with Varying Time Lag and Different Kinematic Models.

<table>
<thead>
<tr>
<th>Lag</th>
<th>Position</th>
<th>Position, Velocity</th>
<th>Pos, Vel, Accel</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>CC (x, y)</td>
<td>MSE (cm²)</td>
<td>CC (x, y)</td>
</tr>
<tr>
<td>0 ms</td>
<td>(0.43,0.39)</td>
<td>7.64</td>
<td>(0.79,0.68)</td>
</tr>
<tr>
<td>50 ms</td>
<td>(0.46,0.40)</td>
<td>7.56</td>
<td>(0.79,0.68)</td>
</tr>
<tr>
<td>100 ms</td>
<td>(0.49,0.40)</td>
<td>7.46</td>
<td>(0.79,0.68)</td>
</tr>
<tr>
<td>150 ms</td>
<td>(0.51,0.41)</td>
<td>7.38</td>
<td>(0.79,0.68)</td>
</tr>
<tr>
<td>200 ms</td>
<td>(0.53,0.41)</td>
<td>7.34</td>
<td>(0.79,0.67)</td>
</tr>
<tr>
<td>250 ms</td>
<td>(0.54,0.40)</td>
<td>7.33</td>
<td>(0.78,0.67)</td>
</tr>
<tr>
<td>Nonuniform</td>
<td>(0.53,0.41)</td>
<td>7.14</td>
<td>(0.79,0.68)</td>
</tr>
</tbody>
</table>

Notes: A uniform time lag of approximately 150 ms was roughly optimal, as was a kinematic model containing just position and velocity (see the boldface entry). Here there was no improvement when using a nonuniform lag.

from noise. In all experiments below involving the pursuit tracking task, except where noted, we used a kinematic model containing only position and velocity.

### 3.5 Conditional Dependence of the Firing Rates.

In section 2, we suggested that the firing rates of the neurons in MI are not independent conditioned on the hand kinematics and emphasized the importance of learning a full covariance matrix $Q$. Conditional independence would imply that the likelihood could be written in terms of the probability of the firing rates, $z_{i,k}$, of the individual neurons, $i = 1 \ldots C$:

$$ p(z_k | x_k) = \prod_{i=1}^{C} p(z_{i,k} | x_k) = \prod_{i=1}^{C} \frac{1}{\sqrt{2\pi q_i}} \exp\left(-\frac{1}{2} (z_{i,k} - H_i x_k)^2 / q_i^2 \right) $$

where $q_i^2$ is the observation variance for cell $i$ and $H_i$ is the $i$th row of $H$. This model corresponds to having a diagonal covariance matrix $Q$ with the $q_i$ along the diagonal. Learning the parameters of the Kalman model proceeds as before but with the restriction that $Q$ is diagonal.

Table 5 shows the decoding results obtained under this conditional independence assumption. We found that the full covariance matrix provides a better probabilistic model of the neural data and results in more accurate decoding. The importance of conditional dependence of the firing rates can be demonstrated using a $t$-test (Larsen & Marx, 2001). For each pair of cells, we obtained the $p$-value under the null hypothesis that the firing rates for this pair were conditionally independent. We found that over all the pairs, 51% (pinball) and 40% (pursuit tracking) of $p$-values were less than 0.05; therefore, the null hypotheses of the independence of the corresponding
Table 5: Decoding Accuracy for Full and Diagonal Matrix for Both Pinball and Pursuit Tracking Tasks.

<table>
<thead>
<tr>
<th>Method</th>
<th>Pinball Task</th>
<th>Pursuit Tracking Task</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>$CC (x, y)$</td>
<td>MSE (cm$^2$)</td>
</tr>
<tr>
<td>Full covariance</td>
<td>(0.82, 0.93)</td>
<td>5.87</td>
</tr>
<tr>
<td>Diagonal covariance</td>
<td>(0.82, 0.93)</td>
<td>6.91</td>
</tr>
</tbody>
</table>

pairs should be rejected. This alternative analysis also suggests the importance of representing a full covariance matrix $Q$. Note that estimating the full covariance matrix may be problematic for large populations of neurons. As the size of $Q$ increases, more training data are needed to avoid overfitting. To cope with this problem, one can use principal component analysis (PCA) to reduce the dimensionality of the observation data. In the reduced-dimensional PCA space, the directions are decorrelated, but since the firing rates are not gaussian, PCA does not make the directions conditionally independent. Consequently, it is still advantageous to fit a full covariance matrix; the advantage is that it can be fit to lower-dimensional data.

