Alters in White Matter Evident Before the Onset of Psychosis

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Introduction

Functional neuroimaging studies suggest that there are alterations in the functional connectivity between different brain regions in schizophrenia and that these abnormalities are evident at the first episode of illness and in people at ultra high risk (UHR) of developing psychosis. Similarly, structural neuroimaging studies have shown that there are global and regional changes in white matter (WM) volume in schizophrenia and that these are also evident at the onset of psychosis and in UHR subjects. Approximately 20%–40% of people at UHR of psychosis develop psychosis within 24 months, and this subgroup shows more marked reductions in gray matter volume in the inferior frontal and medial temporal cortex at presentation than UHR subjects who do not subsequently develop psychosis. Furthermore, repetition of scanning in these subjects indicates that some of these baseline abnormalities progress with the later transition to psychosis and that these longitudinal magnetic resonance imaging (MRI) changes are not evident in UHR subjects who do not become psychotic. However, the extent to which these gray matter changes are related to alterations in WM integrity is unclear.

Diffusion tensor imaging (DTI) can measure the direction and degree of water diffusion as well as its anisotropy (ie, its relative value along ordered structures such as axon bundles vs across them). Anisotropy (commonly reported as fractional anisotropy [FA]) can be altered by pathologic factors, such as demyelination and axonal membrane deterioration, and so is often used as an index of WM integrity. The diffusivity along axons provides complementary information regarding WM structure. The axial (parallel) diffusivity corresponds to the amount of diffusion measured along the direction of principal

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diffusion, while the radial (perpendicular) diffusivity corresponds to the average diffusion in the perpendicular plane. Axial and radial diffusivity have recently been reported to change following axonal degeneration and demyelination in animal models; however, there is no evidence as to whether this holds true in humans.

Several DTI studies have reported reduced WM integrity in chronic schizophrenia, particularly in tracts connecting the frontal and temporal lobes, as well as in first-episode psychosis (FEP). There have only been a few DTI studies in subjects at UHR of psychosis. These have been limited to cross sectional comparisons and have given inconsistent results. One study reported a reduction of FA in the WM of frontal lobe, while another found a reduction in the superior longitudinal fasciculus (SLF). Peters et al. used tractography to assess the uncinate and arculate fasciculi, cingulum bundle, and corpus callosum but did not find any differences between UHR and controls. Only one previous DTI study has subdivided UHR subjects in terms of their clinical outcome. UHR subjects who later became psychotic had lower FA at presentation than healthy controls in the WM of the left frontal lobe, in a region that includes the anterior thalamic radiation and the inferior frontooccipital fasciculus. Compared with UHR subjects who did not become psychotic, they had lower FA in the WM lateral to the right putamen and in the left superior temporal gyrus but higher FA in left posterior temporal WM.

The aim of the present study was to assess WM integrity in individuals at UHR for psychosis, using both cross sectional and longitudinal analyses. We tested 2 hypotheses. The first was that relative to controls, UHR individuals would show qualitatively similar WM abnormalities to patients in the FEP but that the magnitude of these abnormalities would be less severe. Our second prediction was that within the UHR group, individuals who later developed psychosis would show more marked abnormalities at baseline than those that did not, and these abnormalities would progress longitudinally because they made the transition to psychosis.

To date, DTI studies in subjects at increased risk of psychosis have focused on measuring FA. A subsidiary aim of the present study was to also assess WM integrity in UHR subjects using measures of radial and axial diffusivity. Our corresponding hypothesis was that reductions in FA in UHR subjects would be associated with altered diffusivity.

