Predicting Functional Cortical ROIs via DTI-Derived Fiber Shape Models

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Introduction

Mapping structural and functional connectivities of human cerebral cortex has drawn significant interest and effort recently. A fundamental and challenging problem arises when attempting to measure the structural and/or functional connectivities of specific cortical networks: how to identify and localize the best possible regions of interests (ROIs) on the cortex? In our view, the major challenges come from uncertainties in ROI boundary definition, the remarkable structural and functional variability across individuals and high nonlinearities within and around ROIs. In this paper, we present a novel ROI prediction framework that localizes ROIs in individual brains based on their learned fiber shape models from multimodal task-based functional magnetic resonance imaging (fMRI) and diffusion tensor imaging (DTI) data. In the training stage, shape models of white matter fibers are learnt from those emanating from the functional ROIs, which are activated brain regions detected from task-based fMRI data. In the prediction stage, functional ROIs are predicted in individual brains based only on DTI data. Our experiment results show that the average ROI prediction error is around 3.94 mm, in comparison with benchmark data provided by working memory and visual task-based fMRI. Our work demonstrated that fiber bundle shape models derived from DTI data are good predictors of functional cortical ROIs.

Keywords: brain network, diffusion tensor imaging, fMRI, ROI prediction, shape analysis

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In this paper, we present a novel computational framework that learns fiber bundle models of functional cortical ROIs based on both task-based fMRI and DTI data in the training stage and applies the predictive models to locate functional ROIs in testing samples based only on DTI data in the prediction stage. Specifically, in the training stage, all subjects were linearly aligned to a standard space first. Then, functionally activated ROIs were detected from task-based fMRI, and the fiber bundles emanating from these ROIs were extracted. Finally, the trained model was learned and it includes 2 major components: the ROI coordinate principal component analysis (PCA) model and the fiber bundle templates. In the prediction stage, DTI data of an individual subject was aligned to the standard space first. Then, starting from the average location of warped ROIs from the training data set, an energy function was designed to iteratively optimize the ROIs’ locations. This energy function consists of internal and external terms. The internal term was measured by ROI coordinate reconstruction error, which corresponds to the ROI coordinate PCA model component; while the external term was defined by the Hausdorff metric of ROIs’ fiber bundles, which corresponds to the fiber bundle template component. Our experimental results demonstrated that average prediction error is approximately 3.9 mm, compared with benchmark ROIs derived from task-based fMRI data.

The major advantages of this computational framework and our contributions lie in the following 2 aspects. 1) In the training stage, the activated brain regions detected from task-based fMRI data provide the benchmark ROI data for learning shape models of WM fibers emanating from these ROIs. Our experimental results from working memory task-based fMRI data (Li et al. 2010) demonstrate that the fiber connection patterns of corresponding functional ROIs are quite consistent, providing direct evidence that WM fiber connection pattern is a good predictor of functional landmark (Honey et al. 2009). This is similar to the connectional fingerprint concept presented in Passingham et al. (2002). 2) In the prediction stage, only DTI data is needed to accurately locate the functional ROIs using our predictive models. Typically, a DTI scan takes less than 10 min and is widely available. Therefore, the general methodology of predicting functional cortical ROIs based on DTI will have wide applications in brain imaging in the future.

Materials and Methods
The flowchart of our ROI prediction framework is illustrated in Figure 1. It consists of 2 major stages: model training and ROI prediction. The model training (purple boxes) is performed on the data set in which each subject has both fMRI and DTI data. As such, we can obtain both the benchmark ROI locations and the fiber bundles emanating from them. In the first step (left purple box), multimodal data of all subjects were linearly aligned into the standard template space; then in the second step (right purple box), a PCA model of ROI locations is learned to characterize statistical relationship among ROI locations. Meanwhile, fiber bundle templates are obtained from the extracted fiber bundles for each ROI. The outputs of the training procedure consist of 4 components and are displayed in the red box. In the prediction stage (the green box in Fig. 1), a new subject with DTI and fMRI data was linearly aligned to the standard space and then the trained model (red box) was applied on the DTI data of the subject by minimizing an energy function starting from the initial ROIs location, thus generating the predicted ROIs. The predicted ROIs are then evaluated by comparing with the benchmark ROIs obtained from task-based fMRI data (black box).

