Effect of Age and Glaucoma on the Detection of Darks and Lights

Linxı Zhao,1 Caroline Sendek,1 Vandad Davoodnia,2 Reza Lashgari,2 Mitchell W. Dul,1 Qasım Zaidı,1 and Jose-Manuel Alonso1

1Department of Biological and Visual Sciences, State University of New York, College of Optometry, New York, New York, United States
2School of Cognitive Sciences, Institute for Research in Fundamental Sciences, Tehran, Iran

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METHODS. We asked 21 glaucoma patients, 21 age-similar controls, and 5 young control observers to report as fast as possible the number of 1 to 3 light or dark targets. The targets were positioned at random in a binary noise background, within the central 30° of the visual field.

RESULTS. We replicate previous findings that darks are detected faster and more accurately than lights. We extend these findings by demonstrating that differences in detection of darks and lights are found reliably across different ages and in observers with glaucoma. We show that differences in detection time increase at a rate of approximately 55 msec/db at early stages of glaucoma and then remain constant at later stages at approximately 800 msec. In normal subjects, differences in detection time increase with age at a rate of approximately 8 msec/y. We also demonstrate that the accuracy to detect lights and darks is significantly correlated with the severity of glaucoma and that the mean detection time is significantly longer for subjects with glaucoma than age-similar controls.

CONCLUSIONS. We conclude that differences in detection of darks and lights can be demonstrated over a wide range of ages, and asymmetries in dark/light detection increase with age and early stages of glaucoma.

Keywords: retina, thalamo-cortical, light-dark, perimetry, psychophysics

Visual information travels from the eye to the rest of the brain through two major pathways that signal light increments (ON) and decrements (OFF) in local regions of visual space. In mammals, ON and OFF channels remain segregated in the thalamus and combine for the first time in visual cortex. However, ON-OFF cortical mixing is incomplete and unbalanced. Although single cortical neurons receive input from both channels, ON and OFF thalamic afferents segregate in different cortical domains1–4 and cortical current sinks generated by OFF thalamic afferents are stronger and occupy larger territory than those generated by ON afferents.4 Moreover, cortical responses to dark stimuli are stronger, faster, more linearly related to luminance contrast, and have better spatial and temporal resolution than responses to light stimuli.5–10 Consistent with these physiological differences, dark targets are detected faster and more accurately than light targets on noisy backgrounds.11,12 and dark pixels have a more important role in judgments of texture variance than light pixels.13,14

Although dark/light asymmetries are most pronounced in visual cortex,1,6–8,10–13 they also are significant in the retina14,15,20–22 and possibly originate in photoreceptor outputs.13 Therefore, diseases that disrupt retinal function, such as glaucoma, could affect the dark/light asymmetries in visual perception. Glaucoma is a progressive disease that affects retinal ganglion cells and often results in loss of sensitivity in the visual field, especially within the central 30° of fixation.14,15 Glaucoma also has been shown to affect temporal processing16–18 and can have a profound effect on quality of life.19–21 To investigate if dark/light asymmetries are affected by glaucoma within the central 30° of fixation, we asked human observers to report the number of dark or light targets presented in binary noise on a monitor screen. Our results demonstrated that darks are detected more accurately and faster than lights in control observers and observers with glaucoma. Moreover, we showed that these dark/light asymmetries increase with age and in the early stages of glaucoma.