**Methods**

**Participants**

**UHR Group.** Individuals meeting the Personal Assessment and Crisis Evaluation criteria for the at-risk mental state (n = 32) were recruited from Outreach and Support in South London (OASIS). The diagnosis was based on assessment by 2 experienced clinicians using the Comprehensive Assessment for the At-Risk Mental State (CAARMS). All UHR subjects were naive to antipsychotic medication at the time of the baseline scan. They were followed clinically at monthly intervals during the first year, at 3 monthly intervals during the second and third years, and annually thereafter. Twenty-two UHR subjects completed both clinical follow-up and MRI scan (see figure 1). During this period, 5 developed psychosis and 17 did not. Transition to psychosis was defined according to the criteria in the CAARMS, and a diagnosis of schizophrenia was confirmed at re-assessment 12 months after transition using the Structured Clinical Interview for Diagnostic and Statistical Manual of Mental Disorders, Fourth Edition (DSM-IV) (SCID).

Within the transition subgroup (n = 5), the mean interval between the baseline and follow-up MRI scans was 2 years, while in the nontransition subgroup (n = 17), it was 2.4 years. At the time of the second MRI scan, 3 of the transition subgroup and 2 of the nontransition subgroup were receiving antipsychotic medication (Quetiapine).

**First-Episode Group.** Patients from the same geographical area as the UHR sample who had recently presented with an FEP (n = 15) were recruited from the Lambeth Early Onset (LEO) Service. All met DSM-IV criteria for a schizophreniform psychosis at the time of scanning and met SCID (DSM-IV) criteria for schizophrenia when re-assessed 12 months later. Six of the patients were medication naive, and 9 had received less than 3 weeks of treatment with low doses of atypical antipsychotic medication (mean dose in chlorpromazine equivalents = 189 mg/d; mean duration of treatment = 11.6 d).

**Controls.** Healthy volunteers (n = 32) were recruited from the same geographical area, as the clinical subjects via local advertisements, or from the friends of the clinical subjects.

Handedness was assessed using the Edinburgh Handedness Inventory. Intellectual function (IQ) was estimated using the Wechsler Adult Intelligence Scale, 3rd Edition (WAIS-III). The severity of symptoms in both clinical groups was assessed with the Positive and Negative Symptoms Scale on the day of scanning by a psychiatrist (J.B.W) trained in its use. Level of function was assessed using the Global Assessment of Functioning scale. Exclusion criteria included history of neurological disorder, history of alcohol, or other substance misuse disorder according to DSM-IV criteria. Participants gave written informed consent to participate in the study, which was reviewed and approved by the Joint South London and Maudsley and Institute of Psychiatry Research Research Ethics Committee.
Magnetic resonance imaging was performed on all participants on a 1.5 Tesla GE SIGNA NVi scanner (General Electric, Milwaukee, WI). Following localizer, calibration, and structural scans, DTI data were collected using a cardiac-gated single-shot echo-planar sequence with 60 contiguous 2.5 mm thick near axial slices, matrix size $96 \times 96$ over a 24 cm field of view, zero-filled during reconstruction to a $128 \times 128$ matrix, final reconstructed voxel size $= 1.875 \times 1.875 \times 2.5$ mm$^3$; time echo $= 107$ ms; time repetition $= 15$ R-R intervals. At each scan location, 7 images without diffusion gradients were acquired together with 64 diffusion-weighted images ($b = 1300$ s.mm$^{-2}$) with diffusion sensitization directions distributed over a (hemis)phere.

**Image Analysis**

Images were corrected for head movement, eddy currents, and skull-stripped using FSL (http://www.fmrib.ox.ac.uk/fsl/). The 6 elements of the diffusion tensor were calculated for each voxel using linear regression. FA was calculated and data from all subjects realigned to the bicommissural line of a target image (chosen from the study participants) using an affine followed by nonlinear registration. The nonlinear transformation was then applied to each tensor component, and the warped components were recombined into a single tensor file. In order to allow for the effects of this reorientation, the local tensor orientation was adjusted using the “preservation of principal direction” algorithm implemented within Camino (http://cmic.cs.ucl.ac.uk/camino). Finally, realigned diffusion tensor images of all subjects were used to create a population-specific template to which each subject’s images were then (re-)normalized; this final stage of processing was performed with “dti-tk” toolkit (http://www.nitrc.org/projects/dtitk) and is described in more detail below.

