Effects of surface-conditioning methods on shear bond strength of brackets bonded to different all-ceramic materials

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SUMMARY The aims of this study were to investigate the effects of two surface-conditioning methods on the shear bond strength (SBS) of metal brackets bonded to three different all-ceramic materials, and to evaluate the mode of failure after debonding. Twenty feldspathic, 20 fluoro-apatite, and 20 leucite-reinforced ceramic specimens were examined following two surface-conditioning methods: air-particle abrasion (APA) with 25 μm Al₂O₃ and silica coating with 30 μm Al₂O₃ particles modified by silica. After silane application, metal brackets were bonded with light cure composite and then stored in distilled water for 1 week and thermocycled (×1000 at 5–55°C for 30 seconds). The SBS of the brackets was measured on a universal testing machine. The ceramic surfaces were examined with a stereomicroscope to determine the amount of composite resin remaining using the adhesive remnant index. Two-way analysis of variance, Tukey’s multiple comparison test, and Weibull analysis were used for evaluation of SBS.

The lowest SBS was with APA for the fluoro-apatite ceramic (11.82 MPa), which was not significantly different from APA for the feldspathic ceramic (13.58 MPa). The SBS for the fluoro-apatite ceramic was significantly lower than that of leucite-reinforced ceramic with APA (14.82 MPa). The highest SBS value was obtained with silica coating of the leucite-reinforced ceramic (24.17 MPa), but this was not significantly different from the SBS for feldspathic and fluoro-apatite ceramic (23.51 and 22.18 MPa, respectively). The SBS values with silica coating showed significant differences from those of APA. For all samples, the adhesive failures were between the ceramic and composite resin. No ceramic fractures or cracks were observed. Chairside tribochemical silica coating significantly increased the mean bond strength values.

Introduction

The need to bond orthodontic brackets to a variety of dental restorations has become more common as the number of adult patients seeking orthodontic treatment steadily increases. Patients are increasingly demanding dental restorations that are both aesthetic and functional. Manufacturers have introduced numerous all-ceramic alternatives (Donovan, 2008). Therefore, the orthodontist is often confronted with the challenge of effectively bonding orthodontic brackets to different ceramic restorations.

The approaches suggested for bonding orthodontic brackets to ceramic restorations can be classified into three categories: mechanical, chemical, or a combination (Abu Alhaija and Al-Wahadni, 2007). Mechanical alteration of porcelain surfaces to increase bond strength has been achieved by air-particle abrasion (APA; Zachrisson et al., 1996; Cochran et al., 1997; Kocadereli et al., 2001) or by applying coarse diamond stones (Gillis and Redlich, 1998; Abu Alhaija and Al-Wahadni, 2007). Peterson et al. (1998) pointed out that mechanical roughening with diamond burs and APA provokes crack initiation on the ceramic surface. Following orthodontic treatment, ceramic restorations normally remain in the mouth, thus damage to the ceramic due to roughening during surface conditioning should be minimized (Schmage et al., 2003).

Chemical alteration of the porcelain surface can be achieved by either etching or changing the porcelain bonding affinity to adhesive materials (Abu Alhaija and Al-Wahadni, 2007). Etching the porcelain surface with hydrofluoric acid (HFA) to increase bond strength has been advocated (Zachrisson et al., 1996; Cochran et al., 1997; Bourke and Rock, 1999; Kocadereli et al., 2001; Abu Alhaija and Al-Wahadni, 2007). Clinically, there are drawbacks with the use of HFA (Abu Alhaija and Al-Wahadni, 2007). Due to the acidic and extremely corrosive nature and the capability of causing severe trauma to soft tissues and tooth substance, HFA has to be used with great care (Hayakawa et al., 1992).

Silane coupling agents, which are widely accepted as adhesion promoters in clinical practice enhance the bond strength by increasing the chemical bond between the resin composite and ceramic material (Wood et al., 1986; Kao et al., 1986; Kao and Peterson, 1986; Zachrisson et al., 1996; Cochran et al., 1997; Kocadereli et al., 2001). However, hydrofluoric acid has several drawbacks: it is extremely corrosive, cause severe damage to the ceramic surface (Peterson et al., 1998), and it is time-consuming and requires the use of special equipment and personal protective equipment (Abu Alhaija and Al-Wahadni, 2007).
and Johnston, 1991; Cochran et al., 1997; Chung et al., 1999; Huang and Kao, 2001; Kocadereli et al., 2001; Schmage et al., 2003).