METHODS

We recruited 21 patients with open angle glaucoma (48–83 years old; mean, 64.7 ± 7.5 years old), 21 control observers with a similar age range (49–74 years old; mean, 62.2 ± 7.3 years old), and 5 young control observers (21–25 years old). The study was performed following the principles outlined in the Declaration of Helsinki. The inclusion criteria for all groups were: best corrected visual acuity of at least 0.2 logMAR units (approximately 20/30), spherical equivalent refractive error within –6 to +2 diopters (D), cylinder correction within 3 D, clear ocular media, and absence of
known eye disease following a comprehensive eye examination (except for glaucoma in the patient group). The exclusion criteria for all groups were: ocular or systemic disease known to affect the visual field, such as diabetic retinopathy (except glaucoma in the patient group), history of intraocular surgery (except uncomplicated cataract surgery more than 1 year before enrollment or glaucoma surgery in the patient group), and use of medications known to affect vision. Additional exclusion criteria for control observers were a self-reported, first-degree relative with glaucoma and intraocular pressure > 21 mm Hg for two or more clinic visits. No exclusions were based on sex or race. The degree of glaucoma in each patient was based upon the results of static automated perimeter testing performed with the Humphrey Visual Field Analyzer II (Carl Zeiss Meditec, Inc., Dublin, CA, USA), using 24-2 SITA Standard algorithm. It was quantified as the total mean deviation of visual sensitivity in decibels and varied from normal to severe (1.2 to −22.21 dB; mean, −4.76 ± 5.8 dB). We did not measure sensitivity at the fovea and our most central stimulus was 3° away from fixation. In an initial recruitment of 11 glaucoma subjects, we selected a wide range of visual field defects spanning from normal to severe, and found significant differences in accuracy and reaction time between glaucoma subjects and age-similar controls. Based on this sample and power analysis ("sampsizepwr," MATLAB; MathWorks, Natick, MA, USA), we estimated that we would need a sample of 32 subjects (16 control and 16 glaucoma) to reveal significant differences between glaucoma and age-similar controls (e.g., effect size for reduction in dark/light accuracy, 7.1 ± 5.96/10.69 ± 11.54%; power, 0.9; alpha, 0.05; sample size required, 31). To fulfill the requirements of the power analysis, we selected a sample of 42 subjects (21 age-similar controls and 21 glaucomatous patients).

Observers were asked to report as fast as possible the number of square targets embedded in a background of binary white noise consisting of equal numbers of dark and light elements. The number of targets could be one, two, or three, and were either all dark or all light. Stimuli were presented on a monitor screen and observers had to press a key to indicate the number of targets that they saw (Fig. 1). Each time a key press was registered, an auditory tone signaled the progression onto the next trial. Therefore, the duration of each screen was determined by the observer's reaction time. Stimuli were presented using MATLAB and Psych-toolbox31 on a gamma calibrated monitor (Mitsubishi DP2070SB or Display ++ LCD). The monitor covered 23.0° × 30.5° of visual angle at a distance of 1 m and each stimulus target was 1.0° × 1.0° in size. The mean luminance of the monitor was kept constant at 50 candelas per square meter. Each observer was tested monocularly after being properly refractioned. Experiments were conducted in a dark room. Before the testing started, observers were visually adapted to a gray screen for 15 seconds.

A total of 600 to 800 reaction times was collected for each observer in an hour-long session. Observers were given a series of 100 trials at a time followed by a short break. Reaction time histograms (bin size 0.2 s) were averaged and fitted using an exponential-Gaussian function.32 This function assumes that histograms (bin size 0.2 s) were averaged and fitted using an equation of 100 trials at a time followed by a short break. Reaction time was determined by the observer's reaction time. Stimuli were presented using MATLAB and Psych-toolbox31 on a gamma calibrated monitor (Mitsubishi DP2070SB or Display ++ LCD). The monitor covered 23.0° × 30.5° of visual angle at a distance of 1 m and each stimulus target was 1.0° × 1.0° in size. The mean luminance of the monitor was kept constant at 50 candelas per square meter. Each observer was tested monocularly after being properly refractioned. Experiments were conducted in a dark room. Before the testing started, observers were visually adapted to a gray screen for 15 seconds.

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$$f(x|\mu, \sigma, \tau) = \frac{1}{\tau} \exp\left(\frac{\mu - x}{\sigma} - \frac{\mu^2 - x^2}{2\sigma^2}\right) \left(1 + \frac{x - \mu}{\sigma} - \frac{x^2 - \mu^2}{2\sigma^2}\right)$$

The parameters of the equation are the mean (μ) and standard deviation (σ) of the Gaussian function and the mean of the exponential function (τ).