**Population-Specific Template Creation**

A template was created from our cohort of study (patients and controls) in order to avoid the bias associated with using a standard template from a normal population, which is not representative of our patient group. The population-specific template was generated from tensor images, rather than scalar images, such as FA, using an unbiased diffeomorphic method. Whole tensor-based registration was chosen over FA-based registration because this approach has been reported to align WM regions better than scalar-based registration methods. Additionally, templates for FA, axial, and radial diffusivity were calculated from the final tensor template.

**Normalization to the Population-Specific Template**

Images were normalized to the population-specific tensor template using a high-dimensional approach. FA, axial, and radial diffusivity maps were calculated. Finally, the International Consortium for Brain Mapping white matter labels atlas (ICBM-DTI-81) was registered to the 3 population-specific templates (FA, axial, and radial diffusivity) using an affine followed by a nonlinear registration and used as brain mask to restrict subsequent analyses to WM only.

**Group Mapping Analysis**

The main analysis of the data was performed using XBAM v4, a software package developed at King’s College London, Institute of Psychiatry (http://brainmap.co.uk)
which implements a nonparametric approach based on permutations to minimize assumptions of data normality and is based on median statistics to control for outlier effects. Relative to parametric analyses, the nonparametric approach has the additional advantage of allowing test statistics incorporating spatial information such as 3D cluster mass (the sum of suprathreshold voxel statistics), which are generally more powerful than other possible test statistics but for which no parametric approximation is known.

For the cross sectional analysis, between-group differences in the DTI indices of interest (FA, parallel, and perpendicular diffusivity) were estimated by fitting an ANOVA model at each voxel, whereas for the longitudinal analysis, data were analyzed using a nonparametric repeated measures ANOVA.

To test for the interaction between group and time between scans, a series of nonparametric factorial analyses of variance were used. For each analysis, a voxel-level significance threshold within XBAM was initially set to .05 to give maximum sensitivity and to avoid type II errors, and voxels where nonparametric testing of the model gave evidence for rejection of the null hypothesis were highlighted. Three-dimensional spatial clusters generated from the voxels thus highlighted were then subject to more rigorous statistical testing of their cluster mass. At this stage, a cluster mass threshold was computed from the distribution of cluster masses in the permuted data, such that the expected number of type I error clusters under the null hypothesis was less than one over the whole brain. Finally, as multiple groupwise analyses tests were performed on the 3 diffusion indices, results of the cluster analyses were corrected for multiple comparisons in order to further control for false positives.

**Localization of Findings**

Because the population-specific tensor template was not in the Montreal Neurological Institute (MNI) space, significant clusters were warped into the standard MNI space. Scalar image templates were coregistered to the IIT2 DTI brain template using an initial affine registration followed by a nonlinear registration. The transformations so calculated were then applied to the group mapping results. The most likely anatomic localization of each cluster highlighted was finally determined by reference to the IIT2 DTI brain template in the spatial coordinates of the ICBM-152 brain template.

**Statistical Analysis of Clinical and Demographic Data**

Group-wise measures of clinical and sociodemographic variables were analyzed using one-way ANOVA, t test, and chi-square test where appropriate (PASW 18; SPSS Inc, Chicago, IL). When significant differences were found, the Tukey’s honestly significant difference test for pairwise comparisons was applied. Before statistical tests, the data were checked for assumptions of normality and equality of variances. If these assumptions were violated, the Mann–Whitney U test was used.