Data Acquisition and Preprocessing
Data set 1
Fifteen university students voluntarily participated in this study under IRB approval, and none of them was reported to have mental or physical disease. Each volunteer performed a modified version of the OSPAN task (3 blocks: OSPAN, Arithmetic, and Baseline) while fMRI data was acquired (Faraco et al. 2011). DTI scans were also obtained for each volunteer. Briefly, both fMRI and DTI scans were acquired on a 3-T GE Signa scanner with acquisition parameters as follows. fMRI: 64 × 64...
matrix, 4-mm slice thickness, 220-mm field of view (FOV), 30 slices, time repetition (TR) = 1.5 s, time echo (TE) = 25 ms, ASSET = 2; DTI: 128 × 128 matrix, 2-mm slice thickness, 256-mm FOV, 60 slices, TR = 15 100 ms, TE = variable, ASSET = 2, 3 B0 images, 30 optimized gradient directions, $b$-value = 1000.

**Data set 2**

Ten healthy children performed a block-based visual task. Each block has a 30-s rest period and a 20-s task period when pictures were shown as stimuli. For each subject, DTI data were also obtained. Acquisition parameters for the scans were as follows. fMRI: 64 × 64 matrix, 4-mm slice thickness, 220-mm FOV, 30 slices, TR = 2 s, TE = 30 ms; DTI: 256 × 256 matrix, 3-mm slice thickness, 240-mm FOV, 50 slices, TR = 12 000 ms, TE = variable, 1 B0 volume, 15 DTI volumes, $b$-value = 1000.

The preprocessing of the DTI data is composed of brain skull removal, motion correction, and eddy current correction. Afterward, the diffusion tensor was computed and the fiber was tracked via the MEDINRIA (http://www-sop.inria.fr/asclepios/software/MedINRIA/) toolkit. The fMRI data of the OSPAN task was analyzed using the FSL FEAT (http://www-viplab.jinr.ru/software/FSL/) toolkit. The correlation between the GM/WM tissue and the cortical surface. In data set 1, 8 consistently activated working memory ROIs were used in this paper for ROI modeling and prediction stage. It is noteworthy that a ROI location is defined to be a single vertex on the surface onto which the functional activation peaks from fMRI data are mapped.

**PCA Model for ROIs Locations**

Despite considerable variation, the spatial distribution patterns of the ROIs have certain degree of consistency (Fig. 2a,b). In this paper, the spatial distribution patterns of ROIs in the training set were captured and modeled by their coordinates PCA model, which is widely used in the biomedical image analysis community. Figure 2a,b illustrates the distribution of the ROIs in the standard space $s_{std}$ for each data set. We can observe the considerable regularity of the ROI distribution across subjects.

### Table 1

<table>
<thead>
<tr>
<th>ROI</th>
<th>Location</th>
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</thead>
<tbody>
<tr>
<td>ROI 1</td>
<td>Left occipital pole</td>
</tr>
<tr>
<td>ROI 2</td>
<td>Left paracentral gyrus</td>
</tr>
<tr>
<td>ROI 3</td>
<td>Left precuneus</td>
</tr>
<tr>
<td>ROI 4</td>
<td>Right dorsolateral prefrontal cortex</td>
</tr>
<tr>
<td>ROI 5</td>
<td>Right lateral occipital gyrus</td>
</tr>
<tr>
<td>ROI 6</td>
<td>Right paracentral gyrus</td>
</tr>
<tr>
<td>ROI 7</td>
<td>Right precuneus</td>
</tr>
<tr>
<td>ROI 8</td>
<td>Right superior frontal gyrus</td>
</tr>
</tbody>
</table>