**RESULTS**

Previous studies17 demonstrated that observers are faster and more accurate at counting dark than light targets embedded in binary noise (Fig. 1). We used the same method to investigate the extent in which this dark/light asymmetry is affected by age and glaucoma. To measure observer performance, we plotted the number of correct trials as a function of the reaction time and fitted the distributions with a Gaussian-Exponential function (see Methods). Control observers (Fig. 2A) and observers with glaucoma (Fig. 2B) were faster and more accurate at counting dark than light targets. In control observers, accuracy was not correlated with age (Fig. 3A; accuracy versus age for darks, r = 0.052, P = 0.799; lights, r = 0.289, P = 0.270; darks-lights, r = −0.359, P = 0.072). In glaucomatous observers, we found a weak correlation between accuracy and age but only for dark targets (Fig. 3B; accuracy versus age for darks, r = −0.488, P = 0.025; lights, r = −0.285, P = 0.210; darks-lights, r = −0.053, P = 0.888).

Reaction time was correlated with age in control observers (Fig. 3C; darks, r = 0.649, P = 0.0003; lights, r = 0.606, P = 0.001) but not in observers >49 years old (Fig. 3C; darks, r = 0.120, P = 0.603; lights, r = 0.136, P = 0.556) or in glaucoma observers (Fig. 3D; darks, r = 0.038, P = 0.869; lights, r = −0.107, P = 0.645). Differences in reaction time between lights and darks also were correlated significantly with age in control observers (lights-darks, r = 0.422, P = 0.032) but not in observers older than 49 years (lights-darks, r = 0.117, P = 0.613) or glaucomatous observers (r = −0.248, P = 0.279).

On average, observers were more accurate at detecting darks than lights. The difference in accuracy between darks and lights was 8.08% in control observers (Fig. 4A; darks, 95.59% ± 4.69%; lights, 87.51% ± 9.4%; P = 0.0002, Wilcoxon test), 7.01% in age-similar controls (darks, 95.85% ± 4.23% versus lights, 88.84% ± 0.57%; P = 0.0005, Wilcoxon test) and 7.05% in glaucoma observers (darks, 93.06% ± 6.55%; lights, 86.55% ± 10.6%; P = 0.015, Wilcoxon test). The accuracy was only 2.2% better in age-similar controls than glaucomatous observers (Fig. 4A; darks, 95.85% ± 4.23% vs. 93.06% ± 6.55%; P = 0.579; lights, 88.84% ± 0.57% vs. 86.55% ± 10.6%; P = 0.443, Wilcoxon tests), a finding that is not surprising given that most of the glaucoma subjects were at early stages of the disease. If we selected glaucoma subjects with the greatest visual field loss (mean deviation < −6), their accuracy was 6.6% lower than the age-similar controls for dark targets (95.85% ± 4.23% vs. 95.59% ± 4.69%; P = 0.02, Wilcoxon test) and 15.75% lower for light targets (87.51% ± 9.4% vs. 73.09% ± 26.85%; P = 0.03, Wilcoxon test).

Differences in detecting darks and lights also could be demonstrated in measurements of reaction times (Fig. 4B). The difference in reaction time between darks and lights was 0.53 seconds in control observers (darks, 1.39 ± 0.41 seconds; lights, 1.92 ± 0.66 seconds; P = 0.002, Wilcoxon test), 0.6 seconds in age-similar controls (darks, 1.52 ± 0.34 seconds; lights, 2.12 ± 0.58 seconds; P = 0.011, Wilcoxon test), and 0.82 seconds in glaucomatous observers (darks, 1.84 ± 0.54 seconds; lights, 2.66 ± 0.84 seconds; P = 0.0009, Wilcoxon test). The differences between control and glaucomatous observers were significant for light targets and approached significance for dark targets (Fig. 4B; darks, 1.52 ± 0.34 vs. 1.84 ± 0.54 seconds; P = 0.053; lights, 2.12 ± 0.58 vs. 2.66 ± 0.84 seconds; P = 0.036, Wilcoxon tests). Moreover, if we selected glaucomatous subjects with the greatest visual field loss (mean deviation < −6), the differences in reaction time became more pronounced and were significant for light and dark targets (darks, 1.52 ± 0.34 vs. 2.07 ± 0.43 seconds; P = 0.019; lights, 2.12 ± 0.58 vs. 3.09 ± 0.58 seconds; P = 0.009, Wilcoxon tests). The severity of the disease was significantly
correlated with detection accuracy (Fig. 5A; darks, \( r = 0.531, P = 0.013 \); lights, \( r = 0.491, P = 0.024 \)) but not with reaction time (Fig. 5B; darks, \( r = -0.379, P = 0.089 \); lights, \( r = -0.348, P = 0.122 \)). However, the correlations with reaction time reached significance if we selected the glaucomatous subjects with the most limited visual field loss (mean deviation > −3; darks, \( r = -0.57, P = 0.014 \); lights, \( r = -0.529, P = 0.023 \)).