**Demographic and Clinical Variables**

A summary of demographic and clinical variables is reported in table 1. Eight UHR subjects (25%) developed psychosis (UHR-P) subsequent to baseline (see figure 1). Five of this UHR-P subgroup were re-scanned after the onset of psychosis, along with 17 (of the 24) UHR subjects who had not developed psychosis. Eight (25%) of the 32 healthy controls were also re-scanned. The investigators tried to contact all of the subjects who had been scanned at baseline. However, some were not contactable, and others declined to be re-assessed. The mean interval between the baseline and follow-up scans in the total UHR sample was 15 months (range 32), while in the UHR-P and UHR-NP subgroups, it was 23.7 (range 15.8) and 29.3 (range 32) months, respectively. The mean interscan interval in controls was 45.7 months (range 28 months). The interscan interval did not differ between the UHR-P and UHR-NP groups but was significantly longer in controls than UHR subjects (P < .001).

At the time of the follow-up scan, 77% of the UHR sample were still antipsychotic naive (and were not taking any other psychotropic medication), while 23% of them were receiving antipsychotic treatment. Within the UHR-P and UHR-NP subgroups, the corresponding figures were 40% and 60%, and 88.2% and 11.8%, respectively. In the longitudinal analysis, because the interscan interval was longer in controls than UHR subjects, the time between scans was used as a covariate but in order to allow for the potential confounding effects of correlations between the covariate and independent variables this introduces, we also repeated the longitudinal analysis without covariate adjustment.

**Results**

**Cross Sectional Comparisons at Baseline**

**FEP vs UHR vs Healthy Controls.** At baseline, there were significant linear relationships for differences across the 3 groups in FA (for a detailed description of the results, see figure 2A and online supplementary table S1) in 2 clusters. In both clusters, FA was lowest in the FEP group, highest in controls, and intermediate in the UHR group (see figure 2B). The first cluster comprised voxels in areas corresponding to the splenium and body of the corpus callosum, the left inferior and SLF, and the left inferior frontooccipital fasciculus (for details, see online supplementary table S1). The second cluster included the right external capsule, the retrolenticular part of the right internal capsule, and the right posterior corona radiata (for details, see online supplementary table S1).
There was a larger set of regions where there was a significant linear relationship for radial diffusivity across the groups, with it being greatest in the FEP group, lowest in controls, and intermediate in the UHR group (see figure 3).

Linear relationship for axial diffusivity differences was evident in many clusters (see online supplementary figure S4). In some clusters, axial diffusivity was highest in the FEP group and lowest in the controls, but in others, the opposite relationship applied.

Post hoc paired comparisons revealed that differences in FA, radial, and axial diffusivities were driven by differences between the FEP and control groups, while the differences between the UHR group and controls were not significant. There were no FA or RD clusters where the linear relationship across groups was in the opposite direction (eg. FA highest in FEP and radial diffusivity lowest in FEP).

**Findings at Baseline in UHR Subjects Who Later Developed Psychosis**

Within the UHR group, there were no differences in FA, axial, or radial diffusivity between subjects who developed psychosis (UHR-P) and those who did not (UHR-NP). Similarly, there were no significant differences between the UHR-P group and healthy controls.

**Longitudinal Analysis**

There was a significant group (UHR-P vs UHR-NP) by time (baseline vs follow-up scan) interaction on FA in a cluster spanning the anterior limb of the left internal capsule (ALIC), body of the corpus callosum, left superior corona radiata, and left superior frontooccipital fasciculus \( (P = .0009) \). In this cluster, there was a longitudinal reduction in FA in the UHR-P group but a slight increase in the UHR-NP group (see figure 4), although these within-group changes were not themselves significant. This result did not change when the “nuisance covariate” (time between scans) was excluded from the analysis. There were no significant groups by time interactions for axial or radial diffusivity.

**Cross Sectional Comparisons at Follow-up**

At follow-up, there were no significant differences in FA between the UHR subjects who had developed psychosis and the UHR subjects who had not. However, there was greater radial diffusivity in one cluster in middle cerebellar peduncle \( (P < .001) \), while axial diffusivity was reduced in the middle cerebellar peduncle and left cerebral peduncle \( (P = .001) \) but greater in the right superior and posterior corona radiata, splenium, and body of the corpus callosum \( (P < .0004) \); for details, see online supplementary table S2.