3.6 Number of Neurons. We explored the effect of varying the population size on decoding accuracy and, not surprisingly, found that larger populations result in more accurate decoding. For any $N = 1, \ldots, C$, ($C = 42$ in pinball; $C = 25$ in pursuit tracking), we randomly selected subsets of $N$ neurons from our population. We then fit the Kalman model to the training data and reconstructed the test data. The random subsets were chosen 100 times, and the decoding results were averaged (see Figure 6A). We found that for both data sets, the $MSE$ and $CC$ improved with increasing population size. Current recording technology is now able to produce 100 or more simultaneous recordings. The results here suggest that these larger populations may lead to decreases in $MSE$, which should make neural prosthetic control more accurate.

3.7 Amount of Training Data. We also explored the effect of the quantity of training data on decoding accuracy: larger amounts of training data resulted in more accurate decoding. Using the same test data, we selected different amounts of partial training data to learn the Kalman model. The decoding results are shown in Figure 6B. We found that in the pinball task, approximately 2.5 minutes of training data was sufficient; in the pursuit tracking task, we used approximately 10 minutes of training data, although more data improved the results slightly.
Figure 6: (A) Decoding accuracy with respect to number of neurons. The upper plot is the average of the \( MSE \) over 100 random subsets; the lower plot is the corresponding correlation coefficient for \( x \) (circle) and \( y \) (square). The left plot is for the pinball task and the right for the pursuit tracking task. Note that even with a single neuron, the value of the \( CC \) can be deceptively high, while the \( MSE \) is large, as expected. (B) Decoding accuracy with respect to number of training data in both pinball and pursuit tracking tasks. The illustrations of the four plots correspond to those in A. The basic trend is that the larger the training data set, the higher the decoding accuracy, but the improvement appears to diminish as the number of training data increases.

**Modeling Summary.** A Bayesian framework such as the Kalman filter requires us to define a likelihood model and a prior model. The prior model here is given by the linear gaussian system model, and we do not explore various generalizations of that model. Rather, the experiments above pertain to the likelihood and how it is formulated. While the standard Kalman framework constrains us to a linear gaussian model, there are still many modeling choices necessary to match this framework to motor cortical activity. Based on the above experiments, a number of general observations can be made.

We observed that a full covariance matrix is critical for decoding accuracy. Time lags of roughly 150 ms improved results, and while there was some benefit to nonuniform lag times, there was much to be gained from a simple uniform lag. The order of the kinematic model was dependent
on the application motion, but for general, unconstrained, and continuous motions, it appeared that higher-order models (up to fourth order) were beneficial. Not surprisingly, we also found that accuracy increases with the number of cells used. The appendix also contains an analysis of the effect of varying the bin size. We found that larger time bins improved decoding accuracy, but the optimal size depended on the task, with fast motions requiring smaller bins than slow motions.

In summary, the best decoding performance for the two tasks were obtained as follows:

**Pinball:** $CC = (0.84, 0.93), MSE = 4.55$: 140 ms time bin, nonuniform lag, second-order model (pos, vel, accel)

**Pursuit tracking:** $CC = (0.81, 0.70), MSE = 4.66$: 300 ms time bin, 150 ms uniform lag or nonuniform lag, first-order model (pos, vel)

### 3.8 Comparison with Previous Decoding Methods.

A variety of other methods have been proposed for performing motor cortical decoding. Below, we compare the Kalman filter to the most popular methods and then suggest further extensions of the Bayesian decoding framework.

#### 3.8.1 Population Vector Method.

The population vector approach (Georgopoulos et al., 1982, 1986) treats MI cells as having a “preferred” movement direction and models the hand movement direction as a weighted vector average of these preferred directions where the weight is proportional to the firing rate of the cell. The population vector algorithm can be expressed in the following equation (Moran & Schwartz, 1999b),

$$PV_k = \sum_{i=1}^{C} \frac{z_{i,k} - \bar{z}_i}{z_{\text{max}_i} - \bar{z}_i} \cdot \vec{B}_i,$$

where $PV_k$ is the population vector at time $t_k = k \Delta t, k = 1, \ldots, M, z_{i,k}$ is the firing rate of cell $i$ at time $t_k$, $\bar{z}_i$ and $z_{\text{max}_i}$ are the average and maximum firing rates of cell $i$ over all time steps, and $\vec{B}_i$ is the 2D unit length vector pointing in the preferred direction of cell $i, i = 1, \ldots, C$. This formulation models only movement direction and not hand position and hence represents only a subset of the kinematic information modeled by the Kalman filter. To recover hand position, one integrates the direction estimates over time and then normalizes the result to obtain an estimate of hand position (Schwartz, 1993).