The analyses described above revealed pronounced differences in accuracy and detection time between dark and light targets in all subject groups, significant differences between glaucoma subjects and age-similar controls and a correlation between the severity of glaucoma and visual performance, for accuracy and reaction time. To further investigate changes in the dark/light asymmetry with age and glaucoma, we used a method of moving average. To study the effect of age, we used an average sliding window with a fixed border at the oldest age and another border that moved with each increase in age within our sample. To study the effect of glaucoma progression, we placed the fixed border at the highest value of visual sensitivity and the other border moved with each reduction in sensitivity within our sample. These analyses measured how the average reaction time changed as we narrowed the range of ages (or visual sensitivities) from a full range to a range without one of the values, two of the values, and so forth. By fitting the average values obtained with these analyses to linear functions, we found that the reaction time increased faster with age for light than dark targets (Fig. 6A; lights, 23 msec/y, \( r^2 = 0.9495 \); darks, 15 msec/y, \( r^2 = 0.9344 \)) with an average difference of 8 msec/y (Fig. 6B, \( r^2 = 0.9065 \)). Notably, reaction times also increased faster for light than dark targets with glaucoma progression (Fig. 6C; lights, 230 msec/dB, \( r^2 = 0.8127 \); darks, 170 msec/y, \( r^2 = 0.765 \)) with an average difference of 55 msec/dB (\( r^2 = 0.7448 \)), but only at early stages of glaucoma (>−4 dB of mean deviation in visual sensitivity). At later stages, the change in reaction time slowed down by more than one order of magnitude for lights and darks (lights, 4 msec/dB, \( r^2 = 0.5269 \); darks, 4 msec/dB, \( r^2 = 0.8376 \)).

In summary, our results indicated that the difference in reaction time between lights and darks increases at a rate of approximately 55 msec/dB at early stages of glaucoma (Fig. 6D) and then remains constant at later stages at approximately 800 msec difference. It should be noted that a similar analysis revealed a negligible reduction in accuracy with age.
in age-similar controls (lights, 0.1%/y, $r^2 = 0.6731$; darks, 0.04%/y, $r^2 = 0.0428$) and a similar reduction in accuracy for darks and lights in subjects at early stages of glaucoma (darks, 0.7%/dB, $r^2 = 0.7898$; lights, 0.5%/dB, $r^2 = 0.3869$; mean deviation of visual sensitivity $> -4$ dB). At later stages of glaucoma, the reduction in accuracy was still limited but seemed more pronounced for light than dark targets (darks, 0.08%/dB, $r^2 = 0.9679$; lights, 0.2%/dB, $r^2 = 0.9148$).

**DISCUSSION**

We demonstrated that dark targets are perceived faster and more accurately than light targets in subjects spanning a wide range of ages (21–83 years old) that had normal vision or glaucoma. We also demonstrated that glaucoma alters this dark/light asymmetry by affecting the time and accuracy of detection. The reduction in detection accuracy was found mostly in subjects with advanced glaucoma and could be

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**FIGURE 3.** Correlations between age and task performance. Age was weakly correlated with accuracy and reaction time. (A) The correlations between age and accuracy were not significant in control subjects. (B) In glaucomatous subjects, the correlations were only significant for dark targets ($r = -0.488, P = 0.025$). (C, D) The correlations between age and reaction time were significant for lights ($r = 0.649, P < 0.001$) and darks ($r = 0.606, P = 0.001$) in control observers (C) but not in glaucomatous observers (D) or in control observers that were >49 years old (C).