### Table 2

<table>
<thead>
<tr>
<th>ROI</th>
<th>Location</th>
</tr>
</thead>
<tbody>
<tr>
<td>ROI 1</td>
<td>Left occipital pole</td>
</tr>
<tr>
<td>ROI 2</td>
<td>Left lateral occipital cortex</td>
</tr>
<tr>
<td>ROI 3</td>
<td>Left inferior frontal gyrus</td>
</tr>
<tr>
<td>ROI 4</td>
<td>Left dorsolateral prefrontal cortex</td>
</tr>
<tr>
<td>ROI 5</td>
<td>Left frontal pole</td>
</tr>
<tr>
<td>ROI 6</td>
<td>Right postcentral gyrus</td>
</tr>
<tr>
<td>ROI 7</td>
<td>Right occipital pole</td>
</tr>
<tr>
<td>ROI 8</td>
<td>Right superior temporal gyrus</td>
</tr>
<tr>
<td>ROI 9</td>
<td>Right inferior frontal gyrus</td>
</tr>
<tr>
<td>ROI 10</td>
<td>Right frontal pole</td>
</tr>
</tbody>
</table>

Figure 2. (a) Visual evaluation of the effectiveness of ROI coordinate PCA model for data set 1. (b) Visual evaluation of the effectiveness of ROI coordinate PCA model for data set 2. (c) Examples of fiber bundles from ROI #8 of different subjects in data set 1. In (a) and (b), the same ROIs are coded with the same color.

Figure 3. The ratio of the first eigen value to eigen value sum, against the subject number. (a) Brain network in working memory task and (b) brain network in visual task.
Specifically, to train the ROI coordinate PCA model, we first put the coordinates of all ROIs of one subject into a vector as: $v_i=[x_i, y_i, z_i, x_2, y_2, z_2, \ldots, x_n, y_n, z_n]^T$ where $n$ is the number of ROIs. This vector can also be explained as the feature vector of ROI distribution pattern of one subject. Then, the standard PCA method was conducted on feature matrix $M=[v_1, v_2, \ldots, v_m]^T$ where $m$ is the number of training subjects. As a result, the 2 components of the ROI coordinate PCA model $V=[V_{mean}, E]_i$ were obtained: the mean feature $v_{mean}$ and the PCA transformation matrix $E_i=[eig_1, \ldots, eig_p]$ which consists of $p$ eigen vectors of $M$ corresponding to the largest $p$ eigen values that altogether cover 90% of variance.

**Fiber Bundle Models of ROIs**

Fiber bundle model is constructed for each ROI separately across the ROIs spatial distribution patterns, the ROI coordinates of each ROI are reasonably consistent in terms of overall shapes and connectivity patterns.

**Similarity Measurement**

In this section, we will focus on measuring how close a subject to be predicted is to the training ones in terms of the 2 models introduced in Model training. Regarding ROI spatial distribution patterns, the ROI coordinates of the subject to be predicted were extended to be $v_i$, in the same way as that in PCA Model for ROIs Locations. Then, it was projected and reconstructed from the trained PCA model as follows:

$$v_{rec}^i = v_{mean} + Ev_i^T (v^i - v_{mean}).$$

Then, the obtained $v_{rec}^i$ and $v^i$ were converted into the conventional spatial coordinate format, and the Euclidian distance, represented by $\text{Dist}_{pca}(v_{rec}^i, v^i)$, was computed between them, which is the reconstruction error defined as the measurement of how close its distributive pattern is to the training ones.