The population vector method has been used in the decoding of various hand movement tasks, including center-out reaching (Moran & Schwartz, 1999b), sinusoid tracing (Schwartz, 1993), spiral tracing (Moran & Schwartz, 1999a), and figure-eight tracing (Schwartz & Moran, 1999). Recently, this
Figure 7: Preferred directions of all cells in pinball (left) and pursuit tracking (right) tasks. The distributions of directions are not uniform over $[0, 2\pi]$. 

The lack of accuracy may be due to at least two reasons. First, the approach assumes that the population uniformly samples the range of movement directions, yet for the small sample sizes available with current multielectrode recording technology, this may be difficult to satisfy (Gribble & Scott, 2002). For the data sets we considered, the movement directions were not uniformly distributed (see Figure 7). One of the key advantages of the full covariance matrix in the Kalman filter is that it accounts for the nonuniform distribution of encoding properties across the population. If two cells encode the same information, the errors in the likelihood term are correlated, and the covariance matrix appropriately accounts for their conditional dependence; the linear filter method below does something similar. This weighting of the data is critical for sound inference. Another issue with the population vector approach is that the integration of direction estimates to compute position information results in the compounding of errors over time.

Thus, the population vector method may be appropriate for simple stylized motions or motions of short duration, yet to model general, continuous, and complex motions, a more powerful model (richer kinematics and a probabilistic formulation) is preferable.
Table 6: Decoding Results with Different Methods for the Pinball and the Pursuit Tracking Tasks.

<table>
<thead>
<tr>
<th></th>
<th>Pinball task</th>
<th>Pursuit Tracking task</th>
</tr>
</thead>
<tbody>
<tr>
<td>Method</td>
<td>CC (x, y)</td>
<td>MSE (cm²)</td>
</tr>
<tr>
<td>Population vector</td>
<td>(0.26, 0.21)</td>
<td>75.0</td>
</tr>
<tr>
<td>Linear filter (N = 14)</td>
<td>(0.79, 0.93)</td>
<td>6.48</td>
</tr>
<tr>
<td>Kalman ( \Delta t = 140 ) ms, nonuniform lag</td>
<td>(0.84, 0.93)</td>
<td>4.55</td>
</tr>
<tr>
<td></td>
<td>CC (x, y)</td>
<td>MSE (cm²)</td>
</tr>
<tr>
<td>Population vector</td>
<td>(0.57, 0.43)</td>
<td>13.2</td>
</tr>
<tr>
<td>Linear filter (N = 30)</td>
<td>(0.73, 0.67)</td>
<td>4.74</td>
</tr>
<tr>
<td>Kalman ( \Delta t = 300 ) ms, 150 ms uniform lag</td>
<td>(0.81, 0.70)</td>
<td>4.66</td>
</tr>
</tbody>
</table>

Note: Boldface type indicates the best decoding results.

3.8.2 Linear Filter Method. Linear filters reconstruct hand position as a linear combination of the firing rates over some fixed time period (Carmena et al., 2003; Serruya et al., 2002; Warland, Reinagel, & Meister, 1997; Wessberg et al., 2000), that is,

\[
    x_k = a + \sum_{i=1}^{C} \sum_{j=0}^{N} z_{i,k-j} f_{i,j},
\]

where \( x_k \) is the \( x \)-position (or, equivalently, the \( y \)-position) at time \( t_k = k \Delta t, k = 1, \ldots, M \), \( a \) is a constant offset, \( z_{i,k-j} \) is the firing rate of neuron \( i \) at time \( t_{k-j} \), and \( f_{i,j} \) are the filter coefficients. The coefficients can be learned from training data using simple least-squares regression. The method has been used for off-line decoding of MI activity (Paninski et al., 2004) and for real-time neural control (Carmena et al., 2003; Serruya et al., 2002; Wessberg et al., 2000).

The parameter \( N \) specifies the number of time bins used to estimate the hand position. Empirically, \( N \) is chosen so that the total data used are between 500 ms and 2 s. In Serruya et al. (2003), the authors stated that \( N = 30 \) is the optimal choice because “shorter filters did not perform as well and that longer filters did not provide much additional information.” A larger \( N \) results in a large computational cost in estimating the filters (by inverting a large matrix), which becomes prohibitive when the number of cells is large. It also requires more training data to avoid overfitting. Consequently, we took \( N = 30 \) to be the maximum number of time bins.