**FIGURE 4.** Darks are perceived more accurately and faster than lights in observers with normal vision and observers with glaucoma. (A) Accuracy (percent of correct responses) was higher for darks (dark bars) than lights (light bars). (B) Reaction time was faster for darks than lights. The difference in reaction time between observers with normal vision and glaucoma reached significance only for light targets. The histograms illustrate means and standard errors of the mean. ***$P < 0.001$, **$P < 0.01$, *$P < 0.05$, not significant (ns) $P > 0.05$. Wilcoxon tests.
accounted for, in part, by the presence of visual field scotomas. Since the locations of our stimuli were selected randomly, targets that fell by chance within a scotoma had less of a chance of being perceived than targets falling in unaffected regions. Our findings support the notion that darks are processed faster,11,12 have access to more neuronal resources than light targets,4,6–10,12,13,20,21 and that dark/light asymmetries in sensory processing are present across different ages and in retinal disease. It also should be noted that, although response asymmetries in visual search have been studied extensively33–37 and are known to be influenced by the background,38,39 the use of a random-noise background (with only target and distractor colors)17,40 is important because it rules out asymmetries due to experimental design.

Glaucoma is a disease that causes degeneration of retinal ganglion cells frequently in association with increased intraocular pressure.23,41–44 The finding that dark/light asymmetries become more pronounced in glaucoma indicates that the disease may affect differently the ON and OFF pathways. There is strong evidence indicating that the detection of dark targets is mediated mostly by the OFF pathway and the detection of light targets mostly by the ON pathway.12 Visual responses are stronger, faster,
and more temporally precise in OFF- than ON-center neurons if the targets are dark and vice versa if the targets are light. Also, ON and OFF pathways are known to remain segregated in visual cortex and, without the ON pathway, monkeys and humans fail to detect light targets but not dark targets.

Early studies claimed that large ganglion cells were more affected in glaucoma. However, other studies found evidence for cell shrinkage in multiple cell types rather than selective cell-type loss. Because ON retinal ganglion cells have larger dendritic fields than OFF retinal ganglion cells, the ON pathway would be expected to be more affected if the largest cells were more vulnerable in glaucoma. Therefore, if glaucoma caused selective degeneration of the larger ON cells in peripheral retina, it would be expected to make the reaction time increase more for light than dark targets. Consistent with this hypothesis, visual evoked potentials are more affected in glaucoma subjects when measured with positive than negative luminance contrast and our results also revealed the strongest increase in reaction time when using light targets. On the other hand, because cortical responses to dark stimuli are stronger and have better spatial resolution than cortical responses to light stimuli, dark stimuli may be more appropriate to map the borders between glaucomatous and normal regions in the visual field.

It is important to note that measurements of reaction time and accuracy are closely related. Our results suggested that, as ganglion cell pathology progresses within an early stage of the disease, the reaction times increase very rapidly (170–230 msec/db), keeping the accuracy loss restricted to less than 1%/db. However, as the disease progresses even further, the reaction times stop increasing and the accuracy loss becomes more noticeable (15.75% for light targets). It also is important to emphasize that our measurements were obtained in observers >48 years old that had lived with glaucoma over several years. A recent study has demonstrated that, a few days after inducing elevated intraocular pressure in mice, the most affected retinal ganglion cells have dendrites in the OFF sublamina of the inner plexiform layer. In the future, it will be interesting to investigate the differences in the detection of darks and lights near the onset of the disease. However, this study will require a large sample of subjects. To meet this challenge, we have developed a mobile app, “eye speed,” that will allow any clinician across the world to measure dark/light asymmetries and monitor disease progression using our visual test. The mobile app is freely available and takes advantage of the fact that our stimuli are binary (black or white) and do not require screen calibration. That is, the mid-gray background adaptation used in the experiments reported here is equivalent to the background of the mobile app, which is made of an equal number of black and white squares. The response time does vary across mobile devices, but differences between darks and lights can be reproduced with android and iOS versions of the app.

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