Another abrasive method is tribochemical silica coating, which provides micromechanical retention and sites for chemical adhesion. The alumina particles that are chemically silica coated are blasted onto the metal surfaces (such as base metal, noble metal alloys, or titanium) and onto the polymeric resin composite or ceramic surfaces (Matelinna and Vallittu, 2007b). The particles form a reactive silica layer on the substrate, and, thereafter, silane must be applied for chemical bonding with a resin-based system (Hansson and Mober, 1993).

There are several types of porcelain for ceramic restorations: silica-based ceramics (e.g. feldspathic, fluorapatite, leucite-reinforced glass ceramics, lithium disilicate glass ceramics), glass-infiltrated or densely sintered aluminium oxide ceramics, and zirconium oxide ceramics (Blatz et al., 2003; Karan et al., 2007). However, only a limited number of studies exist concerning the bond strength of orthodontic brackets to different all-ceramic restorations (Chay et al., 2005; Türk et al., 2006; Abu Alhaija and Al Wahadni, 2007; Karan et al., 2007; Kukiattrakoon and Samruajbenjakul, 2010).

The objectives of this study were to observe the outcomes of two different surface-conditioning methods (sandblasting and tribochemical silica coating) on the shear bond strength (SBS) of metal orthodontic brackets to three different silica-based all-ceramic restorative materials (feldspathic, fluorapatite, and leucite reinforced), and to evaluate the mode of failure after debonding.

Materials and methods

A post hoc power calculation showed that for a power of 0.99, a sample of 20 ceramic specimens for each group would be required. Forty feldspathic (Vitatur Alpha; Vita Zahnfabrik, Bad Säckingen, Germany), 40 fluoro-apatite (IPS Eris layering material; Ivoclar Vivadent, Schaan, Liechtenstein), and 40 leucite-reinforced (IPS Empress Esthetic; Ivoclar Vivadent) ceramic specimens with a diameter of 6 mm and a thickness of 3 mm were fabricated and glazed according to the manufacturers’ recommendations. The specimens were embedded in autopolymerizing acrylic resin blocks (Meliodent; Heraeus Kulzer Ltd, Newbury, Berkshire, UK) with their glazed surfaces facing upwards. For each all-ceramic material, the specimens were randomly divided into two groups according to random number tables. Each group consisted of 20 specimens and two different surface-conditioning methods were used. In the first group, APA was performed using 25 μm aluminium trioxide (Al2O3) with an air abrasion device (Bego TopTec; Bego, Germany) at a distance of approximately 10 mm and a pressure of 2.5 bars for 4 seconds. In the second group, the surfaces were treated with APA with 30 μm Al2O3 particles modified by silica (CoJet Sand; 3M-Espe, Seefeld, Germany), using an intraoral device (Microetcher; Danville Eng., San Ramon, California, USA). APA was used with a nozzle distance of approximately 10 mm from the surface at an angle of 90 degrees for 4 seconds at 3 psi.

Subsequently, silane and the adhesive primer (Transbond XT; 3M Unitek, Monrovia, California, USA) were applied to all roughened specimens. The light cure adhesive paste (Transbond XT; 3M Unitek) was applied to the mesh base of a maxillary central incisor bracket (Gemini bracket; 3M Unitek). The bracket was then seated and positioned manually on the ceramic surface. Excess composite was carefully removed from the periphery of the bracket base with an explorer. The surface-conditioning methods and the placement of the brackets were performed by two operators, YSS and TT, respectively. The adhesive paste was cured for a total of 20 seconds from two directions using a visible light-curing unit (Hilux 200; Bensioglu Dental Inc., Ankara, Turkey) with an output of 600 mW/cm2. All specimens were stored in distilled water at 37 ± 2°C for 1 week. The specimens were thermocycled 1000 times between 5 and 55°C with a dwelling time of 30 seconds. The shear bond test was performed with a universal testing device (Lloyd LRX; Lloyd Instruments Ltd, Fareham, Hants, UK) at a crosshead speed of 1 mm/minute. The bond strengths were calculated in megapascals (MPa).