To make the linear filter effective and compare it to the Kalman filter, we selected the \( N \) that gave the best decoding results, where we allowed \( N \) to range over \( \{1, 2, \ldots, 30\} \) time bins. For the pinball task, \( N = 14 \) (approximately 1 sec) gave the best decoding accuracy, while in the pursuit tracking...
task, \( N = 30 \) (approximately 1.5 sec) was optimal (although there is little difference in the results for \( N \geq 27 \)).

A 1 sec worth (pinball) and 1.5 sec worth (pursuit tracking) of firing-rate information before hand kinematics is also used in the method described in Serruya et al. (2002, 2003). Note that since the linear filter uses data over a long time window, it does not benefit from the use of time-lagged data. Note also that it does not explicitly reconstruct velocity or acceleration. One could compute velocity with the linear filter (Carmena et al., 2003), but to estimate position, one would need a way to combine linear filter estimates for position and velocity. The Kalman filter automatically does this within an optimal Bayesian framework.

The linear filter reconstruction of position for the pinball data is shown in Figure 8. The results are visually similar to the Kalman results (compare Figure 4), yet Table 6 shows that the Kalman filter gives a more accurate reconstruction (higher \( CC \) and lower \( MSE \)). Figure 9 shows the linear filter reconstruction for the same four trials as in the pursuit tracking task shown in Figure 3B.

The linear filter is a discrete Wiener filter (Gelb, 1974) in the sense that at each time instant, the hand position is a linear function of the firing rates of all the cells over the past \( N \) bins; the appendix explores this relationship formally.

The linear filter approach lacks an explicit generative model of neural activity and hence provides little insight into neural coding (apart from suggesting a linear relationship between hand position and firing rate). Both the linear filter and population vector lack an explicit prior model for how the system state evolves. This results in noisy estimates of the state and necessitates the use of large time windows for the linear filter. In practice, post hoc smoothing is often used to reduce the noise in the linear filter estimates, yet this introduces undesirable lags in the reconstruction. The Kalman filter uses many fewer data at each time instant than the linear filter, but has an explicit temporal model that incorporates prior estimates in a recursive fashion. In particular, the probabilistic model (first-order...
Markov) underlying the Kalman filter means that only a single bin of data is used at each time instant, and these bins should never overlap in time.

3.8.3 Artificial Neural Networks. Artificial neural networks (ANNs) have also been used for neural decoding (Ghazanfar, Stambaugh, & Nicolelis, 2000; Sanchez et al., 2003) and real-time prediction of hand trajectories from neural ensembles in MI (Wessberg et al., 2000). ANNs can perform many types of statistical learning, yet they do not provide explicit generative or probabilistic models that are open to inspection. The models can, however, be analyzed to varying degrees to try to tease out what they encode (Sanchez et al., 2003). Wide variability in the specific implementation and training of these methods makes it impractical to quantitatively compare our results with previous ANN implementations.

4 Discussion

Our focus in this letter has been the development of a decoding algorithm appropriate for neural prosthetic applications. The Kalman filter is
computationally efficient (real time), requires little training data, and provides more accurate off-line decoding than previous methods such as population vectors or linear filtering. While the linear gaussian model of neural coding is an approximation, it provides a reasonable trade-off between computational efficiency and accuracy. Its successful use in decoding may be thought of as resulting from its achieving a good bias/variance trade-off (Geman, Bienenstock, & Doursat, 1992); equivalently, it provides a reasonable solution to the model selection problem, given the complexity of the task and the size of the training data sets at hand. More powerful nonlinear, and nongaussian, likelihood models can be constructed (Brockwell et al., 2004; Gao et al., 2002; Gao, Black, Bienenstock, Wu, & Donoghue, 2003) and used for Bayesian decoding; the decoding task, however, becomes more difficult. For example, the likelihood can be formulated using generalized linear models (Gao et al., 2003), generalized additive models (Gao et al., 2003), mixture models (Wu et al., 2004a), and fully nonparametric models (Gao et al., 2002).