To measure the similarity between fiber bundles, we adopted the Hausdorff metric, a simple but effective measurement (Zöllei et al. 2010). In our problem, although the overall shape patterns of fiber bundles of the same corresponding ROI are reasonably consistent across subjects, there is still considerable variation in local fiber shapes (Fig. 2e). Therefore, by considering a fiber bundle as a set of individual fiber curves, we measure the supremum of the infimum of the distances between 2 fiber curve sets (2 bundles). Denote 2 fiber bundles as $F_1$ and $F_2$, and let $f_1 \in F_1$ and $f_2 \in F_2$ be the fiber curve. The Hausdorff metric is defined as follows (Henriksson 1999):

$$\text{Dist}_H(F_1, F_2) = \max \left\{ \sup_{f_1 \in F_1}\inf_{f_2 \in F_2} d(f_1, f_2), \sup_{f_2 \in F_2}\inf_{f_1 \in F_1} d(f_1, f_2) \right\}$$

where sup represents the supremum of a set, inf is the infimum of a set, and $d(\cdot, \cdot)$ denotes the distance between 2 fiber curves. In this paper, $d(\cdot, \cdot)$ was defined as the minimum distance between 2 fiber curves.

It should be noted that although we had already applied global alignment between subjects, the distance caused by the ROI location variation across subjects should be eliminated before computing the Hausdorff metric. Currently, we adopted a linear registration method to globally align fiber bundles of corresponding ROIs.

**ROI Prediction Framework**

As already illustrated in Figure 1, ROI prediction for a subject starts with linearly registering it into the standard space $s_{std}$. Then, the entire-brain fibers of the subject are extracted, and the triangulated cortical surface is reconstructed using the same method in Data Acquisition and Preprocessing. The core procedure of the ROI prediction framework is formulated and solved as an energy minimization problem. We defined the energy function as:

$$E = \lambda E_{int} + (1-\lambda) E_{ext}$$

where the internal term $E_{int}$ is expressed by the PCA constraint of ROI coordinates and the external term $E_{ext}$ is formulated by the Hausdorff metric.
Note: Means across ROIs and subjects are in bold fonts.

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of consistent location distribution pattern (Fig. 2)
Considering that potential ROI locations cannot vary too much because
In each iteration, the search space for each ROI is adaptable.
reduce the computation load, we conducted an iterative global search.
trained model and ends when the location becomes stable. In order to
Let \( r \) automatically set the search scope for each individual ROI as follows.
neighborhood on the surface. In the following
global search iteration, the search scope is uniformly set as 8-ring
subjects, \( n \) where \( \frac{1}{C_8} \)

Table 3
Distances between the predicted ROIs and the benchmark ROIs (mm) in the working memory task-based fMRI data set

<table>
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<tr>
<th>Subject</th>
<th>ROI 1</th>
<th>ROI 2</th>
<th>ROI 3</th>
<th>ROI 4</th>
<th>ROI 5</th>
<th>ROI 6</th>
<th>ROI 7</th>
<th>ROI 8</th>
<th>Subject mean</th>
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<tr>
<td>1</td>
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<td>1.87</td>
<td>4.7</td>
<td>3.71</td>
<td>1.45</td>
<td>2.37</td>
<td>2.81</td>
<td>3.53</td>
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<tr>
<td>2</td>
<td>5.87</td>
<td>2.96</td>
<td>2.54</td>
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<td>3.09</td>
<td>8.85</td>
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<td>4.13</td>
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<td>1.92</td>
<td>8.21</td>
<td>1.62</td>
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</table>

ROI ± mean 
6.72 ± 1.55 2.64 ± 0.82 2.81 ± 0.55 3.96 ± 1.51 3.05 ± 1.31 2.93 ± 1.45 5.91 ± 2.78 2.86 ± 0.57

Note: Means across ROIs and subjects are in bold fonts.