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**Table 1. Demographic Characteristics of the Experimental Groups**

<table>
<thead>
<tr>
<th>Variable</th>
<th>Baseline</th>
<th>Follow-up</th>
</tr>
</thead>
<tbody>
<tr>
<td>Group size</td>
<td>15</td>
<td>32</td>
</tr>
<tr>
<td>Age at DTI scan: years (SD)</td>
<td>24.1 (5.2)</td>
<td>25.9 (5.0)</td>
</tr>
<tr>
<td>Gender (male/female)</td>
<td>14/1</td>
<td>26/6 (4.3)</td>
</tr>
<tr>
<td>Handedness (right/left/ambivalent)</td>
<td>15/0/0</td>
<td>20/0/0</td>
</tr>
<tr>
<td>IQ (SD)</td>
<td>97.8 (6.7)</td>
<td>97.2 (8.9)</td>
</tr>
</tbody>
</table>

**Note:** FEP, first episode of psychosis; UHR, ultra high risk; HC, healthy controls; WAIS-III, Wechsler Adult Intelligence Scale III.

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Discussion

Our first hypothesis was that the UHR state would be associated with alterations in WM integrity qualitatively similar to, but less severe than, those seen in schizophrenia. Consistent with this hypothesis, we found that, at baseline, FA, radial diffusivity, and axial diffusivity values in UHR subjects were intermediate relative to those in the first-episode patients and controls. These differences were evident in regions of WM corresponding to the major associative fibers that connect fronto-parieto-temporal (SLF) and fronto-parieto-occipital regions (inferior frontooccipital fasciculus), commissural fibers (corpus callosum), and cortico-subcortical pathways (corona radiata, corticospinal tract, and corticopontine tract). The findings in the SLF corroborate previous findings in FEP and UHR populations.22

Our results suggest that structural abnormalities in fronto-temporo-parietal connections are present before the onset of psychosis, in line with functional connectivity findings in UHR subjects.3 These abnormalities are comparable to those reported in DTI studies of patients with FEP.18,19,35 We also found reduced FA in the splenium of the corpus callosum in the UHR group. A previous study in UHR subjects did not find differences in this region,23 whereas reduced FA in the splenium of the callosum has been reported in some studies of FEP.17,19

Our second hypothesis was that DTI abnormalities would be more marked in UHR subjects who later developed psychosis than in those who did not. Consistent with this prediction, we found a significant interaction between “group” (UHR-P and UHR-NP) and time, which post hoc analyses indicated was driven by a longitudinal reduction in FA the UHR-P group (figure 4). This difference was evident in a region that comprised the left anterior limb of the internal capsule (ALIC), left corona radiata, left superior frontooccipital fasciculus, and anterior body of the corpus callosum. To our knowledge, this is the first evidence that transition to psychosis in UHR subjects is associated with longitudinal changes in WM integrity. The ALIC is traversed by...
axonal fibers that connect the thalamus to the prefrontal cortex and form part of a circuit linking the frontal lobe and basal ganglia. WM abnormalities have previously been reported in the ALIC, body of the corpus callosum, and along the superior occipitofrontal fasciculus in FEP, and oligodendrocyte abnormalities have been described in the prefrontal WM in schizophrenia. The localization of our findings is also consistent with those in previous DTI studies of individuals at high genetic risk of schizophrenia.

We did not find significant differences at baseline between UHR subjects who subsequently developed psychosis and UHR subjects who did not. However, a recent DTI study reported that, at presentation, the former subgroup had lower FA than the latter in the right putamen and left superior temporal lobe but higher FA in a posterior part of the left temporal lobe. This difference in findings may reflect differences in the nature of the respective UHR samples. Although the total number of UHR subjects was similar, a greater proportion developed psychosis in the previous study, which may have provided more power when comparing the UHT-P and UHT-NP subgroups. On the other hand, in the Bloemen study, the proportion of UHR subjects who had already been treated with antipsychotics was significantly greater in the UHR-P than in the UHR-NP group, whereas at baseline, all our UHR subjects were medication naive. The potentially confounding

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**Fig. 3.** Linear changes in RD across 3 groups. Figure (A) displays areas of increased radial diffusivity (FEP > UHR > HC); images are radiologically oriented (participant’s left is to the right). The figure (B) shows differences in RD for significant clusters (median ± range). Radial diffusivity is measured in 10⁻⁶ mm²/s.