In Gao et al. (2002) we introduced particle filtering to solve the general Bayesian decoding task in MI with nonlinear, nongaussian, likelihoods (see also Brockwell et al., 2004; Shoham, 2001). The particle filtering method is more general than the Kalman filter proposed here. With sufficient computational resources, linear gaussian decoding using a particle filter approaches the accuracy of the Kalman filter. Additionally, more complex likelihood models can give higher accuracy than the linear-gaussian model (Gao et al., 2003). Current implementations of particle filtering, however, do not run in real time and, hence, are not yet appropriate for neural prosthetic applications.

The method proposed here assumes that firing rates can be approximated by a linear model and that action potentials from multiple cells recorded by a single electrode can be cleanly separated (sorted). In practice, however, automated spike sorting methods may incorrectly classify multiple waveforms as being produced by the same cell. This can reduce decoding accuracy since it violates the model assumptions. An extension of the Kalman filter reformulates the likelihood as a probabilistic mixture of linear gaussian models (Wu et al., 2004a) in order to cope, to some extent, with errors of this type. An efficient algorithm known as the switching Kalman filter (Murphy, 1998) can be used for decoding with this mixture model. Wood, Fellows, Donoghue, & Black, 2004) suggest this sorting may not be a significant problem for neural prosthesis applications and that good decoding accuracy can be obtained using a Kalman filter with unsorted, multiunit data.

Our formulation also assumes that motor cortex codes movement in terms of firing rates. In the Bayesian formulation, this assumption too can be relaxed and a point process model, taking into account spike timing, can be used for decoding (Brown et al., 1998; Eden, Frank, Barbieri, Solo, & Brown, 2004). The resulting decoding algorithm is more complex, however, than the simple Kalman filter presented here.
Here we focused on the likelihood (measurement model) as derived from studies of neural coding. To evaluate different choices for the likelihood, we used a simple linear gaussian temporal prior (system model). More complex, nonlinear models or higher-order Markov assumptions might lead to more accurate models of arm motion and more accurate decoding results.

The linear filter and Kalman filter both produce reasonable decodings of neural activity. Depending on the specifics of the model, the Kalman filter can be viewed as a linear filter (Weiner filter) in which all measurements back to the initial time step are taken into account, yet the contribution of measurements decays exponentially with time. The Kalman filter, however, provides a number of benefits. It is easier to train (less computationally intensive) and, more important, formulates the problem as one of Bayesian inference. Since assumptions about the data and the noise are explicitly spelled out, the Kalman model provides more insight into the encoding model that is used. Moreover, by making the assumptions explicit, it suggests avenues for improving both modeling and decoding by relaxing some of these assumptions.

We have studied off-line decoding accuracy rather than online control. It is reasonable to expect that algorithms that provide better off-line decoding will provide better online accuracy as well. One might also posit that better control algorithms may make the training of paralyzed human subjects easier. Results of online control studies, however, suggest that even algorithms such as the population vector method, with its poor off-line accuracy, can be used to control devices (Taylor et al., 2002). It may be the case that the brain adapts to a particular control algorithm and that improving the algorithm produces little gain in accuracy. Such a hypothesis remains to be tested.

Research on decoding for neural control has focused on cells in motor cortex. The rationale underlying this choice is that it will be easier for subjects to learn to control physical devices when this area of cortex is used, since it already represents information about motion. Even in paralyzed subjects, imagined arm motions produce activity in MI, suggesting its appropriateness for human neural prostheses (Kennedy & Bakay, 1998). Other brain areas, however, may provide useful control signals for motor prosthetic applications. The applicability of the Kalman filter outside MI remains to be tested.

The results reported here involved only two animals, and each animal was trained on, and performed, a slightly different task. More studies will be required to generalize these results to a broader range of tasks and conditions.

5 Conclusions

We have described a discrete linear Kalman filter that is appropriate for the neural control of 2D cursor motion. We showed that the model could be easily learned using a few minutes of training data and provided real-time
estimates of hand position given the firing rates of a population of cells in primary motor cortex. The estimated trajectories were more accurate than those produced by the population vector and linear filtering methods most commonly used in the literature. Analysis of the method was performed using two data sets involving complex, continuous hand motions. Neural recordings from two different monkeys were obtained from chronically implanted microelectrode arrays. The experiments suggested that a linear gaussian model provided an approximate model relating the firing rates with continuous hand movement. Moreover, the model enabled the use of the Kalman filter to perform real-time recursive Bayesian decoding.