measurement of fiber bundle similarity of all ROIs, and \( \lambda \) trades off the 2
terms.
Specifically, the external energy term is formulated as:

\[
E_{ext} = \sum_{m} \sum_{j} \sum_{j'} Dist_{ij} \left( F_i, F_j^2 \right),
\]

where \( n \) is the number of ROIs, the \( m \) is the number of training
subjects, \( F_i \) is the fiber bundle extracted from the subject to be
predicted and \( F_j^2 \) in \( F_j \) is the template fiber bundles introduced in Fiber
Bundle Models of ROIs. It is noted that the template fiber bundles \( F_j^2 \) in
\( F_j \) equally contribute to the Hausdorff metric. As to the internal energy
term, it is directly formulated as the reconstruction error of the
coordinates of all ROIs from the PCA model:

\[
E_{int} = Dist_{pca}.
\]

A whole-space search was conducted to minimize the energy function. The search starts from the mean ROIs location \( \mu_{\text{mean}} \) of the
trained model and ends when the location becomes stable. In order to
reduce the computation load, we conducted an iterative global search.
Considering that potential ROI locations cannot vary too much because
of consistent location distribution pattern (Fig. 2a,b), in the initial
global search iteration, the search scope is uniformly set as 8-ring
neighborhood on the surface. In the following \( k \)th iteration, we
automatically set the search scope for each individual ROI as follows. Let \( e_k \) be the distance that ROI \( i \) moves in the \( k \)th iteration, and \( N_k \) be the
search scope of ROI \( i \) in the \( k \)th iteration on the cortical surface. If
\( e_k < \text{small} \), \( N_k \) will be shrunk. In other word, \( |N_k| \approx e_k^{-1} \). Then, \( N_k^1 \times N_k^2 \times \ldots \times N_k^M \) forms the search space \( R^n \), on which the
\( k \)th global search is conducted for all possible combinations of \( n \) ROIs. Denote \( r \in R^n \) as one combination of ROIs. To further prune the search
space \( R^n \), we added a constraint to the energy function in equation (5)
by eliminating candidates of ROI \( i \) in \( N_k^1 \) if the fiber bundle emanating
from it satisfies \( \sum_{m} Dist_{ij} \left( F_i, F_j^2 \right) > \text{small} \). The constrained search space is
denoted as \( C_k^i \equiv R^n \), which induces the final form of equation (3) as:

\[
\arg \min_{R^n} \left( \lambda E_{int} + (1 - \lambda) E_{ext} \right), \quad C_k^i \equiv R^n.
\]

Finally, the iterative global search stops if all ROI locations are stable and we have \( \sum_{m} Dist_{ij} \left( F_i, F_j^2 \right) \leq \text{small} \). It is worth noting that the 2 measurements
\( Dist_{ij} \) and \( Dist_{pca} \) are computed and normalized into \([0, 1]\) before the
iterative global search begins.

Experimental Results

Evaluation of ROI Coordinate PCA Model and Hausdorff Metric

As the internal energy term, the ROI coordinate PCA model was
used to constrain the ROI locations based on the assumption that
ROI coordinates are roughly following Gaussian distribution.
This assumption can be partly verified by checking
whether the first principal component of matrix
\( M = [v_1, v_2, \ldots, v_m]^T \) is relatively large, that is, the ratio of
the first eigen value to the eigen value sum is expected to be large.
Also, we explored if the subject number \( m \) will be an
influencing factor of the consistency of ROI coordinate
distribution. Therefore, we randomly select \( p \) subjects from
one data set for 50 times and computed the 50 ratios of the first
eigen value to the eigen value sum, as well as their means and
standard deviations. The results shown in Figure 3 demonstrate
2 points: the ratio is as high as above 0.5; the number of subjects does not significantly affect the consistency of ROI coordinate distribution pattern. This result indicates that the PCA model of ROI locations is valid.