The ceramic surfaces were examined with a stereomicroscope (Stemi 2000-C; Carl Zeiss, Göttingen, Germany) at a magnification of ×10 to determine the amount of composite resin remaining according to the adhesive remnant index (Årtun and Bergland, 1984) and to assess the damage to the ceramic which may have occurred during shear bond testing.

To evaluate the effect of surface-conditioning methods on the ceramic surfaces, three additional feldspathic, three fluoro-apatite ceramic, and three leucite-reinforced ceramic specimens were prepared and glazed. The surfaces of two specimens of each ceramic were then conditioned with the same experimental protocol described above. Two roughened specimens for each ceramic were gold sputtered with a sputter coater (S150B; Edwards, Crawley, Sussex, UK) and examined under a field emission scanning electron microscope (SEM, JSM-6335F; Jeol, Tokyo, Japan) at 20.0 kV. The SEM photomicrographs were taken at ×500 magnification for visual inspection.

Two-way analysis of variance (ANOVA) was used to determine significant differences among all-ceramic materials and surface-conditioning methods and their interactions. All treatment combination means for bond strength values were compared using the Tukey’s multiple comparison test \( P < 0.05 \).

A Weibull analysis was performed, and the Weibull modulus, characteristic bond strength, correlation coefficient, and the stress levels at 5 and 10 per cent probability of failure were calculated.
Results

The results of the two-way ANOVA are shown in Table 1. The main effects were significant differences for the surface-conditioning methods and all-ceramic materials on the SBS values ($P < 0.001$; Table 1). The interaction between the conditioning methods and ceramic materials was not significant ($P > 0.05$; Table 1).

The mean SBS, minimum and maximum values, and standard deviations (SDs) for each group are presented in Table 2. For each group, box plots of the SBSs are presented in Figure 1. The results of the Tukey’s multiple comparison test for the mean SBS values are given in Table 2.

The lowest SBS was with APA for the fluoro-apatite ceramic (11.82 MPa), which was not significantly different from APA for the feldspathic ceramic (13.58 MPa). The SBS for the fluoro-apatite ceramic was significantly lower than for the leucite-reinforced ceramic with APA (14.82 MPa).

The highest SBS values were obtained with silica coating of the leucite-reinforced ceramic (24.17 MPa), but these were not significantly different from the SBS for feldspathic and fluoro-apatite ceramic (23.51 and 22.18 MPa, respectively). The SBS values obtained with silica coating showed significant differences from that obtained with the APA.

The parameters of the Weibull analysis for each group are given in Table 1. The Weibull distribution plots of the probability of failure at a certain shear stress level for the two groups are depicted in Figure 2.

The modes of bond failure for the brackets after different surface-conditioning methods are given in Table 3. Adhesive failures between the ceramic and adhesive resin were found in all groups. No cracks or fractures of the ceramic surfaces were observed.

Scanning electron photomicrographs of the feldspathic, fluoro-apatite, and leucite-reinforced ceramic surfaces conditioned using different methods are presented in Figure 3. APA with 25 $\mu$m $\text{Al}_2\text{O}_3$ particles demonstrated slightly more prominent irregularities and deeper erosions (Figure 3A, 3C, and 3E). However, the silica-coating procedure created superficial irregularities and shallow erosions on the surface. The white spots, observed on the surface, were silica (Figure 3B, 3D, and 3F).

Discussion

The results of the present study confirm that surface-conditioning methods and the type of the all-ceramic materials affect the bond strength of metal orthodontic brackets to ceramic surfaces. These results support previously published studies on this topic (Türk et al., 2006; Abu Alhaija and Al-Wahadni, 2007; Karan et al., 2007; Kukiatrakoon and Samruajbenjakul, 2010).

Table 1 Two-way analysis of variance of force (Megapascals) required to debond metal brackets from dental ceramic.