The Kalman filter proposed here provides a rigorous probabilistic approach with a well-understood theory. By making the assumptions explicit and providing an estimate of uncertainty, the Kalman filter offers significant advantages over previous methods. Unlike previous methods, this model estimates a full kinematic state vector (position, velocity, and higher-order terms). It also provides an estimate of the uncertainty in the result in terms of an error-covariance matrix. Various experiments explored the use of this decoding model to choose the kinematic variables that gave the best encoding and decoding performance.

In contrast to the relatively constrained pursuit tracking task, we showed that for the more natural 2D motions of the pinball task, incorporating acceleration and higher-order terms into the model improved the accuracy of the decoding. The experiments suggest a number of general conclusions, which remain to be verified in more subjects and in online experiments:

1. A time lag of 140 to 150 ms between firing activity and hand kinematics improves decoding results.
2. As the number of neurons in the population increases, one observes a corresponding increase in decoding accuracy. While even small populations produce reasonable results, the ability, in the not-too-distant future, to record from much larger populations is likely to increase accuracy even further.
3. A few minutes of training data are sufficient for learning the linear gaussian model. The number of data required may depend on the task.
4. With the gaussian model, a full covariance matrix usefully captures the conditional dependence between the firing rates of different neurons. Decoding accuracy is improved by using a full covariance matrix as compared to a diagonal matrix.
5. Firing rates in larger bin sizes, which are better approximated by a gaussian model, improve the decoding accuracy up to a task-specific limit.
Currently, we are working to evaluate the performance of the Kalman filter for the closed-loop neural control of cursor motion in tasks such as described here. Our recent work demonstrates the feasibility of Kalman filter in the online neural control experiment (Wu, Shaikhouni, Donoghue, & Black, 2004b). More experiments with more animals, however, are needed to confirm those observations. Our future work will focus on the application of automated spike sorting methods that provide an estimate of uncertainty in the rate signal. This uncertainty can be naturally incorporated into the Kalman model by allowing an adaptive measurement covariance matrix $Q_k$. Additionally, one may explore alternative measurement noise models, nonlinear system models, and nonlinear decoding methods.

Appendix: Algorithmic and Experimental Details

**A.1 Learning the Linear Gaussian Model.** Training the Kalman model requires that we learn the matrices $A$, $H$, $W$, $Q$ from example data. We seek the coefficient matrices and covariance matrices that maximize the joint probability $p(X_M, Z_M)$, that is,

$$\arg\max_{A,W,H,Q} p(X_M, Z_M) = \arg\max_{A,W,H,Q} p(X_M) p(Z_M | X_M)$$

$$= \{\arg\max_{A,W} p(X_M), \arg\max_{H,Q} p(Z_M | X_M)\}.$$ 

Using the linear gaussian properties of $p(X_M)$ and $p(Z_M | X_M)$, the above maximization has closed-form solutions:

$$A = \left( \sum_{k=2}^{M} x_k x_k^T - 1 \right) \left( \sum_{k=2}^{M} x_{k-1} x_{k-1}^T \right)^{-1}$$

$$W = \frac{1}{M-1} \left( \sum_{k=2}^{M} x_k x_k^T - A \sum_{k=2}^{M} x_{k-1} x_{k-1}^T \right)$$

$$H = \left( \sum_{k=1}^{M} z_k x_k^T \right) \left( \sum_{k=1}^{M} x_k x_k^T \right)^{-1}$$

$$Q = \frac{1}{M} \left( \sum_{k=1}^{M} z_k z_k^T - H \sum_{k=1}^{M} x_k z_k^T \right).$$

**A.2 Decoding (the Kalman Filter Algorithm).** The assumptions of linear gaussian models for the system and measurement equations allow us to exploit the Kalman filter algorithm for recursive Bayesian inference. The theory is well developed (Kalman, 1960) and the algorithm is summarized here. The algorithm comprises two steps:
**Step 1: Time Update Equations.** At each time $t_k$, we use the system model to take the a priori state estimate, $\hat{x}_{k-1}$, from the previous time $t_{k-1}$, and predict it forward to time $t_k$:

$$\hat{x}_k^- = A\hat{x}_{k-1}. \quad (A.1)$$

Recall that the uncertainty in the system model is expressed in the covariance matrix $W$ and this uncertainty must be incorporated into our a priori estimate of the posterior covariance:

$$P_k^- = AP_{k-1}A^T + W, \quad (A.2)$$

where $P_k^-$ is the a priori error covariance matrix at time $t_k$.