In order to further demonstrate that the PCA model of ROI location coordinates really captures the intrinsic relationship of the common human brain architecture, we designed and performed the following experiment on the working memory data set. This experiment also aims to demonstrate that the reconstruction error Dist_{pca} defined in PCA Model for ROIs Locations can be used as a meaningful constraint in ROI prediction. Taking one subject from data set 1, for example, we uniformly sampled 100 groups of the 8 ROIs in the neighborhood of each one. The 100 groups of 8 ROIs were then projected and reconstructed by the trained PCA model and thus generated the reconstructed errors. Five subjects from data set 1 were randomly chosen for this experiment. Additionally, the sampling range, that is, sizes of neighborhood, was considered as another parameter. The results in Figure 4 show the mean reconstruction error Dist_{pca} of each 100-group test. The mean trend line for each subject shows that the minima Dist_{pca} are always at the original ROI locations for each subject, suggesting that the ROIs identified by task-based fMRI have much less variation in terms of their spatial locations, in comparison to random samplings around their neighborhoods. As the random sampling range was enlarged, Dist_{pca} grows accordingly. This result demonstrates the validity of Dist_{pca} for use as the meaningful constraint and similarity measurement in ROI prediction.
In order to evaluate the effectiveness of Hausdorff metric for fiber bundles, we performed an experiment on the working memory data set to examine the similarity measurements between fiber bundles, as shown in Figure 5. For each benchmark ROI, we extracted fiber bundles for every vertex within its neighborhood. Then, Hausdorff metric Dist_{ij} were computed between those fiber bundles and the one extracted from the benchmark ROI itself. The local region $R_j^i$ used to extract fiber
bundle is 3-ring neighborhood size here. Afterward, the Hausdorff metrics were color coded and mapped onto the corresponding neighboring vertices. By visual inspection, a rough Gaussian-like distribution centered at the original ROI location (white arrows) can be found, which suggests that the shape pattern of fiber bundle is a distinctive feature and the Hausdorff metric $\text{Dist}_H$ is an effective measurement for fiber bundle similarity. In other words, a ROI's fiber bundle can distinguish itself from other neighbors. This characteristic of uniqueness is much desired in ROI search and prediction.

**Figure 8.** The impact of $\lambda$ on the prediction result. Values of $\lambda$ are labeled by the horizontal axis, while the prediction errors are represented by the vertical axis with the unit mm.

**Figure 9.** Fiber bundle illustration for ROI #1, #4, and #7 (sub-fig 1, sub-fig 2, and sub-fig 3). (a) Fiber bundles emanating from predicted ROI and benchmark ROI are overlapped; (b) Fiber bundles emanating from predicted ROI; (c) Fiber bundles emanating from benchmark ROI; (d–f) Template fiber bundles of ROI in the training data set. Yellow bubbles: benchmark ROI locations; Green bubble: predicted ROI locations.
selected subject from each data set in Figure 6 and Figure 7, respectively. Corresponding fiber bundles of 3 subjects randomly selected from the training subjects are also shown for comparison. It is evident that the fiber bundles of the predicted ROIs (column 5) are quite similar to those of the benchmark ROIs derived from task-based fMRI (column 4), indicating the effectiveness and accuracy of our ROI prediction framework. It is also evident that the fiber bundles of the predicted ROIs and benchmark ROIs are quite similar to those of the corresponding ROIs of the training subjects (column 1–3). These results reveal that there are consistent fiber connection patterns for corresponding functional ROIs in different brains, which provides the neuroscience foundation and technical feasibility for the work in this paper.

As an important parameter, the influence of $\lambda$ in the energy function equation (6) is explored. We tested it on one randomly selected subject in data set 1 by ranging $\lambda$ from 0.0 to 1.0, and the corresponding mean prediction errors of the 8 ROIs were computed and illustrated in Figure 8. We can observe that the prediction error is the smallest when $\lambda$ is around 0.3. Therefore, in this paper, $\lambda$ was assigned as 0.3 for all the experiments.