<table>
<thead>
<tr>
<th>Source of variation</th>
<th>Mean square</th>
<th>df</th>
<th>Sum of squares</th>
<th>F ratio</th>
<th>Significance</th>
</tr>
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<tbody>
<tr>
<td>Ceramic</td>
<td>63.410</td>
<td>2</td>
<td>126.820</td>
<td>9.229</td>
<td>0.000</td>
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<tr>
<td>Surface conditioning</td>
<td>2929.543</td>
<td>1</td>
<td>2929.543</td>
<td>426.396</td>
<td>0.000</td>
</tr>
<tr>
<td>Ceramic × surface conditioning</td>
<td>2.564</td>
<td>2</td>
<td>5.127</td>
<td>0.373</td>
<td>0.689</td>
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<tr>
<td>Error</td>
<td>6.870</td>
<td>114</td>
<td>783.233</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Corrected total</td>
<td>3844.724</td>
<td>119</td>
<td></td>
<td></td>
<td></td>
</tr>
</tbody>
</table>

Table 2 Mean shear bond strengths, standard deviations (SDs), minimum (Min) and maximum (Max) values, and Weibull parameters for each group ($n = 20$).

<table>
<thead>
<tr>
<th>Groups</th>
<th>Mean*</th>
<th>SD</th>
<th>Min</th>
<th>Max</th>
<th>Weibull modulus</th>
<th>Correlation coefficient</th>
<th>Characteristic bond strengths (MPa)</th>
<th>Shear stress at the 5% probability of failure (MPa)</th>
<th>Shear stress at the 10% probability of failure (MPa)</th>
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<tr>
<td>Air-particle abrasion</td>
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<td></td>
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<td></td>
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<tr>
<td>Feldspathic</td>
<td>13.58 A</td>
<td>2.56</td>
<td>10.36</td>
<td>18.51</td>
<td>4.95</td>
<td>0.91</td>
<td>16.82</td>
<td>9.23</td>
<td>10.68</td>
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<tr>
<td>Fluoro-apatite</td>
<td>11.82 A</td>
<td>2.06</td>
<td>9.61</td>
<td>15.97</td>
<td>5.12</td>
<td>0.85</td>
<td>14.57</td>
<td>8.16</td>
<td>9.40</td>
</tr>
<tr>
<td>Leucite reinforced</td>
<td>14.82 B</td>
<td>1.99</td>
<td>11.63</td>
<td>18.39</td>
<td>7.05</td>
<td>0.93</td>
<td>17.28</td>
<td>11.43</td>
<td>12.55</td>
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<tr>
<td>Silica-coating</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Feldspathic</td>
<td>23.51 C</td>
<td>3.11</td>
<td>17.82</td>
<td>27.70</td>
<td>7.17</td>
<td>0.98</td>
<td>27.33</td>
<td>18.07</td>
<td>19.97</td>
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<td>Fluoro-apatite</td>
<td>22.18 C</td>
<td>2.71</td>
<td>19.10</td>
<td>26.93</td>
<td>7.30</td>
<td>0.86</td>
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<td>17.14</td>
<td>18.93</td>
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<tr>
<td>Leucite reinforced</td>
<td>24.17 C</td>
<td>3.08</td>
<td>18.09</td>
<td>27.70</td>
<td>7.46</td>
<td>0.98</td>
<td>27.94</td>
<td>18.76</td>
<td>20.66</td>
</tr>
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*Means for groups having the same letters show homogeneous subsets, alpha = 0.05
Glazed porcelain surfaces are not amenable to resin penetration for orthodontic bonding (Smith et al., 1988). For successful bonding of orthodontic brackets to porcelain, mechanical or chemical removal of the glazed surface is essential to obtain mechanical interlocking. A tensile bond strength value of 6–8 MPa would be adequate to resist treatment forces (Reynolds, 1975). In this study, the SBS values obtained with APA were above this clinically acceptable level. Nevertheless, silica coating showed higher SBS values than APA. APA is used to roughen the ceramic surface to increase the amount of bonding area and mechanical locking. Silica-coating systems are used to produce a silica layer on the ceramic surface with the aid of the high-speed surface impact of the alumina particles modified by silica followed by silanization (Della Bona, 2005). The tribochemical effect of the silica-coating system may be explained by two bonding mechanisms: 1: the creation of a topographic surface allowing for micromechanical bonding to resin and the chemical bond of the silica-coated ceramic surface, the silane agent, and the resin material (Della Bona, 2005). Sun et al. (2000) reported that the components of the blasting abrasive can penetrate into the metal to a depth of 15 μm. The third step of the tribochemical system is to apply silane on the treated surfaces. After silica coating, the silica layer on the ceramic surface provides a base for silane. An immediate silane application forms covalent bonding between the silica-coated ceramic layer and resin composite (Matinlinna and Vallittu, 2007a). Moreover, the silane also contributes to the improved surface wettability to resin (Thurmond et al., 1994; Della Bona et al., 2004). For enhanced clinical success, the use of a silane coupling agent for creating long-term bonds of resin to ceramic has been suggested (Matinlinna and Vallittu, 2007a). All these findings may explain the higher SBSs with silica coating compared with APA.
found that the highest SBS values between the composite and ceramic/composite interface are preferred to avoid ceramic fractures during debonding (Smith et al., 1988).