**Step 2: Measurement Update Equations.** Using the prediction $\hat{x}_k^-$ and firing rate $z_k$, we update the state estimate using the measurement and compute the posterior error covariance matrix:

$$\hat{x}_k = \hat{x}_k^- + K_k(z_k - H\hat{x}_k^-), \quad (A.3)$$

$$P_k = (I - K_kH)P_k^-, \quad (A.4)$$

where $P_k$ represents the state error covariance after taking into account the neural data and $K_k$ is the Kalman gain matrix, given by

$$K_k = P_k^-H^T(HP_k^-H^T + Q)^{-1}. \quad (A.5)$$

This $K_k$ produces a state estimate that minimizes the mean-squared error of the reconstruction (see Gelb, 1974, for details).

**A.3 Comparison of the Kalman Filter and the Wiener Filter.** Simple linear filtering methods that directly reconstruct the system state from a history of firing rates are commonly used for decoding. These methods compute the state as a linear combination of previous firing rates. In particular, the Wiener filter is an optimal linear filter that uses all previous firing data. The simplified Kalman filter developed here can be viewed as an efficient, recursive version of the Wiener filter in which the modeling assumptions ($A$, $H$, $W$, $Q$) are made explicit.

We can obtain several basic properties of Kalman filter by studying its relationship with the Wiener filter. From equations A.1 and A.3, we have that

$$\hat{x}_k = \hat{x}_k^- + K_k(z_k - H\hat{x}_k^-)$$

$$= (I - K_kH)\hat{x}_k^- + K_kz_k$$

$$= (I - K_kH)A\hat{x}_{k-1} + K_kz_k.$$
Note that equations A.2, A.4, and A.5 are independent of the new measurements of firing rates. If $A$, $H$, $W$, $Q$ are constant over time, the propagation of $P_k$, $K_k$, $P_k$, $K_k$ by equations A.2, A.4, and A.5 converges to steady-state solutions (Kalman & Bucy, 1961). Let $K = \lim_{k \to \infty} K_k$, and $M = (I - KH)A$. For $k$ large enough (i.e., $k > 20$ in practice),

$$
\hat{x}_k \approx M\hat{x}_{k-1} + Kz_k \\
\approx M^2\hat{x}_{k-2} + MKz_{k-1} + Kz_k \\
\approx \ldots \\
\approx M^{k-1}\hat{x}_1 + \sum_{j=0}^{k-2} M^j Kz_{k-j}.
$$

where $M^j$ is the $j$th power of matrix $M$ (i.e. $M^2 = M \cdot M$).

The above equation shows that in the Kalman framework, the estimate at time step $k$ is a linear function of the firing rates at all time instants from time $t_2$ to the present. This corresponds to the Wiener filter (Gelb, 1974), but the advantage of the Kalman implementation is that it computes the state estimate recursively, resulting in an efficient algorithm.

Note also that the coefficients of all firing rates decay exponentially with respect to the current time step. This shows three basic properties of the Kalman filter: (1) it estimates the state at each time step using all the previous and present measurements (firing rates); (2) the weights of the firing rates decay exponentially (those far from the present time have a weak effect on the state estimate); and (3) for $k >> 1$, the state estimate is approximately independent of the initial state. This last point means that the choice of the initial state is relatively unimportant.

**A.4 Effect of Bin Size on Decoding Accuracy.** We studied the effect of varying the bin size on decoding accuracy and found that accuracy was improved by increasing the bin size beyond the 70 ms and 50 ms bins used in the analysis above. Table 7 and Figure 10A summarize the results. For the pinball task, we varied the bin size, $\Delta t$, by multiples of 70 ms from 0 to 700 ms. For the pursuit tracking task, we considered bins ranging from 0 to 700 ms in 50 ms increments. In all cases, we used nonoverlapping time bins, as the use of overlapping bins results in a severe violation of the assumption of conditional independence underlying by the Kalman framework (see equation 2.7). With overlapping bins, data are “reused,” and the resulting estimates are no longer statistically valid.

For each test condition (bin size), the Kalman model was trained, and hand kinematics were calculated every $\Delta t$ ms. Table 7 shows that larger bins resulted in better decoding accuracy, up to a limit. One reason for this
Table 7: Decoding Results for Varying Bin Sizes.