Notably, some ROIs (e.g., #1, #4, #7 in data set 1 and #1, #5, #8, #10 in data set 2) have relatively large prediction errors, and as an example, the corresponding fiber bundles of those in data set 1 (#1, #4, #7 in data set 1) are shown and examined in Figure 9. We can see that although the distance between the predicted ROI and the benchmark one is relatively large (7.29, 3.96, and 5.91 mm), their fiber bundle similarity is still high, either by the overlapping views (Fig. 9, 1a–3a) or separated views (Fig. 9, 1b–3b and Fig. 9, 1c–3c). This visualization suggests that our energy minimization procedure in ROI Prediction Framework might be trapped in a local minimum, thus resulting in those predicted ROIs converged to a wrong location with similar emanating fiber bundle. In the future, other constraint terms will be considered to further reduce the chance of being trapped in local minima during the energy minimization procedure.

Finally, the functional connectivity matrices between ROIs of one randomly selected subject from each data set were shown in Figure 10. The connectivity matrix was computed as follows: we mapped the ROIs into the fMRI data space, and for each ROI, functional signals from the 27-neighborhood voxels were extracted and averaged. The Pearson correlation was computed between any pair of ROIs. We computed the connectivity matrix for both the benchmark ROIs and the predicted ROIs. In Figure 10, only minor difference between $a$ and $b$, or $c$ and $d$, can be observed, demonstrating that the functional connectivity measured by our predicted ROIs is very close to the real connectivity. Importantly, the columns of the ROIs with relatively large prediction errors are highlighted, from which we can find that there is no direct relationship between the prediction error and functional connectivity changes.

### Comparison Studies

For the purpose of comparison, we conducted ROI prediction by linear (via FSL FLIRT), nonlinear registration (via the HAMMER software package [Shen and Davatzikos 2002]), and DTI registration approaches (denoted as DTI-Reg) (Yang et al. 2008). The prediction procedure is as follows. Taking the linear registration method for instance, we randomly chose a subject as a template from the training data set and registered its fMRI

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**Table 5**

Prediction errors by the FSL FLIRT, HAMMER, and DTI-based registration algorithm (mm)

<table>
<thead>
<tr>
<th>ROI</th>
<th>ROI 2</th>
<th>ROI 3</th>
<th>ROI 4</th>
<th>ROI 5</th>
<th>ROI 6</th>
<th>ROI 7</th>
<th>ROI 8</th>
<th>Mean</th>
</tr>
</thead>
<tbody>
<tr>
<td>FLIRT</td>
<td>7.48</td>
<td>4.95</td>
<td>6.24</td>
<td>6.18</td>
<td>5.41</td>
<td>4.51</td>
<td>6.46</td>
<td>4.54</td>
</tr>
<tr>
<td>HAMMER</td>
<td>6.18</td>
<td>4.92</td>
<td>6.40</td>
<td>7.50</td>
<td>5.15</td>
<td>3.06</td>
<td>6.08</td>
<td>4.95</td>
</tr>
<tr>
<td>DTI Reg</td>
<td>8.40</td>
<td>4.97</td>
<td>4.84</td>
<td>7.50</td>
<td>2.70</td>
<td>5.15</td>
<td>3.06</td>
<td>4.86</td>
</tr>
</tbody>
</table>

Note: Means across ROIs and subjects are in bold fonts.

### ROI Prediction

We used the leave-one-out strategy to evaluate the ROI prediction framework on the 2 data sets individually. In all the experiments, $\lambda$ was assigned as 0.3 in the global search. In this paper, we did not consider the impact of ROI size. Therefore, the local region $R_k^j$ centered at location of ROI $j$ on subject $i$’s surface and from which fiber bundle emanating was extracted, was uniformly assigned to be the size of 3-ring neighborhood.

As the subject to be predicted has task-based fMRI data, the fMRI-derived ROIs are used as the benchmark data to evaluate the ROI prediction results. Table 3 and Table 4 show the Euclidian distances between the predicted ROIs and the benchmark data for ROIs, that is, the prediction errors for all the leave-one-out experiments. Most of the prediction errors are approximately 2–4 mm, which is 1–2 voxels in DTI volumes. On average, the average prediction errors for ROIs are $3.99 \pm 2.18$ mm and $3.99 \pm 2.22$ mm in data set 1 and data set 2, respectively. It is interesting that there are ROIs (#2, #3, #6, #8 in data set 1 and #2, #4, #6, #9 in data set 2) that have average prediction errors below 3 mm, which is considered as very accurate.