**Fig. 4.** Group x time interaction analysis results. Fractional anisotropy map (A) indicating the areas where there is an interaction between group membership and time between scans. Image is radiologically oriented (participant’s left is to the right). Plot of FA values (median ± 95% CI) extracted from the significant cluster (B).
effects of medication are discussed further below. The UHR subjects in the previous study were also around 4 years younger than in our study, and the pattern of DTI findings in patients who develop psychosis appears to vary according to the age of the subject at illness onset. A previous volumetric study of WM in UHR subgroups found that, at baseline, individuals who developed psychosis (UHR-P) significantly differ from subjects who did not (UHR-NP). There are several possible explanations for this difference in findings. Methodological differences between our study and the one by Waltersfang et al may account for these inconsistencies. Another possible explanation for this might be that the pathophysiological processes underlying WM volume changes in psychosis may not be reflected by changes in FA. Our results suggest that further research is needed to understand how volumetric and diffusion changes relate to each other in UHR individuals.

We also predicted that alterations in FA in UHR subjects would be associated with changes in axial and radial diffusivity. This hypothesis was confirmed, although the relationship between alterations in FA and in diffusivity varied according to the site of the findings (see online supplementary table S3). Alterations in radial diffusivity have been associated with demyelination in animal models. However, we were not able to directly assess myelination. While increased radial diffusivity may suggest axonal damage, in some regions, this was associated with increased axial diffusivity, which is evident when fibers are tightly aligned within the WM. In other areas, radial diffusivity was increased despite no alteration in FA, while in the ALIC, there was reduced FA but no diffusivity changes. Further work is required to clarify the basis of these different relationships between FA and diffusivity.

We acknowledge some limitations to our study. Although larger than those in most previous DTI studies of UHR subjects, our sample was still modest, and the findings require confirmation in a larger group. Given the small number of females involved in the study, we could not assess the effects of gender on DTI results. Because 3 of the UHR subjects who developed psychosis had been started on antipsychotic medication by the time of the follow-up scan, we cannot exclude the possibility that the longitudinal findings in this subgroup were influenced by treatment after the onset of psychosis. However, previous DTI studies in schizophrenia have not identified a clear effect of antipsychotic medication on FA. Furthermore, a recent meta-analysis of antipsychotic-naive voxel-based morphometry (VBM) studies showed that cortical volume loss observed at the onset of psychosis is independent of antipsychotic treatment. Group-mapping analyses of FA maps have been criticized for inaccuracies in the alignment of individual images to the template. We used a diffeomorphic deformable tensor-based image registration because it registers DTI images better than other techniques, reduces the susceptibility to false positives due to tensor shape confounds, and improves the sensitivity to detect anisotropy changes. However, we acknowledge that while misregistration can be minimized by the use of voxel-based or tract-based analysis techniques, it can never be completely eliminated, and results should therefore always be interpreted in light of this potential confound. Data were analyzed using a whole brain rather than a region of interest (ROI) approach because the existing DTI literature indicates that multiple tracts are affected in schizophrenia and in UHR populations.

In conclusion, these data suggest that the UHR state is associated with reduced WM integrity in similar areas to those affected in FEP, but to a lesser degree. Furthermore, we have provided the first evidence that the onset of psychosis in UHR subjects may be associated with a longitudinal progression of abnormalities in the left frontal WM.

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Supplementary Material

Supplementary material is available at http://schizophreniabulletin.oxfordjournals.org.

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