The Weibull analysis conveys information concerning the probability of bracket failure and presents the orthodontist with an indication of how the material or bracket is likely to perform in a clinical situation, i.e. the oral environment (Fox et al., 1994). Littlewood et al. (2001) suggested using the 5 per cent chance of failure as a more appropriate level to assess bond strength. According to those authors, the bond strength of a material with a 5 per cent chance of failure should be at least 5.4 MPa. In the present study, SBS showed shear stress levels higher than 5.4 MPa at the 5 per cent probability of failure for all groups. This result suggests acceptable SBS for all groups in the oral environment. Nevertheless, as with any in vitro study, discretion should be exercised when attempting to extrapolate laboratory findings to the clinical setting.

Conclusions

1. Chairside tribochemical silica coating significantly increased mean bond strength values.
2. With all surface-conditioning methods, leucite-reinforced ceramic, in general, showed a higher SBS than feldspathic and fluoro-apatite ceramics.
3. For all samples, the adhesive failures were between the ceramic and composite resin. No ceramic fractures or cracks were observed.

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Karan et al. (2007) found that the highest SBS values were achieved with silica coating on three different ceramics (feldspathic, lithium disilicate, and leucite-reinforced). They concluded that silica-coating could replace other conditioning techniques in bonding brackets to ceramic. Ozcan et al. (2004) also observed that brackets treated with silica coating had significantly greater bond strengths on tested feldspathic porcelain.

When the results of the study are considered in terms of the type of the all-ceramics, both surface treatments increased bond strength. There was no statistical difference between the veneering materials, feldspathic, and fluoro-apatite ceramics, but bond strength values were higher for leucite-reinforced ceramic. This was probably due to microstructural differences, processing techniques, and the more porous structure of the veneering materials. However, leucite-reinforced ceramic is processed by heat-press techniques and is based on extremely homogeneous and increased density of the crystals (Oh and Shen, 2003, 2005; Shen et al., 2004).

For all samples, adhesive failures between the ceramic and composite resin were observed in the present study. This type of adhesive failure demonstrates that the bond strength between the composite and bracket and the cohesive strength of the composite was stronger than the bond strength between the composite and ceramic. Adhesive failures at the ceramic/composite interface are preferred to avoid ceramic fractures during debonding (Smith et al., 1988).

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Figure 3 Scanning electron photomicrographs: (A) Feldspathic ceramic—air-particle abrasion (APA) with 25 μm Al₂O₃, (B) Feldspathic ceramic—silica coating with 30 μm SiO₂, (C) Fluoro-apatite ceramic—APA with 25 μm Al₂O₃, (D) Fluoro-apatite ceramic—silica coating with 30 μm SiO₂, (E) Leucite-reinforced ceramic—APA with 25 μm Al₂O₃, (F) Leucite-reinforced ceramic—silica coating with 30 μm SiO₂. Original magnification ×500 and bar = 10 μm.
Karan S, Büyükyılmaz T, Toroğlu M S 2007 Orthodontic bonding to several ceramic surfaces: are there acceptable alternatives to conventional methods? American Journal of Orthodontics and Dentofacial Orthopedics 132: 7–14