<table>
<thead>
<tr>
<th>Method</th>
<th>CC (x, y)</th>
<th>MSE (cm²)</th>
<th>Method</th>
<th>CC (x, y)</th>
<th>MSE (cm²)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Δt = 70 ms</td>
<td>(0.82, 0.93)</td>
<td>5.87</td>
<td>Δt = 50 ms</td>
<td>(0.79, 0.68)</td>
<td>5.99</td>
</tr>
<tr>
<td>Δt = 140 ms</td>
<td>(0.83, 0.93)</td>
<td>5.29</td>
<td>Δt = 100 ms</td>
<td>(0.80, 0.68)</td>
<td>5.63</td>
</tr>
<tr>
<td>Δt = 210 ms</td>
<td>(0.81, 0.92)</td>
<td>5.45</td>
<td>Δt = 150 ms</td>
<td>(0.81, 0.68)</td>
<td>5.27</td>
</tr>
<tr>
<td>Δt = 280 ms</td>
<td><strong>(0.82, 0.93)</strong></td>
<td><strong>5.16</strong></td>
<td>Δt = 200 ms</td>
<td>(0.81, 0.69)</td>
<td>5.03</td>
</tr>
<tr>
<td>Δt = 350 ms</td>
<td>(0.78, 0.92)</td>
<td>5.95</td>
<td>Δt = 250 ms</td>
<td>(0.81, 0.69)</td>
<td>4.89</td>
</tr>
<tr>
<td>Δt = 420 ms</td>
<td>(0.78, 0.92)</td>
<td>5.81</td>
<td>Δt = 300 ms</td>
<td><strong>(0.81, 0.70)</strong></td>
<td><strong>4.66</strong></td>
</tr>
<tr>
<td>Δt = 490 ms</td>
<td>(0.75, 0.89)</td>
<td>7.25</td>
<td>Δt = 400 ms</td>
<td>(0.79, 0.70)</td>
<td>4.59</td>
</tr>
<tr>
<td></td>
<td></td>
<td></td>
<td>Δt = 500 ms</td>
<td>(0.79, 0.71)</td>
<td>4.64</td>
</tr>
</tbody>
</table>

Notes: The other model parameters are as described above: pinball task: uniform lag = 140 ms, kinematic model = (pos, vel, accel); pursuit tracking task: uniform lag = 150 ms, kinematic model = (pos, vel). Boldface type indicates the best decoding results.

may be that as the bin size grows, the variation in the firing rate is better approximated by the gaussian model used in the Kalman filter.

In the case of the slow motions of the pursuit tracking task, larger bin sizes were appropriate. For the fast motions of the pinball task, bin sizes beyond approximately 280 ms resulted in a loss of accuracy. This suggests

Figure 10: (A) Decoding accuracy (MSE) as a function of bin size for the pinball task (left) and the pursuit tracking task (right). (B) Example reconstruction with varying bin size. (left) Pinball task: 70 ms (solid), 280 ms (tightly dashed), and 490 ms (loosely dashed). (right) Pursuit tracking task: 50 ms (solid), 300 ms (tightly dashed) and 500 ms (loosely dashed).
that while larger bin sizes can increase accuracy, the ultimate size is limited and is related to the speed of motion.

Additionally, increased bin size had a negative effect on the detail of the recovered trajectories (see Figure 10B). As bin size increases, the frequency of state estimates decreases, resulting in a coarser approximation to the underlying trajectory. In general, larger bin sizes (up to some limits) produce more accurate results but at the cost of introducing a delay in estimating the system state. The constraints of a particular application will determine the appropriate bin size.

Note that if a uniform lag of, for example, 140 ms time bins is used, we can exploit measurement data binned into 140 ms time bins without introducing any delay (or output lag) in the estimate of the system state relative to the natural hand motion. For real-time prosthesis applications, this system delay should be less than 200 ms, which suggests that overall bin size minus the uniform lag time should be less than 200 ms. For the pinball task, with a 140 ms lag, this would mean a maximum bin size of approximately 280 ms. For the pursuit tracking task, with a 150 ms lag, a maximum bin size of 250 to 300 ms would be appropriate. While this increases accuracy, it comes at the cost of a “jerkier” reconstruction.

Acknowledgments

This work was supported in part by the DARPA BioInfoMicro Program, the NIH NINDS Neural Prosthesis Program and Grant #NS25074, and the NSF ITR Program award #0113679. We thank D. Mumford, E. Brown, M. Serruya, A. Shaikhouni, J. Dushanova, C. Vargas-Irwin, L. Lennox, D. Morris, D. Grollman, and M. Fellows for their assistance. J.P. D. is a cofounder and shareholder in Cyberkinetics, Inc., a neurotechnology company that is developing neural prosthetic devices.

References


Received July 8, 2004; accepted May 3, 2005.