To visualize the consistency of fiber bundles of the predicted ROIs, we showed the fibers emanating from predicted ROIs and fibers emanating from benchmark ROIs for one randomly

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**Figure 10.** Functional connectivities between ROIs. The color bar is at the bottom. (a) Functional connectivity matrix of the benchmark ROIs of one subject from data set 1. (b) Functional connectivity matrix of the predicted ROIs of one subject from data set 1. (c) Functional connectivity matrix of the benchmark ROIs of one subject from data set 2. (d) Functional connectivity matrix of the predicted ROIs of one subject from data set 2. The columns with relatively large prediction errors (#1, #4, #7 in data set 1 and #1, #5, #8, #10 in data set 2) are highlighted by black frames.
image and the corresponding ROI location into its DTI space. Then, we registered its fractural anisotropy image obtain from DTI data onto that of a subject from the testing data set via FSL FLIRT. Finally, the predicted ROIs were obtained by applying the registration transform on the ROI location of the template, and the distances between the predicted ROIs and benchmark ones from the testing subject were computed.

The mean prediction errors for the 3 methods are shown in Table 5. On average, the prediction errors by FSL FLIRT, HAMMER, and DTI Reg are 5.72, 5.53, and 4.94 mm, respectively. As can be seen, our method (3.94 mm) significantly outperforms them. The fiber bundles emanating from predicted ROIs using the 3 methods of one subject were shown in Figure 11. The differences in comparison with the benchmark ones can be easily inspected.

Conclusions
We presented a novel framework for functional brain ROI prediction using the working memory and vision networks as test beds. From the training subjects which include both DTI and fMRI data, we trained the model of ROI location distribution and the model of fiber bundles emanating from functionally cortical ROIs. Predicting ROIs on testing subjects was performed by matching the trained models onto the DTI data of individual subjects. This problem was formulated as an energy minimization one, in which fiber bundle shape and ROI location pattern were, respectively, considered as external and internal terms. Experimental results demonstrated that the ROI prediction framework has promising performance, in comparison to other methods based on linear and nonlinear image registration algorithms.

It should be noted that our ROI prediction framework might be trapped into local minima for some ROIs (as illustrated in Fig. 9), although global search is conducted. This may be caused by the fiber bundle similarity measurement (Hausdorff metric) used in this paper, which should be further investigated. Moreover, variability across subjects in terms of ROI's structural and anatomical locations and ROI size may be other reasons.
Therefore, in the near future, we plan to investigate improved metrics for fiber bundle similarity and model the variability of the ROI’s structural and functional profiles with ROI size problem considered. For instance, the group replicator dynamics approach (Ng et al. 2009) could possibly be used to model the variability of the structural and functional connectivities among the ROIs. Notably, our methods focus on the most consistent ROIs at current stage. In the future, we will consider adding other less consistent ROIs into the prediction framework and evaluate the performance of ROI prediction.

Currently, the computational pipeline takes around a few minutes in the training stage and, approximately, 4h in the prediction stage on a typical PC computing environment. It is worth noting that in the future, optimization strategies like developing robust fiber shape features that require less computation load and automatically pruning the search space could significantly reduce the computation load.

Our work has demonstrated that fiber bundle shape models of functional brain ROIs have remarkable prediction capability, providing direct support to the connective fingerprint concept (Passingham et al. 2002). In the future, we plan to apply and evaluate this ROI prediction framework in other brain networks, such as executive function, attention, and semantics memory systems and apply and validate this framework on clinical data sets such as the DTI data sets of Alzheimer’s disease and Autism.

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**References**


